

SIMULATION OF COMPLEX NONLINEAR ELASTIC BODIES USING LATTICE DEFORMERS

Taylor Patterson

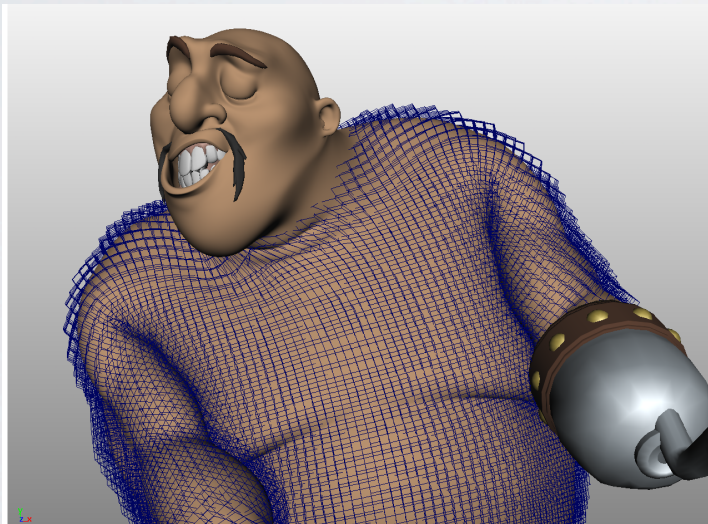
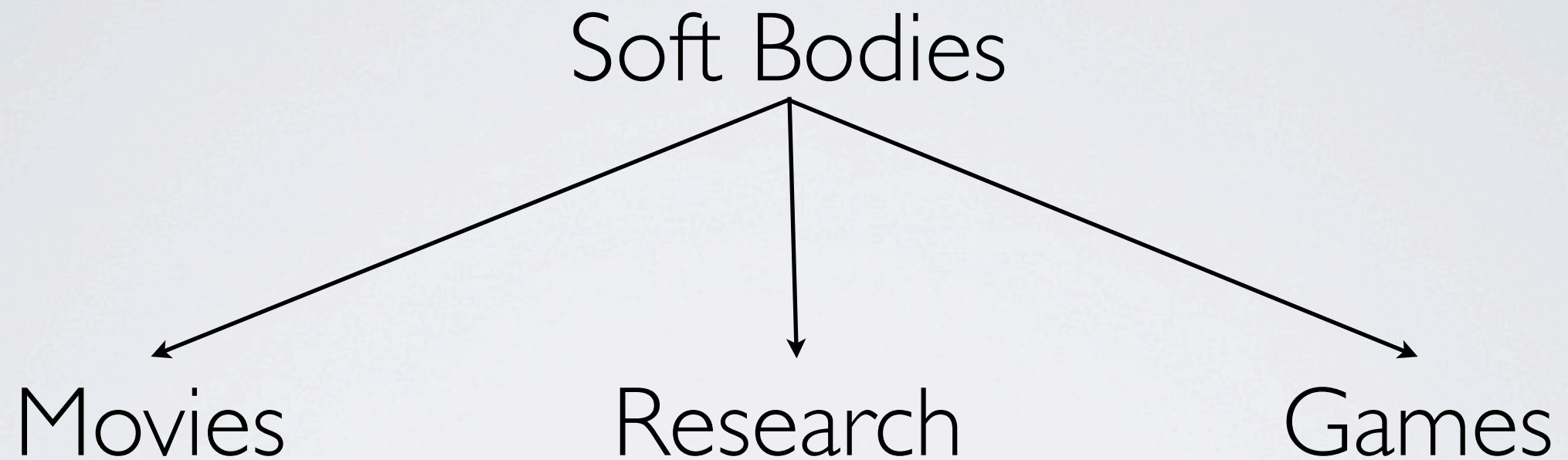
Department of Computer Sciences
University of Wisconsin-Madison

February 8, 2013

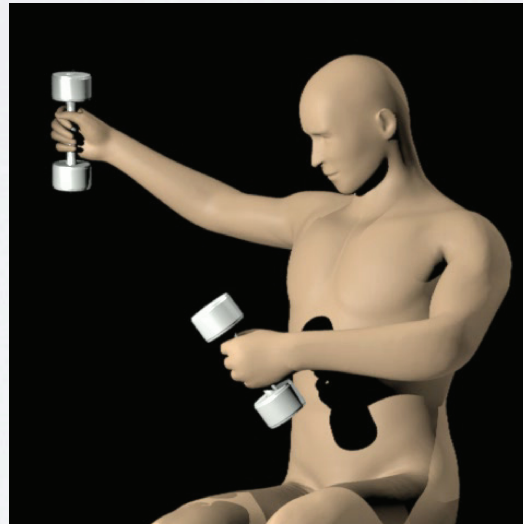
INTRODUCTION: SOFT BODIES

Soft Bodies

INTRODUCTION: SOFT BODIES



[McAdams, et al. 2011]



[Lee, et al. 2009]

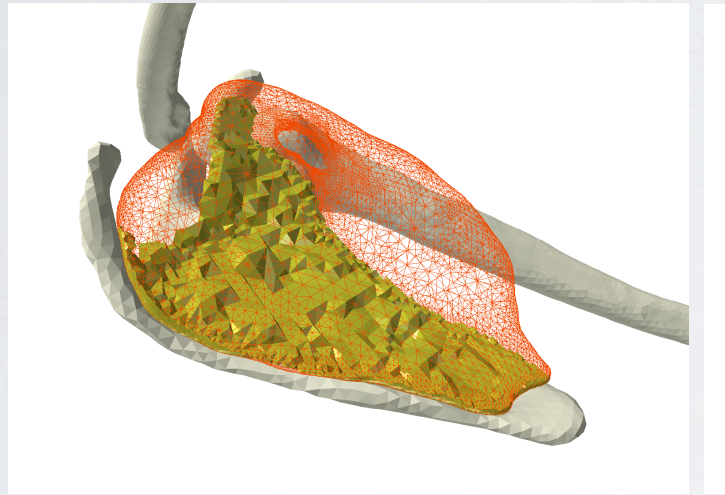


[Parker, et al. 2009]

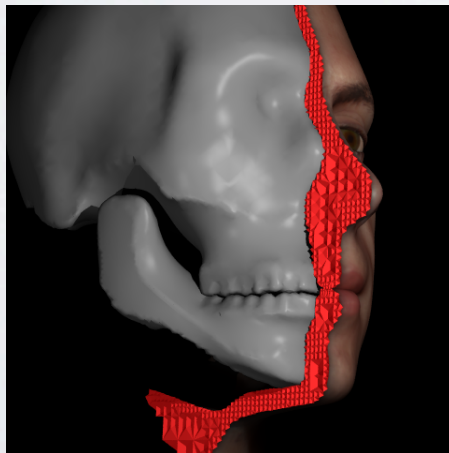
INTRODUCTION: SOFT BODIES

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Conforming Meshes



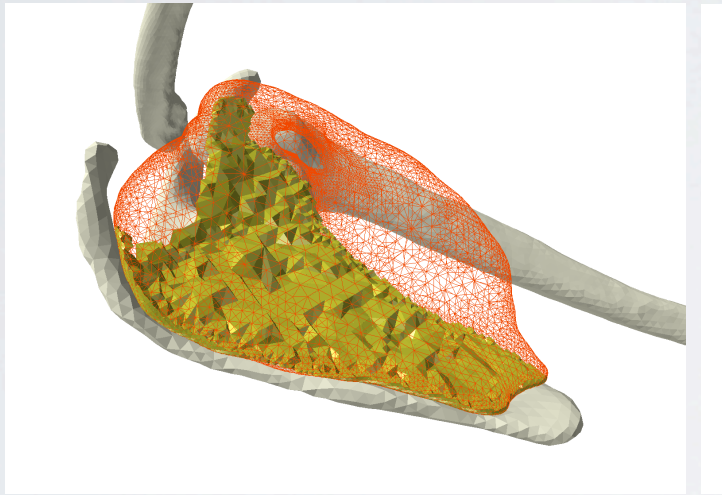
[Teran et. al. 2005]



[Sifakis et. al. 2005]

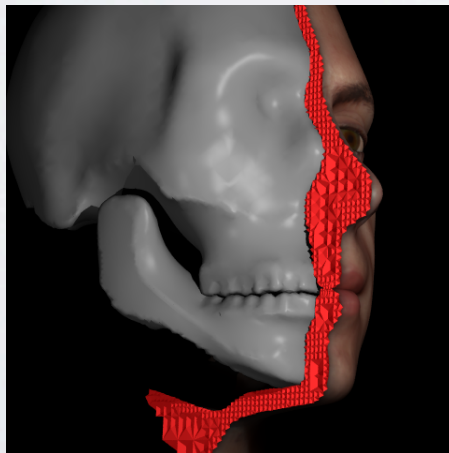
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Conforming Meshes



[Teran et. al. 2005]

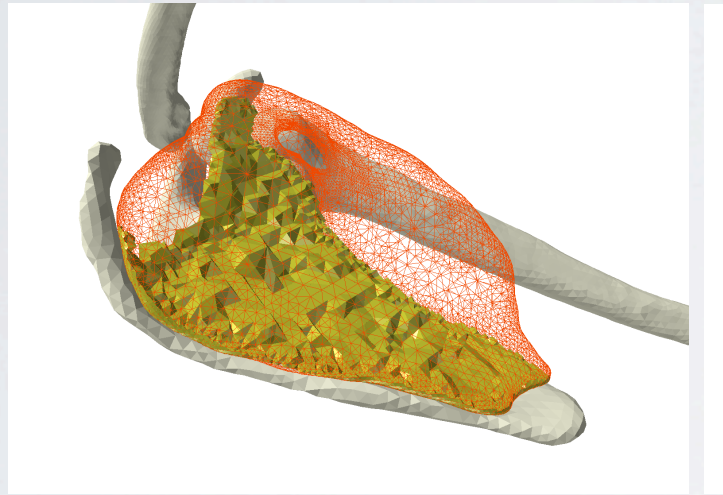
VS.



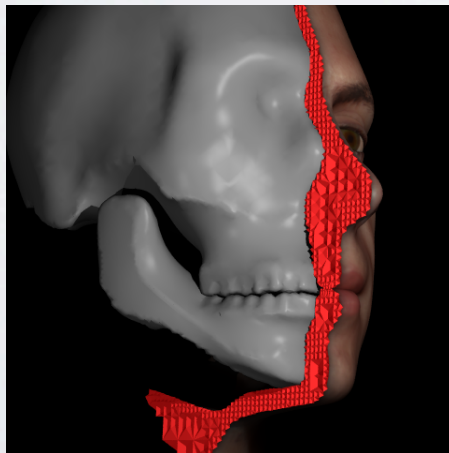
[Sifakis et. al. 2005]

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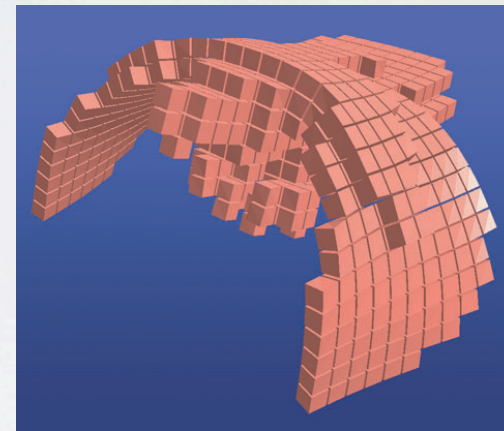


[Teran et. al. 2005]



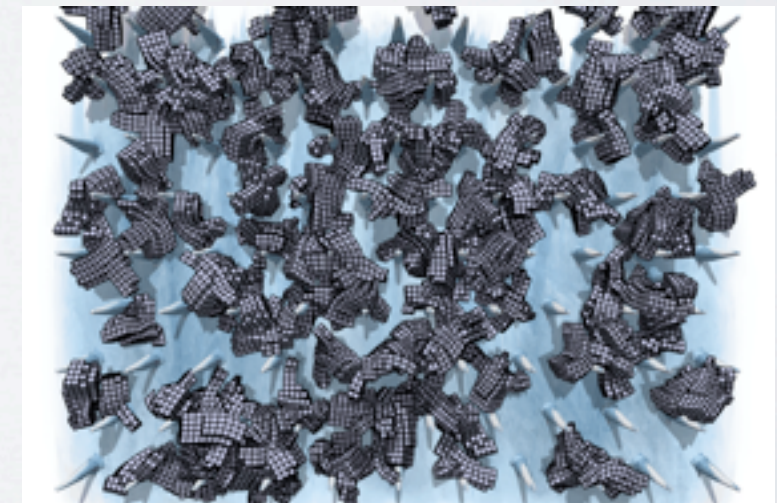
[Sifakis et. al. 2005]

Embedded Deformers



VS.

[Müller et. al. 2004]



[Rivers, A. & James, D. 2007]

FEATURES

Arbitrary Materials

Incompressibility

Sub-voxel Precision

Robust

Parallelism

FEATURES

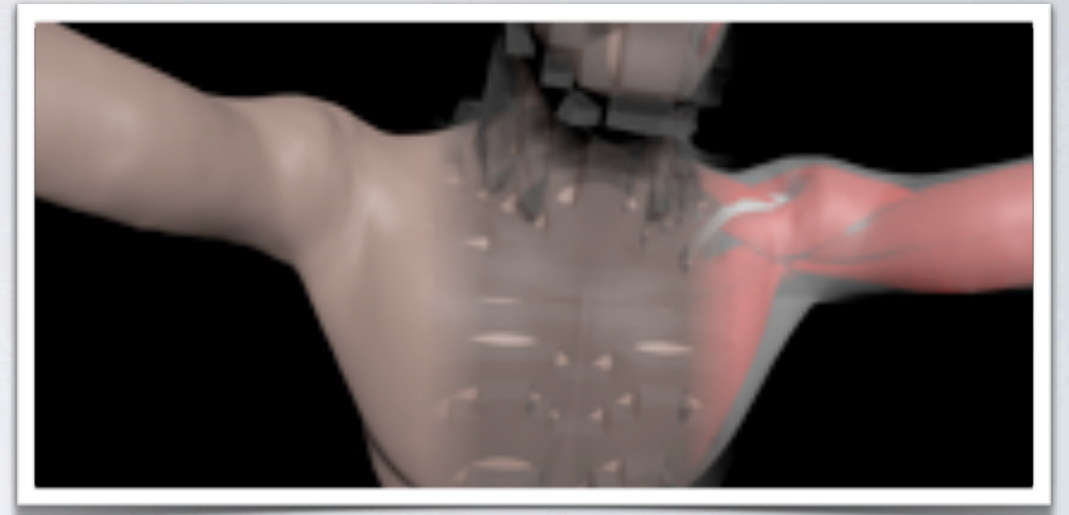
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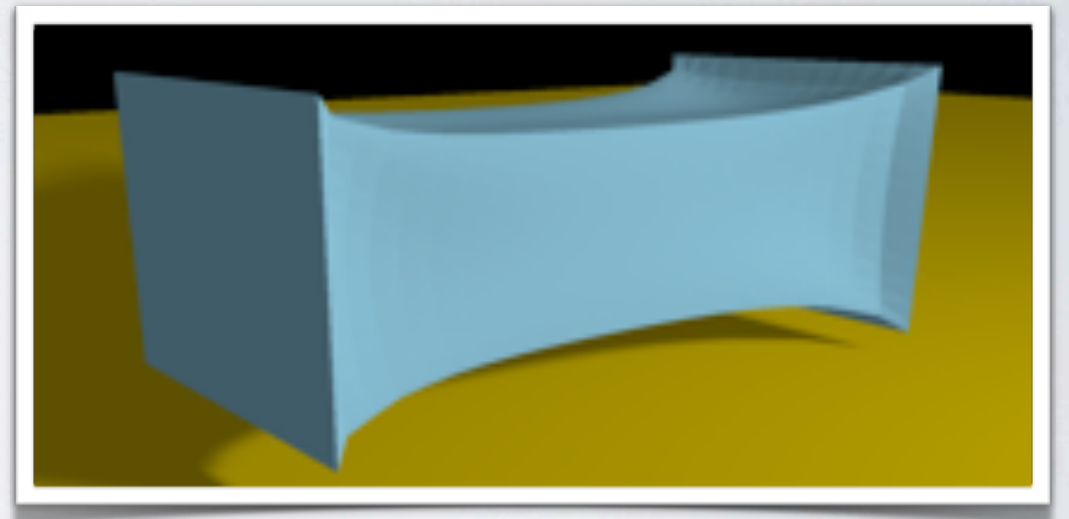
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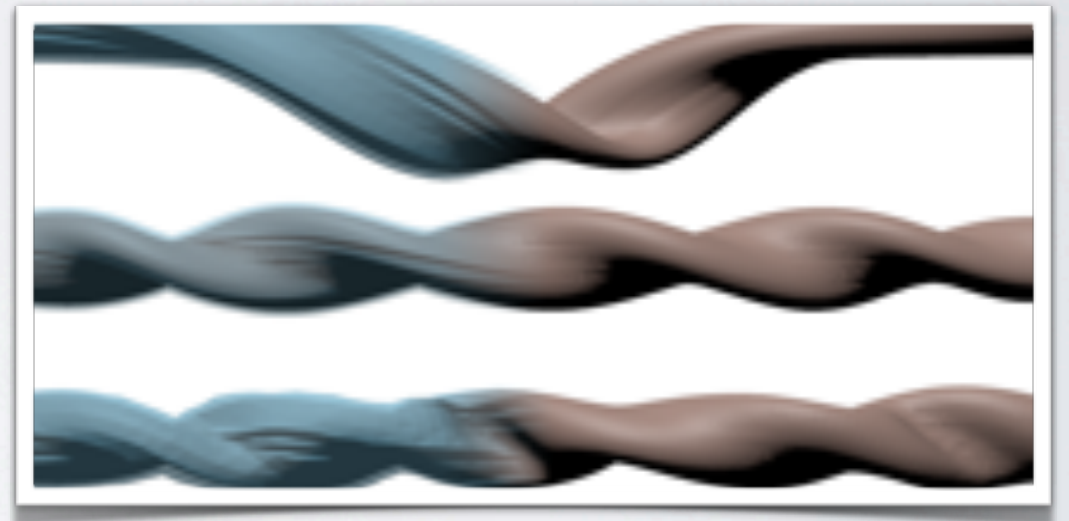
✓ Arbitrary Materials

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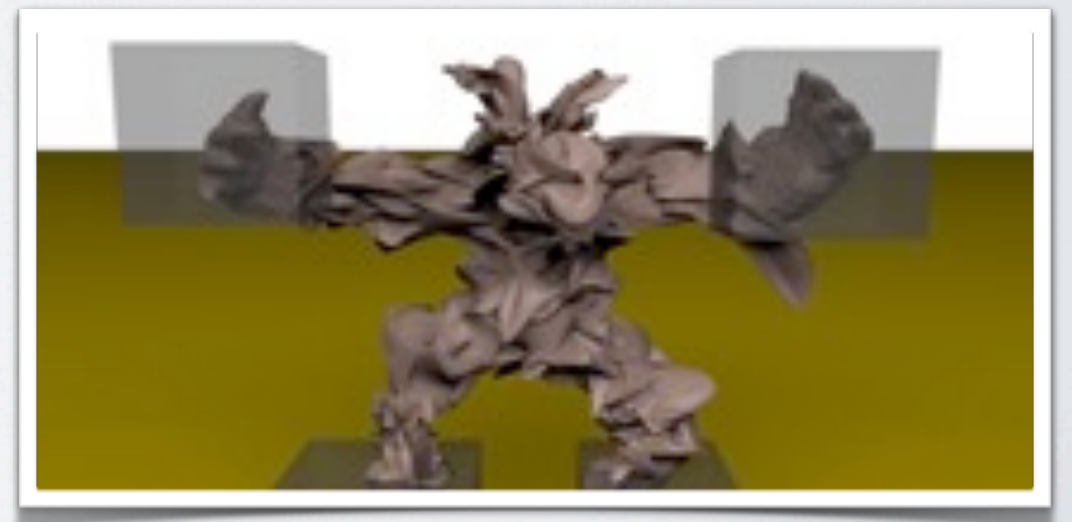
Parallelism

FEATURES

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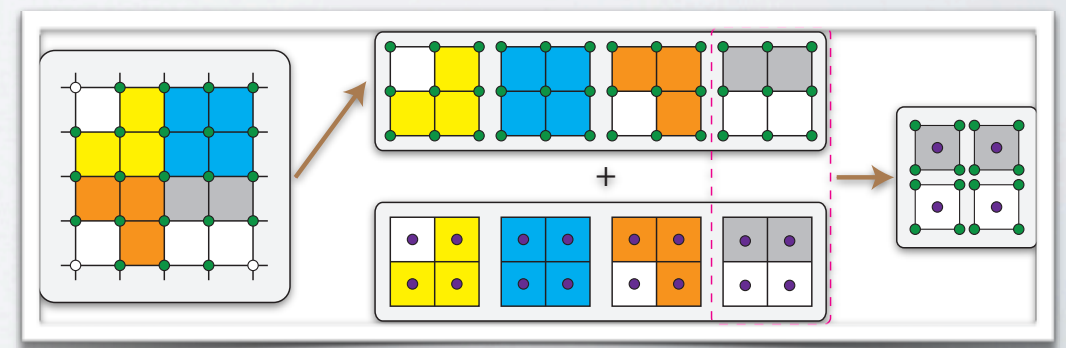
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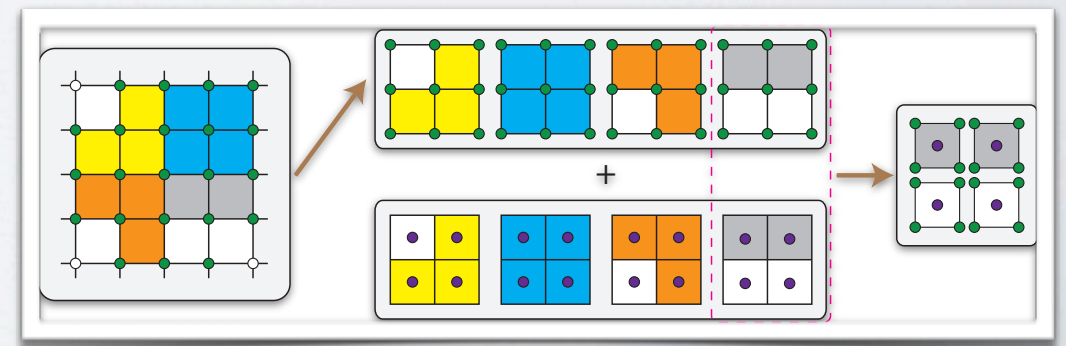
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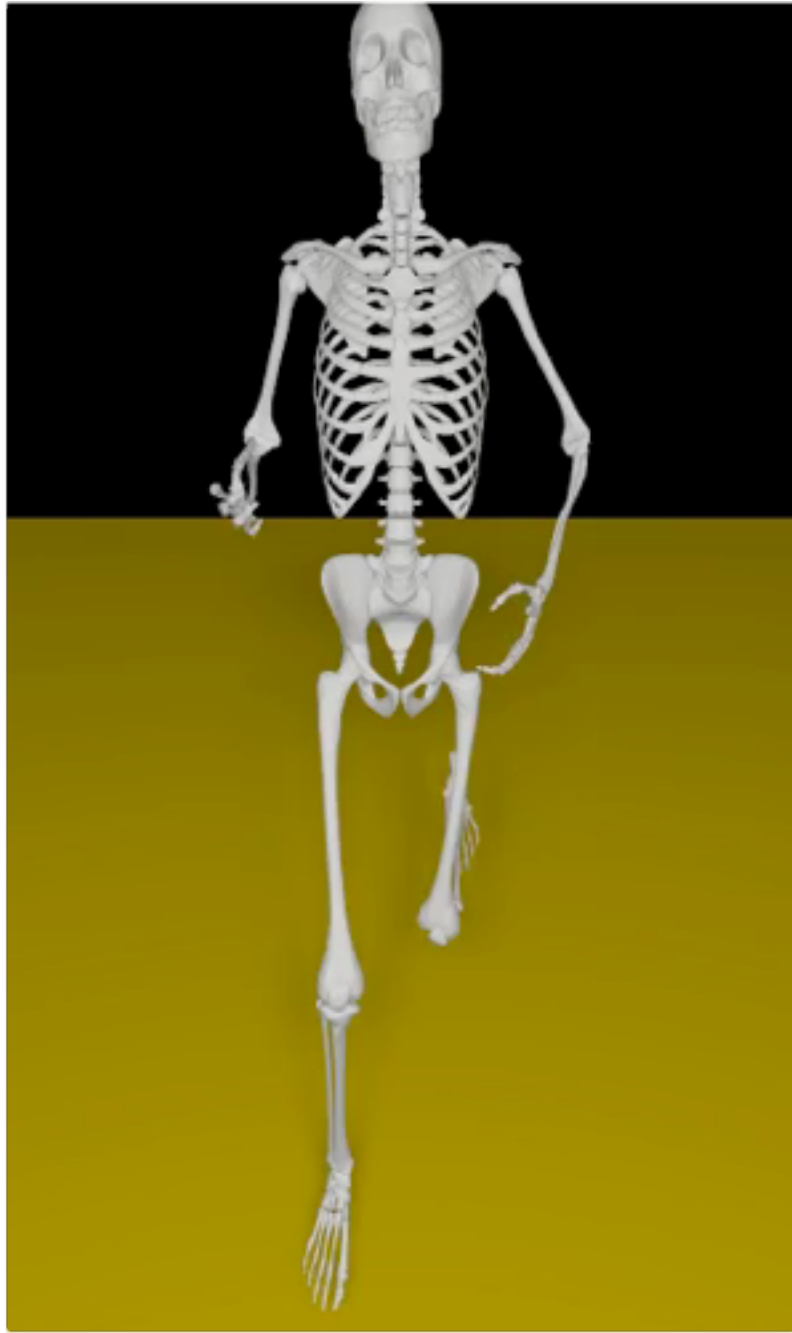
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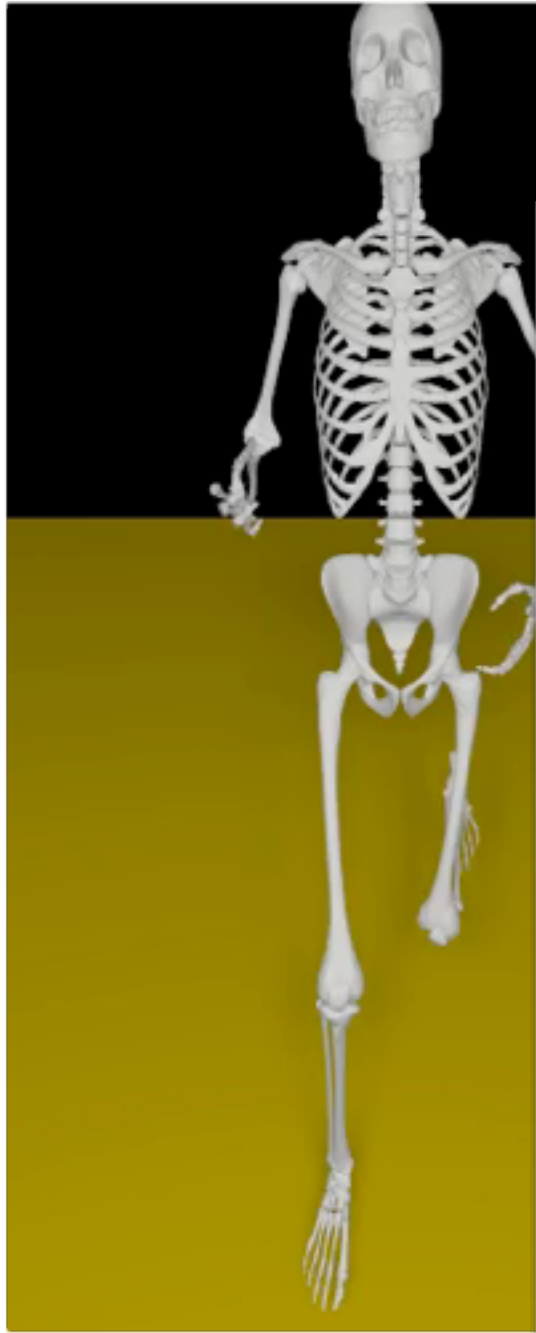
✓ Parallelism

MOTIVATION

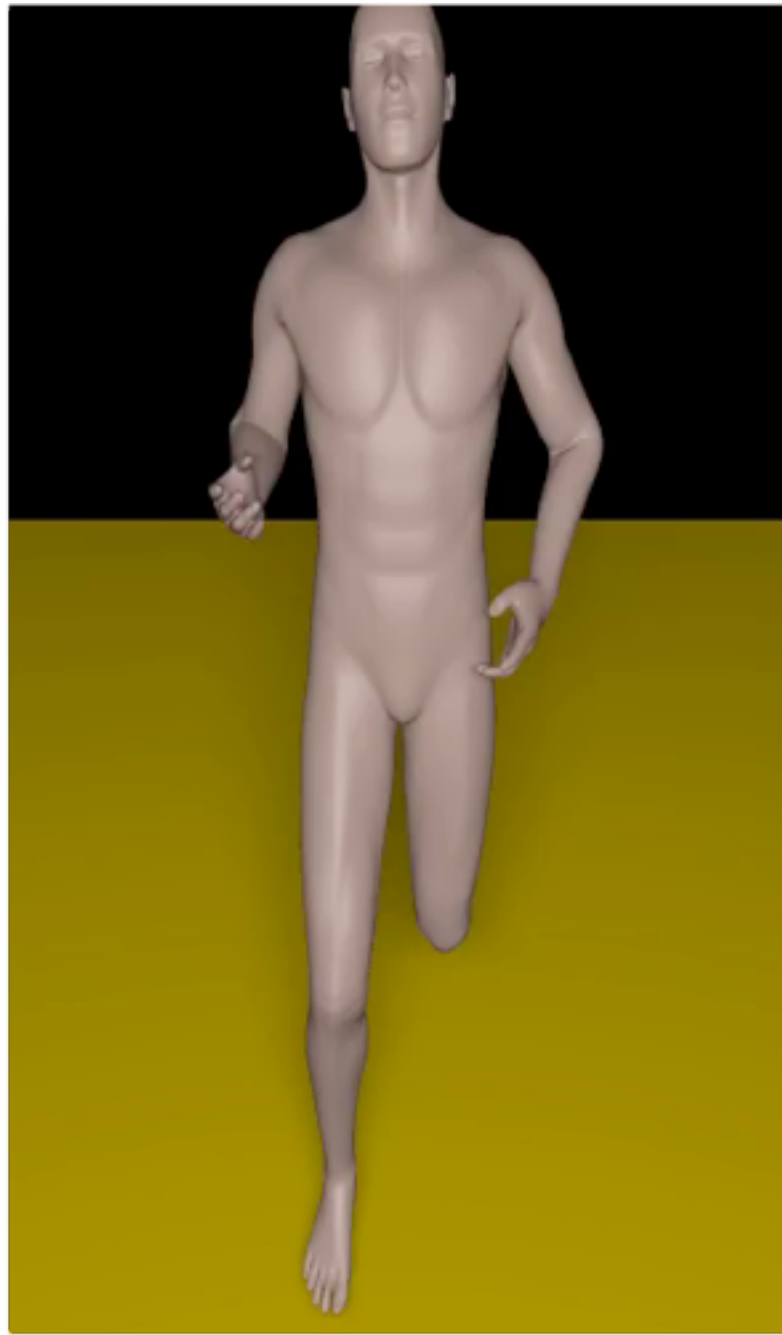
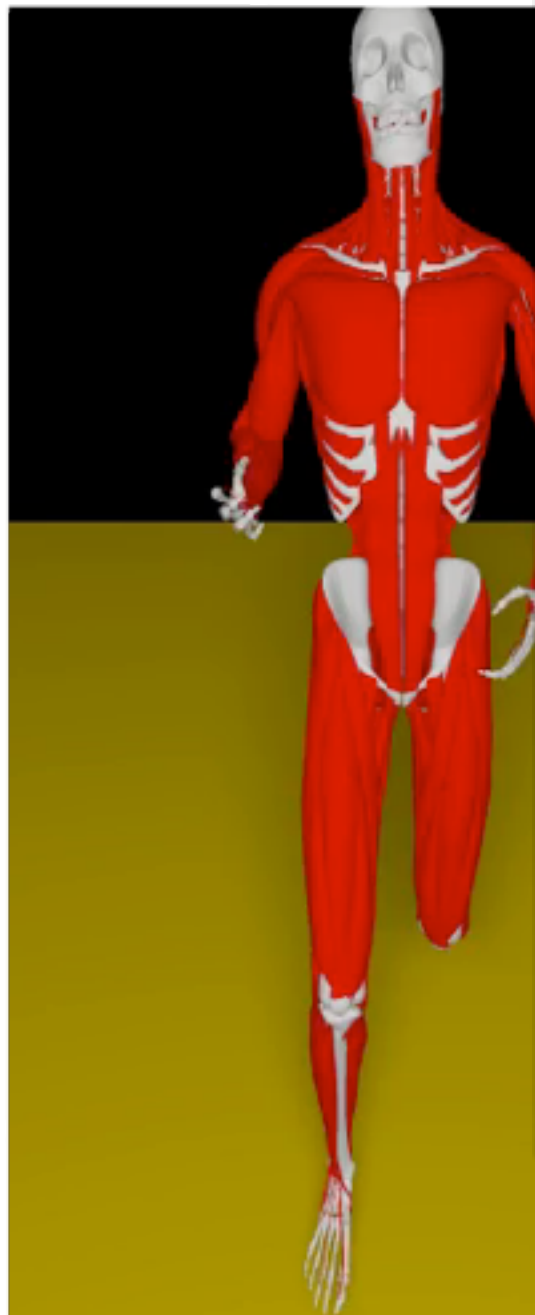
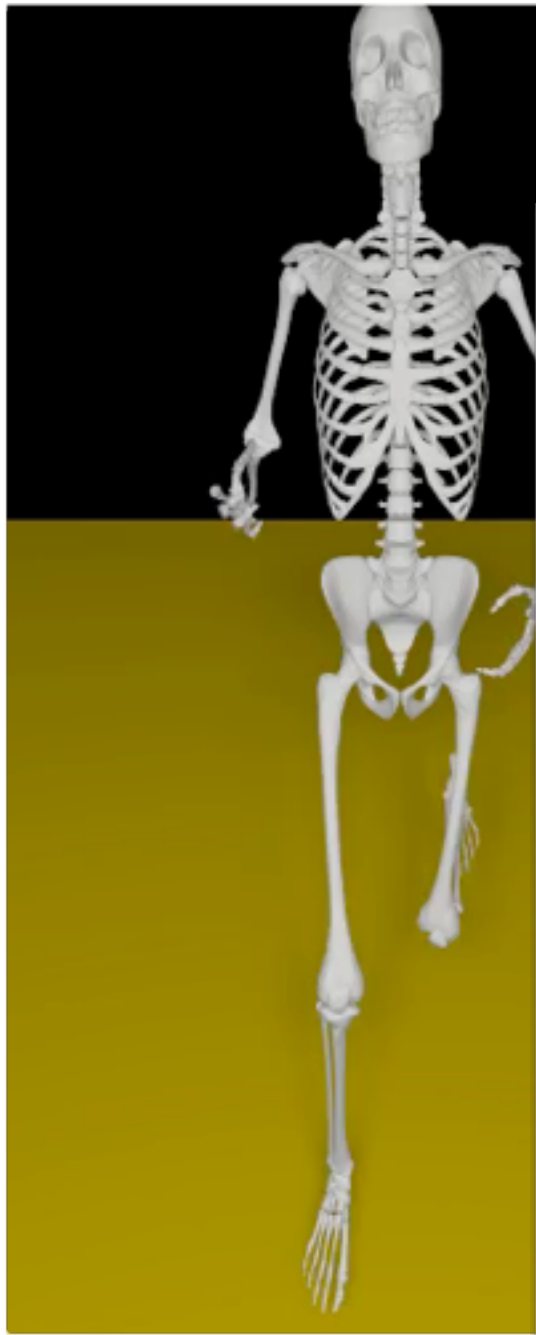
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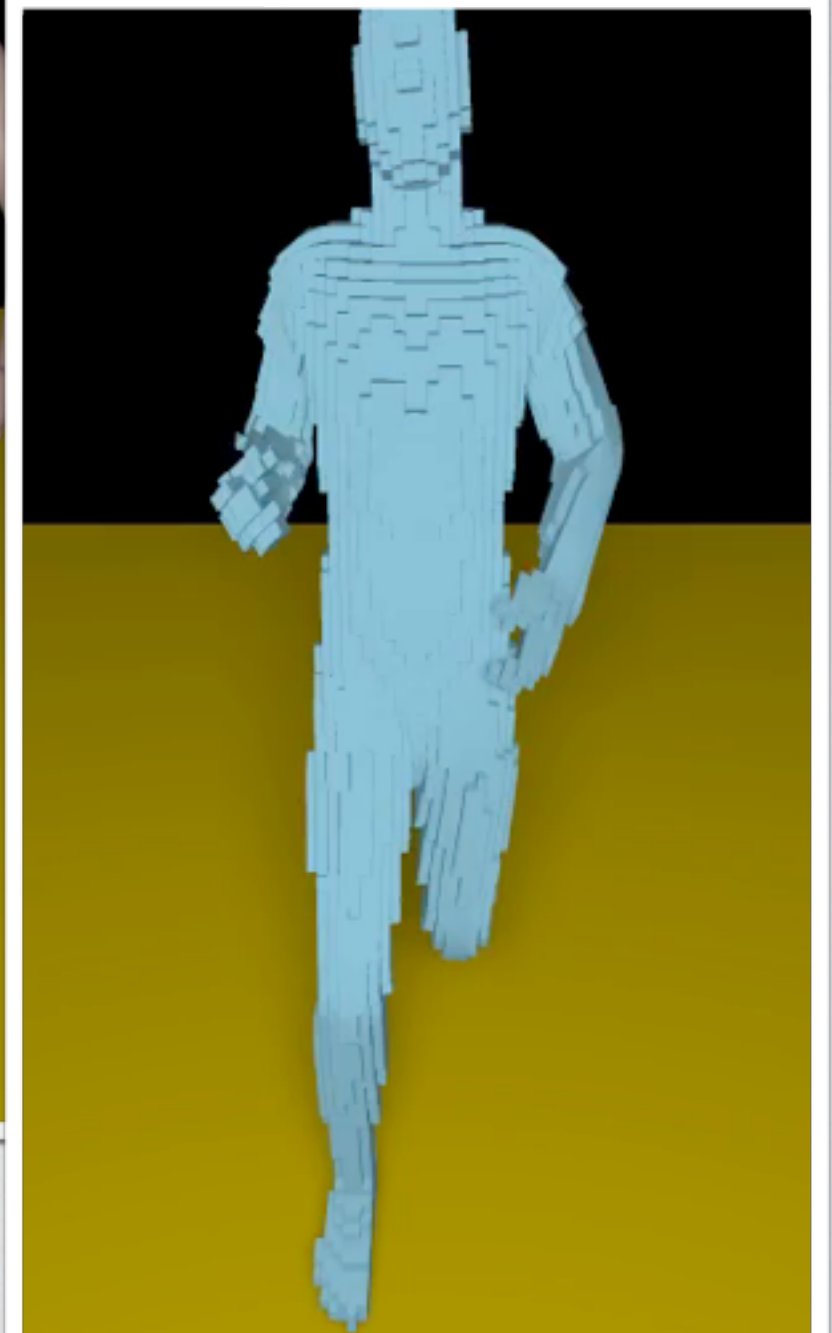
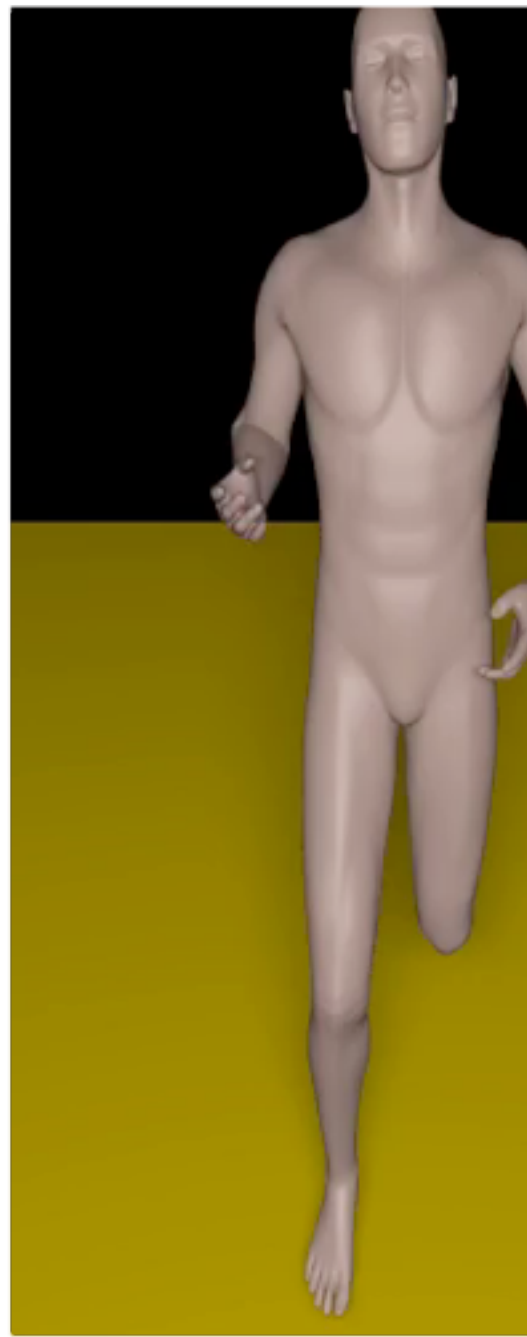
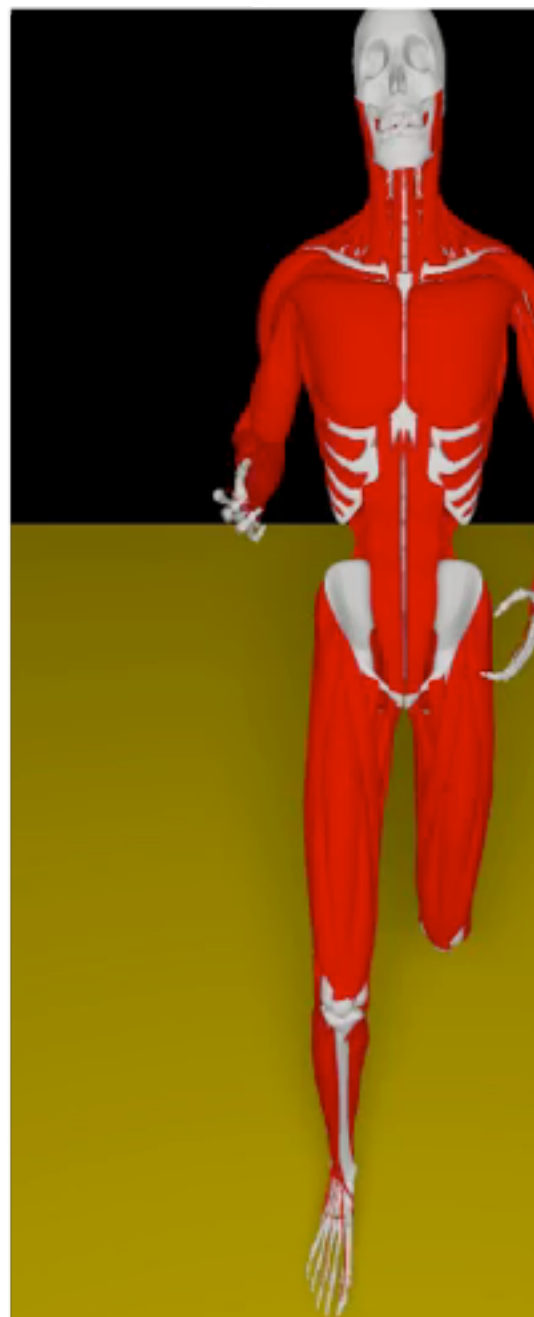
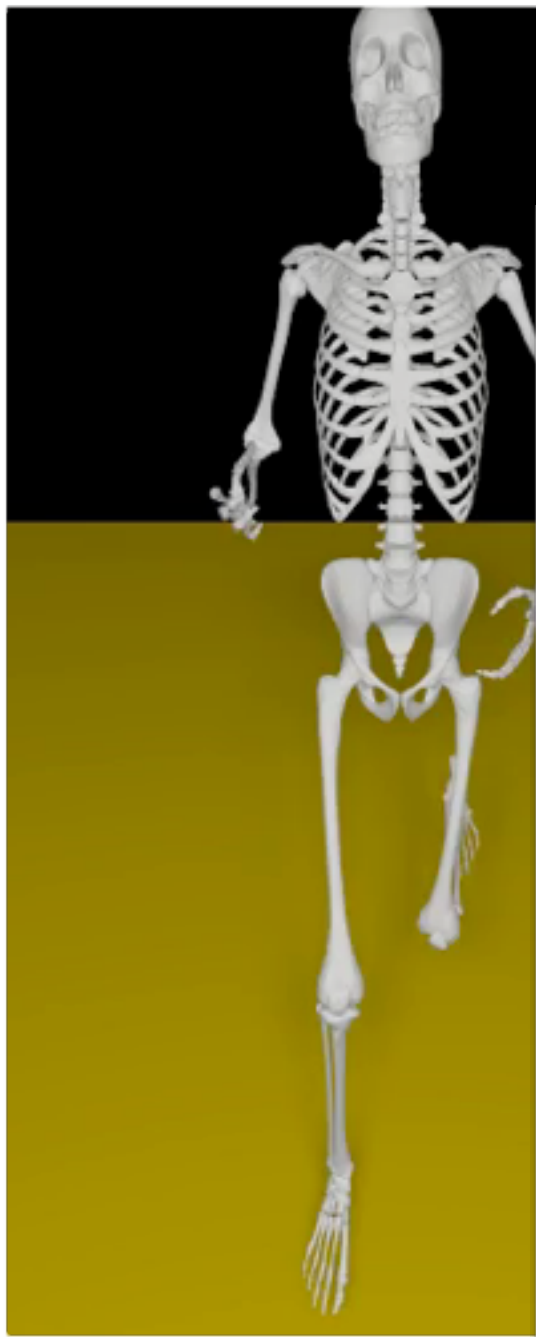
MOTIVATION



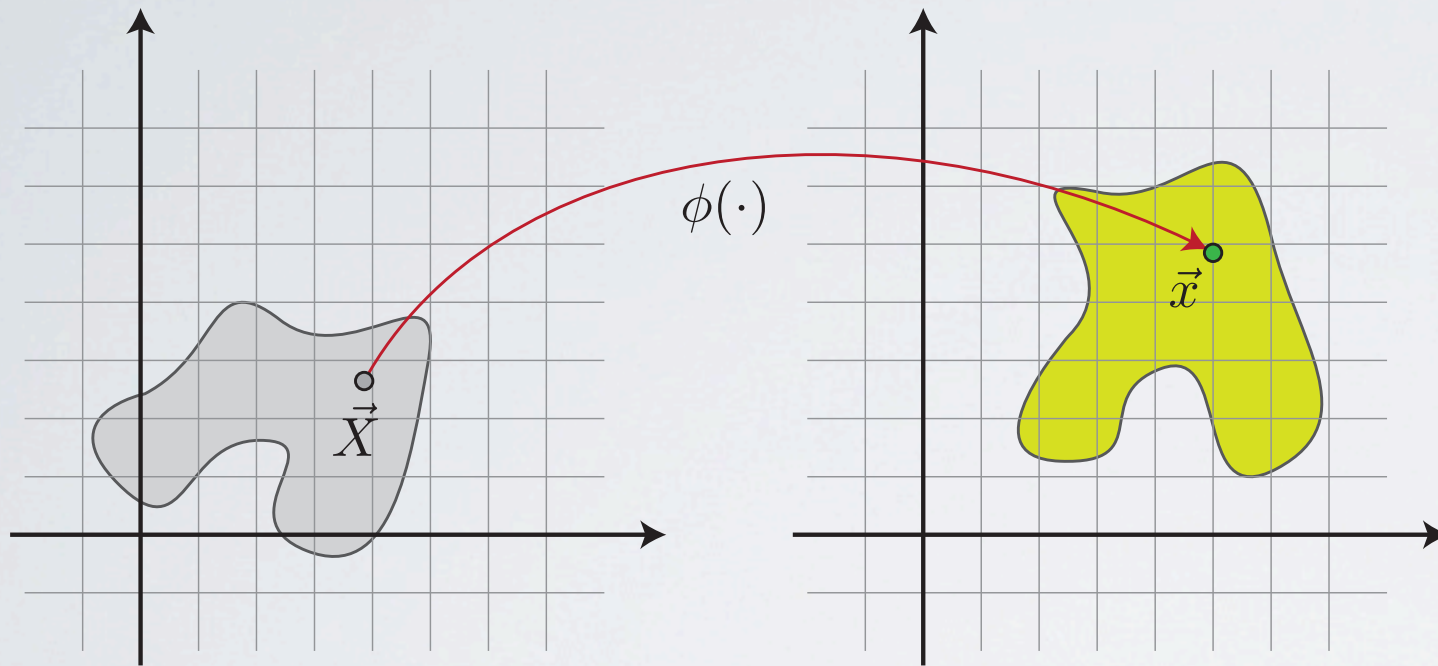
MOTIVATION



MOTIVATION



THE BASICS



Deformation Map

$$\phi = \mathbb{R}^3 \rightarrow \mathbb{R}^3$$

Deformation Gradient

$$F = \partial\phi/\partial X$$

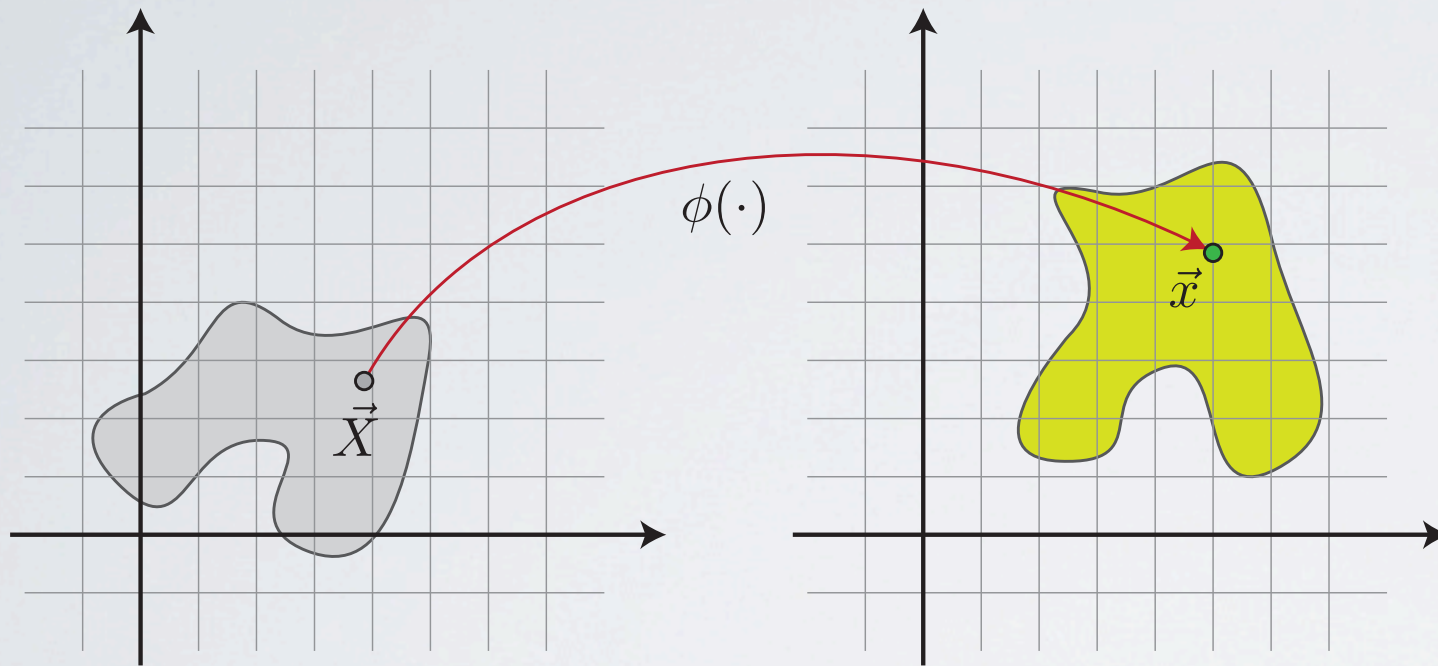
Energy Density

$$\Psi = \Psi(F)$$

Elastic Energy

$$E = \int_{\Omega} \Psi(F) \delta X$$

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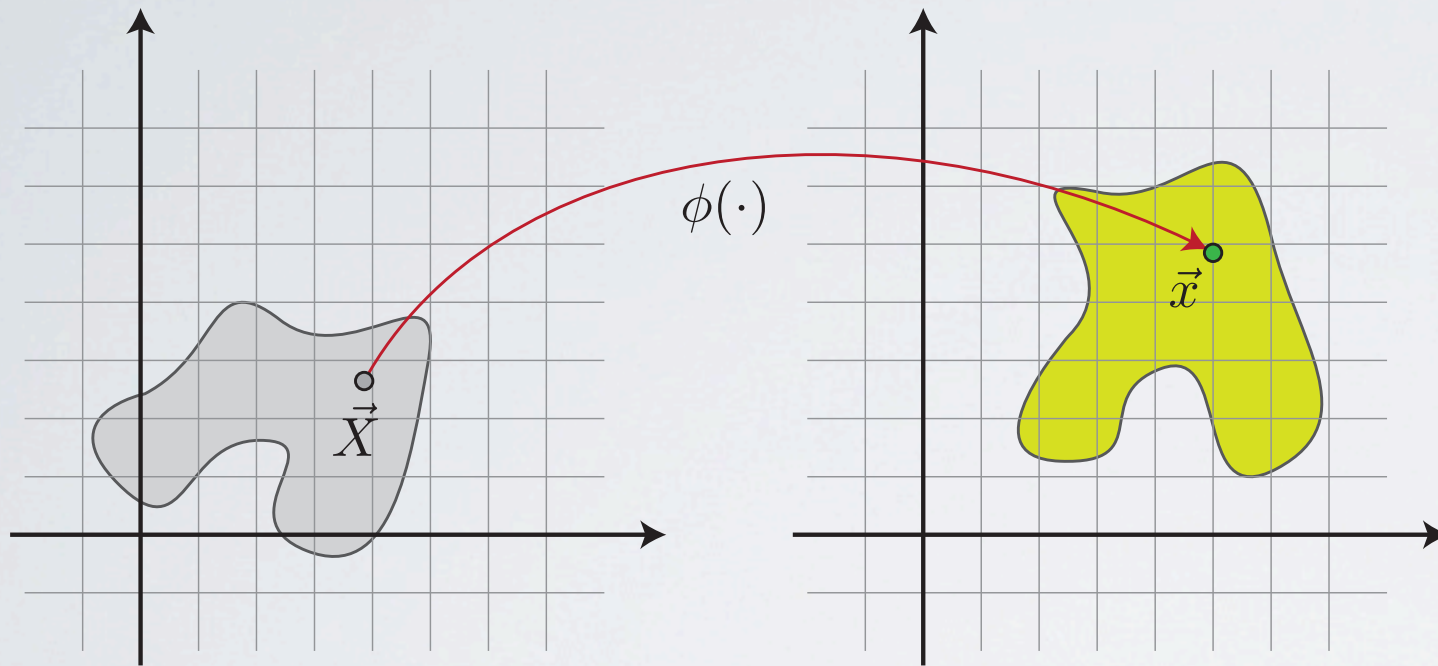
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Neohookean elasticity

$$\Psi = \frac{\mu}{2} (\|F\|_F^2 - 3) - \mu \log(J) + \frac{\kappa}{2} \log^2(J)$$

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Apply Incompressibility Adjustment



THE BASICS

Start with Energy Density



Apply Incompressibility Adjustment



Compute Discrete Energy \hat{E}



THE BASICS

Start with Energy Density



Apply Incompressibility Adjustment



Compute Discrete Energy \hat{E}



Derive Nodal Forces $f(x)$



THE BASICS

Start with Energy Density



Apply Incompressibility Adjustment



Compute Discrete Energy \hat{E}



Derive Nodal Forces $f(x)$



Find Equilibrium $f(x) = 0 \implies \min \hat{E}$

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Start with Energy Density

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Materials and
Incompressibility

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Boundary Cell Treatment

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Materials and Incompressibility

Boundary Cell Treatment

Newton-Raphson Iteration

FEATURES

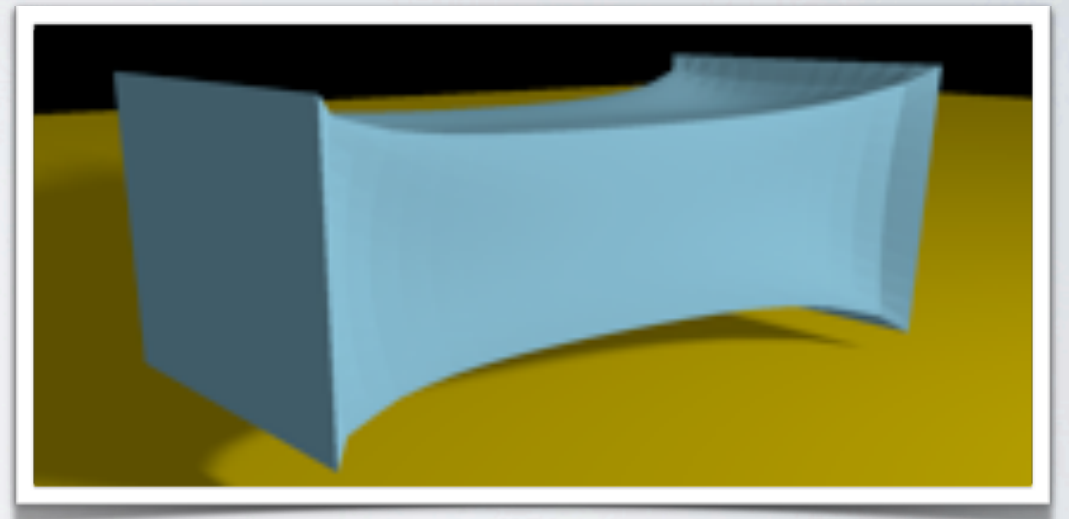
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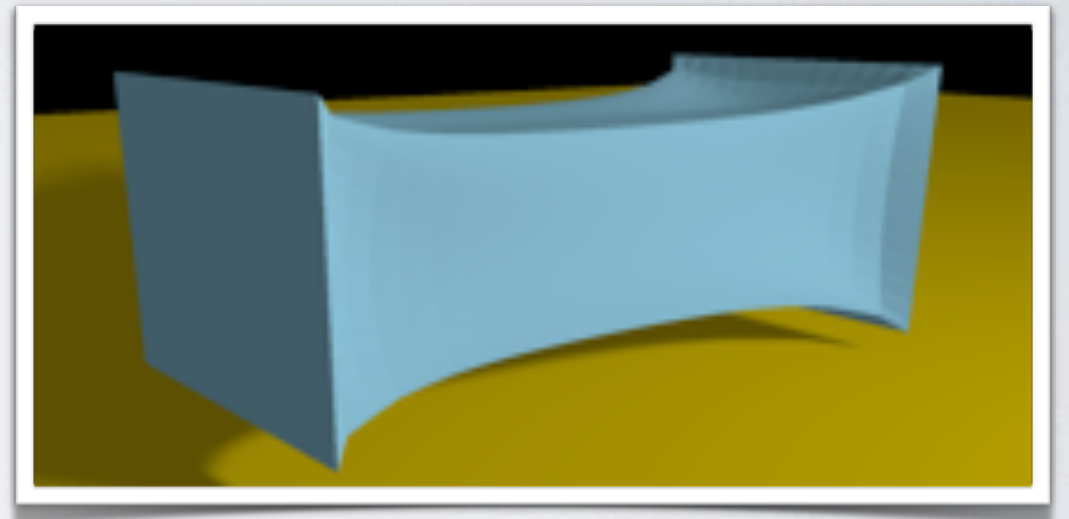
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INCOMPRESSIBILITY: MOTIVATION

Importance

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Importance

Increasing realism

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Importance

- Increasing realism

- Human flesh is incompressible

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Challenges

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- Do we really have true volume preservation?

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Linear elasticity

$$\Psi = \mu \|\epsilon\|_F^2 + \frac{\kappa}{2} \text{tr}^2(\epsilon)$$

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Corotated linear elasticity

$$\Psi = \mu \|\mathbf{F} - \mathbf{R}\|_F^2 + \frac{\kappa}{2} \text{tr}^2(\mathbf{S} - \mathbf{I})$$

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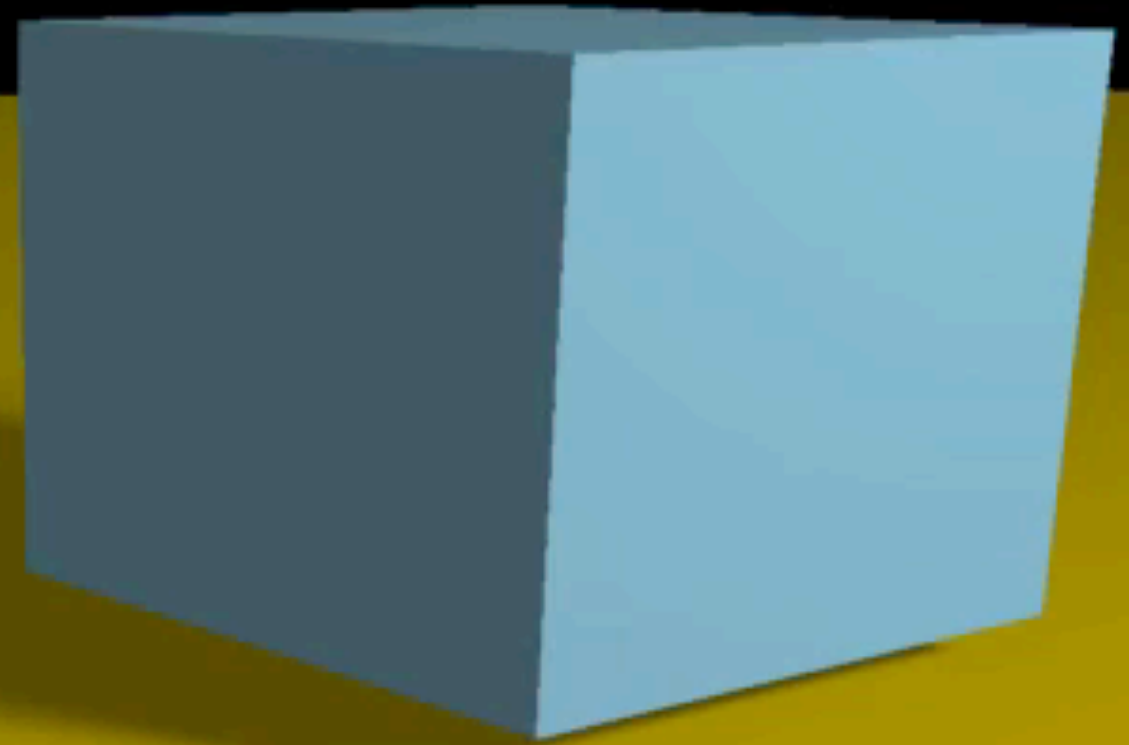
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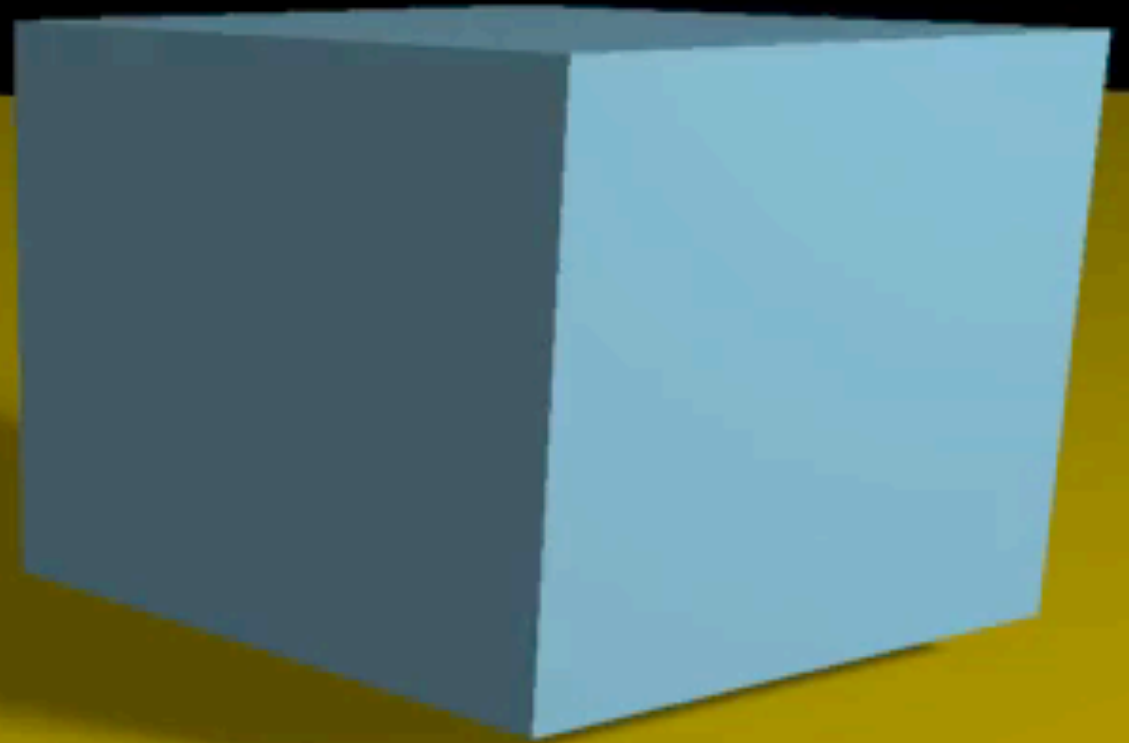
Raise κ to enforce incompressibility.

$$\kappa \rightarrow \infty$$

Implies complete incompressibility

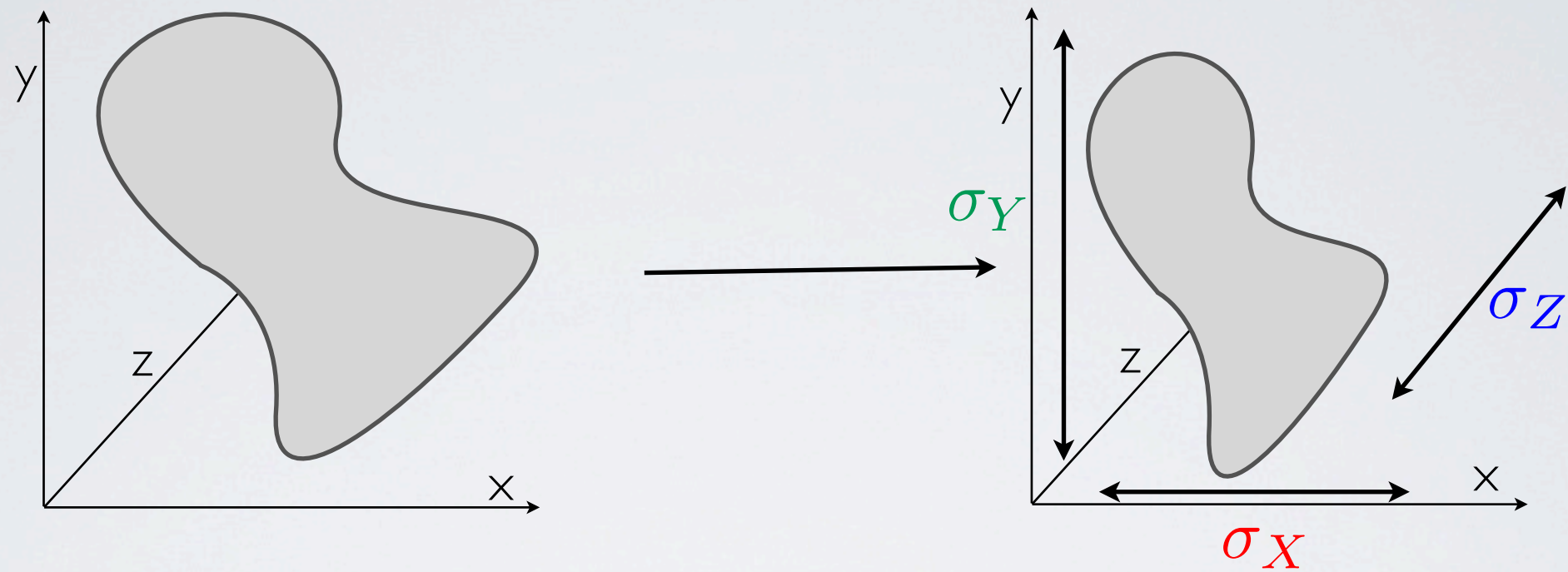


Corotated Linear Material - Inaccurate Volume Preservation

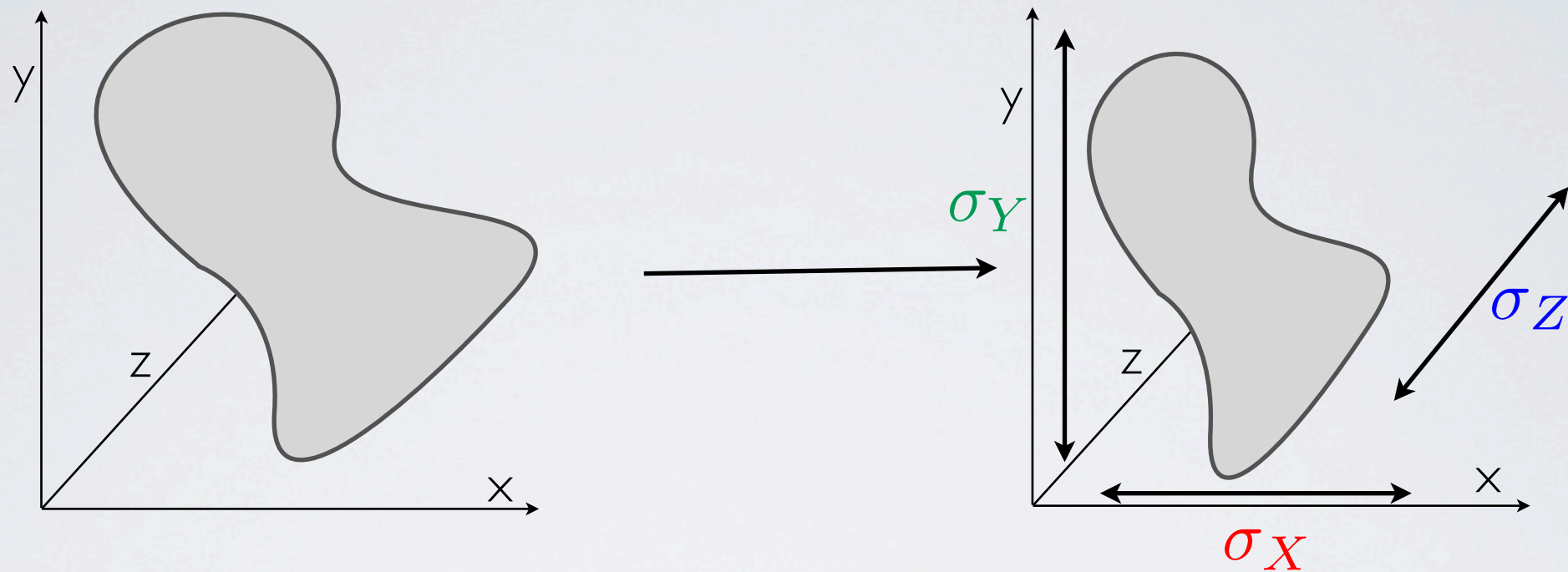


Neohookean Material - Accurate Volume Preservation

INCOMPRESSIBILITY: MATERIALS



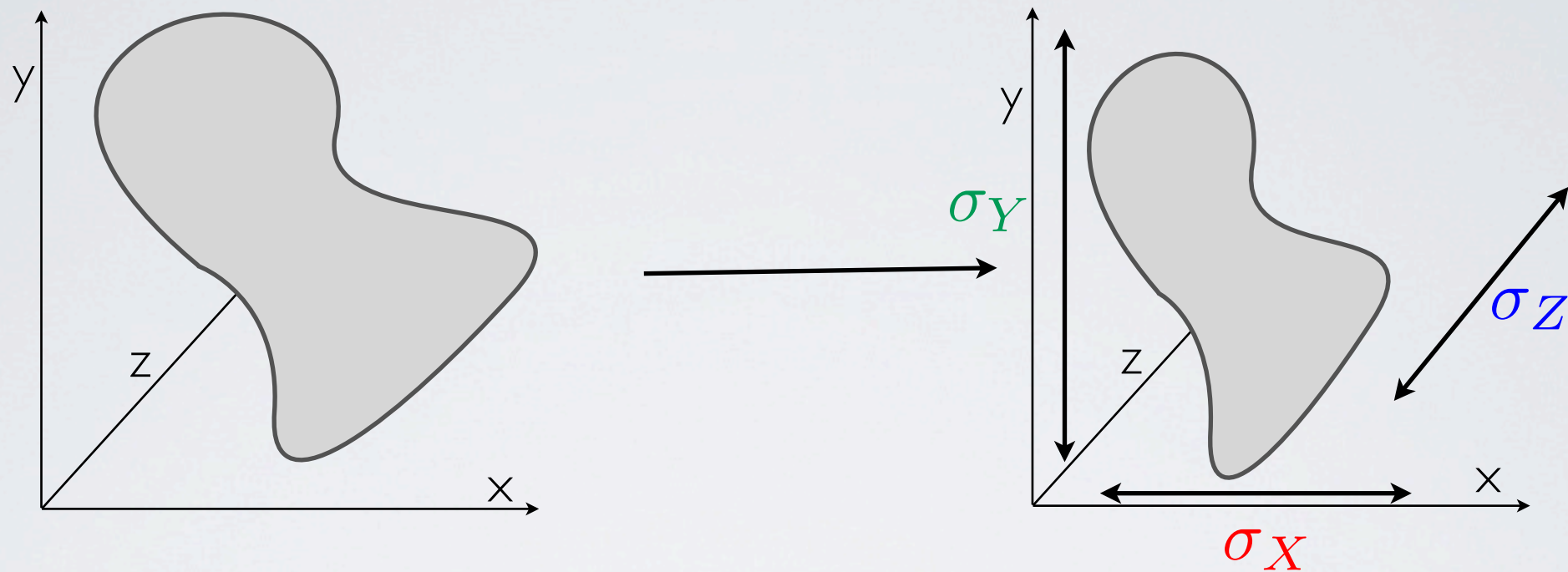
INCOMPRESSIBILITY: MATERIALS



Corotated linear elasticity

$$\text{tr}^2(S - I) = 0 \implies \frac{\sigma_X + \sigma_Y + \sigma_Z}{3} \approx 1$$

INCOMPRESSIBILITY: MATERIALS



Neohookean elasticity

$$\log^2(J) = 0 \implies \sigma_X \cdot \sigma_Y \cdot \sigma_Z \approx 1$$

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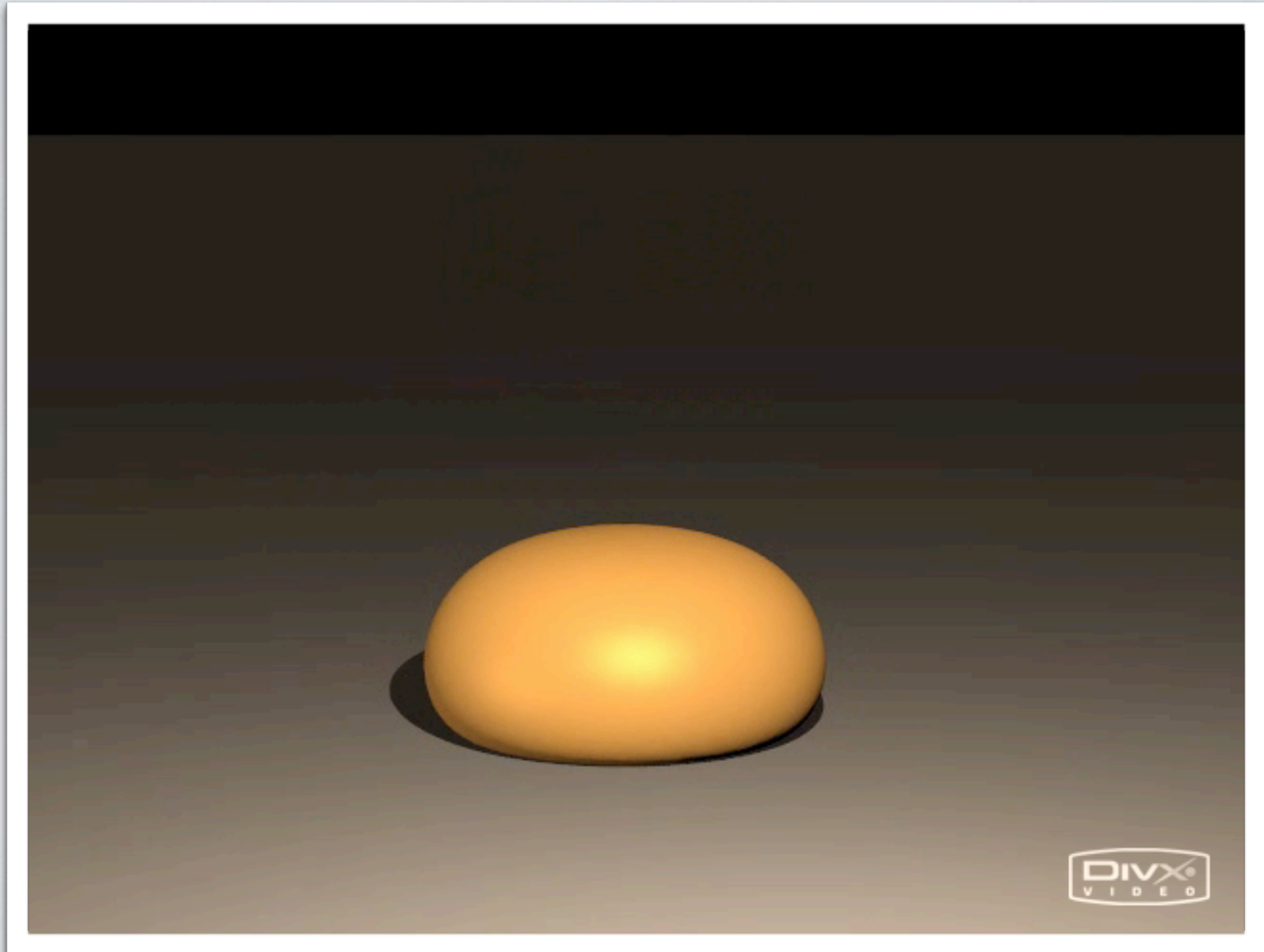
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INCOMPRESSIBILITY: LOCKING

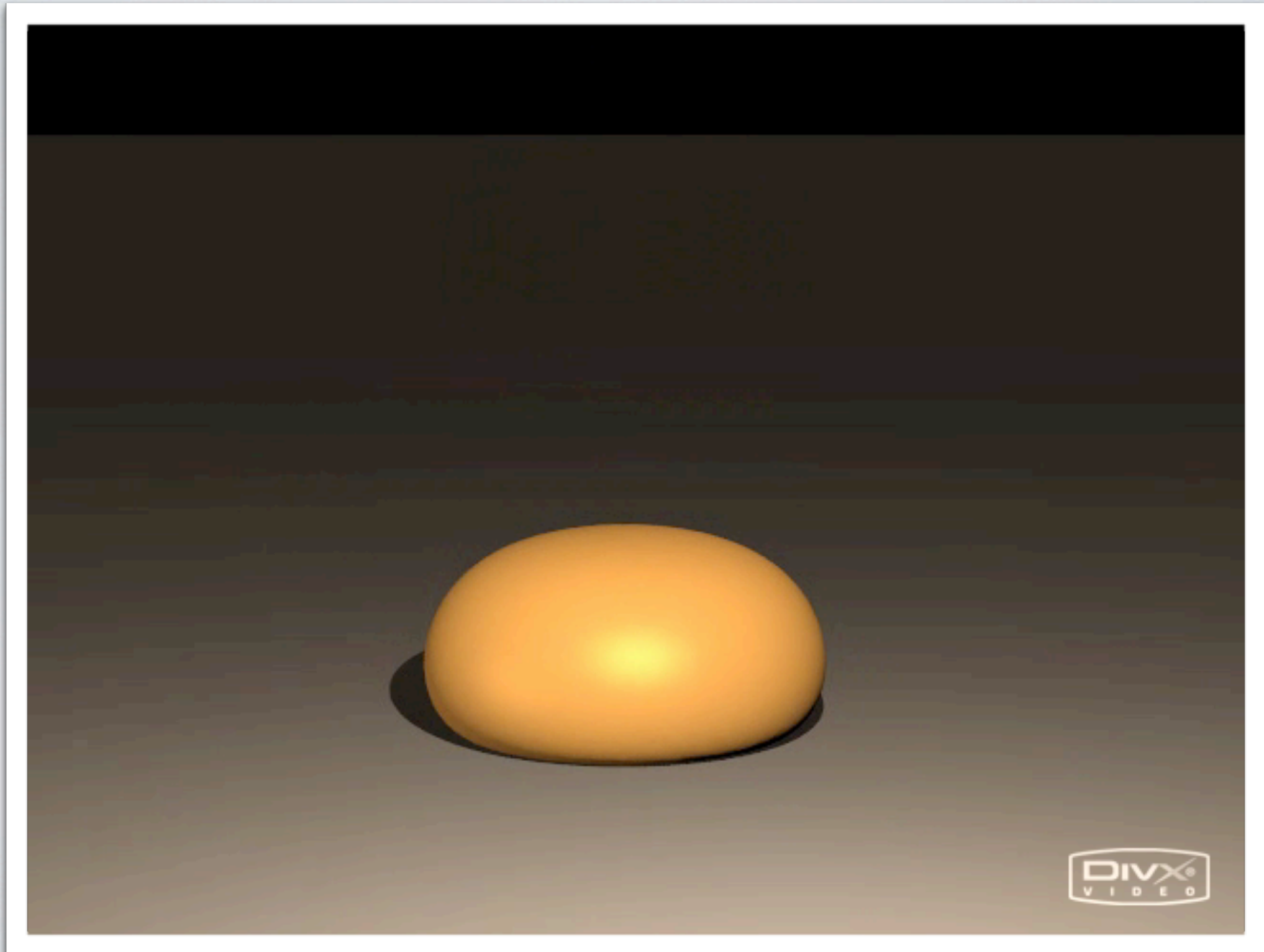
[Irving et al. 2007]

INCOMPRESSIBILITY: LOCKING



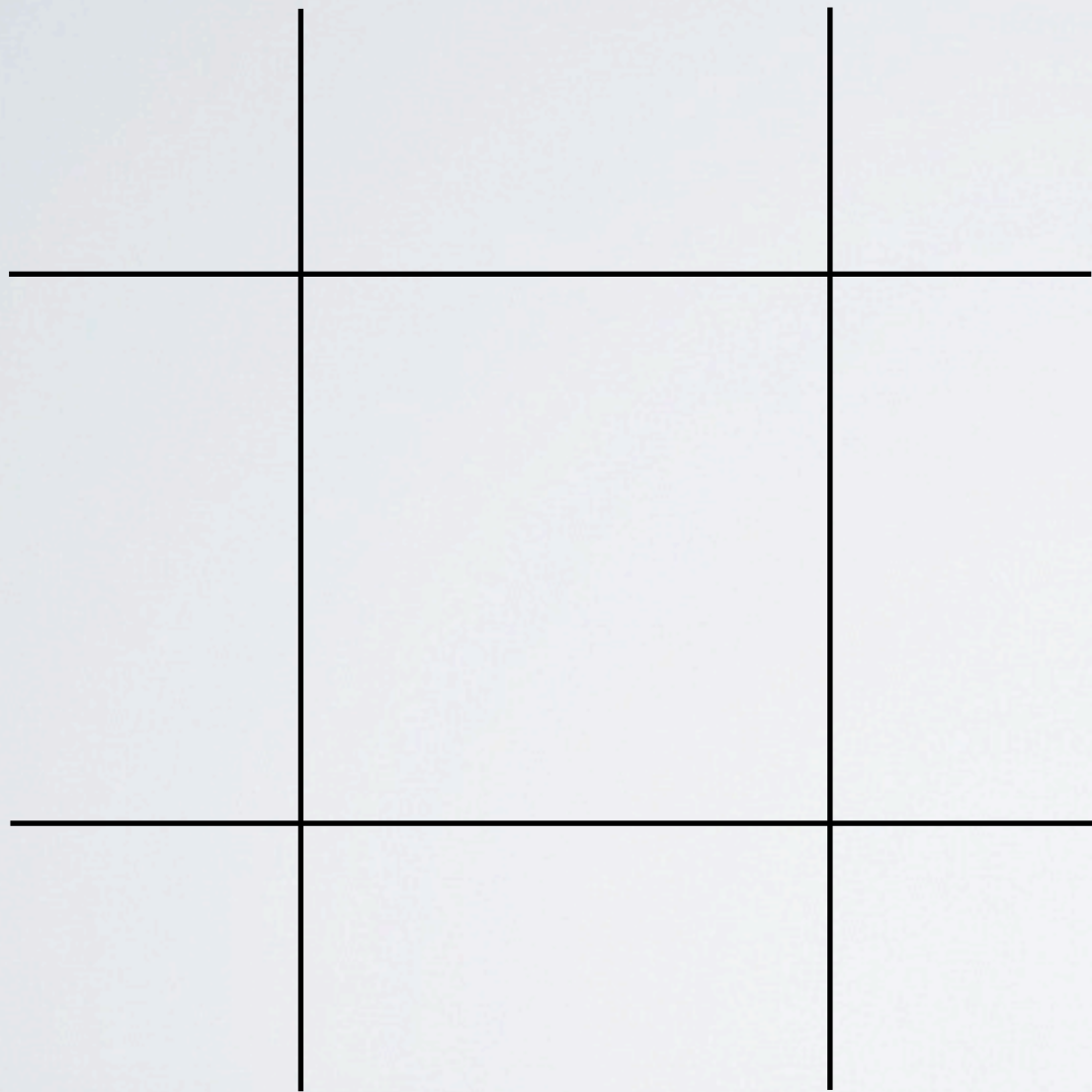
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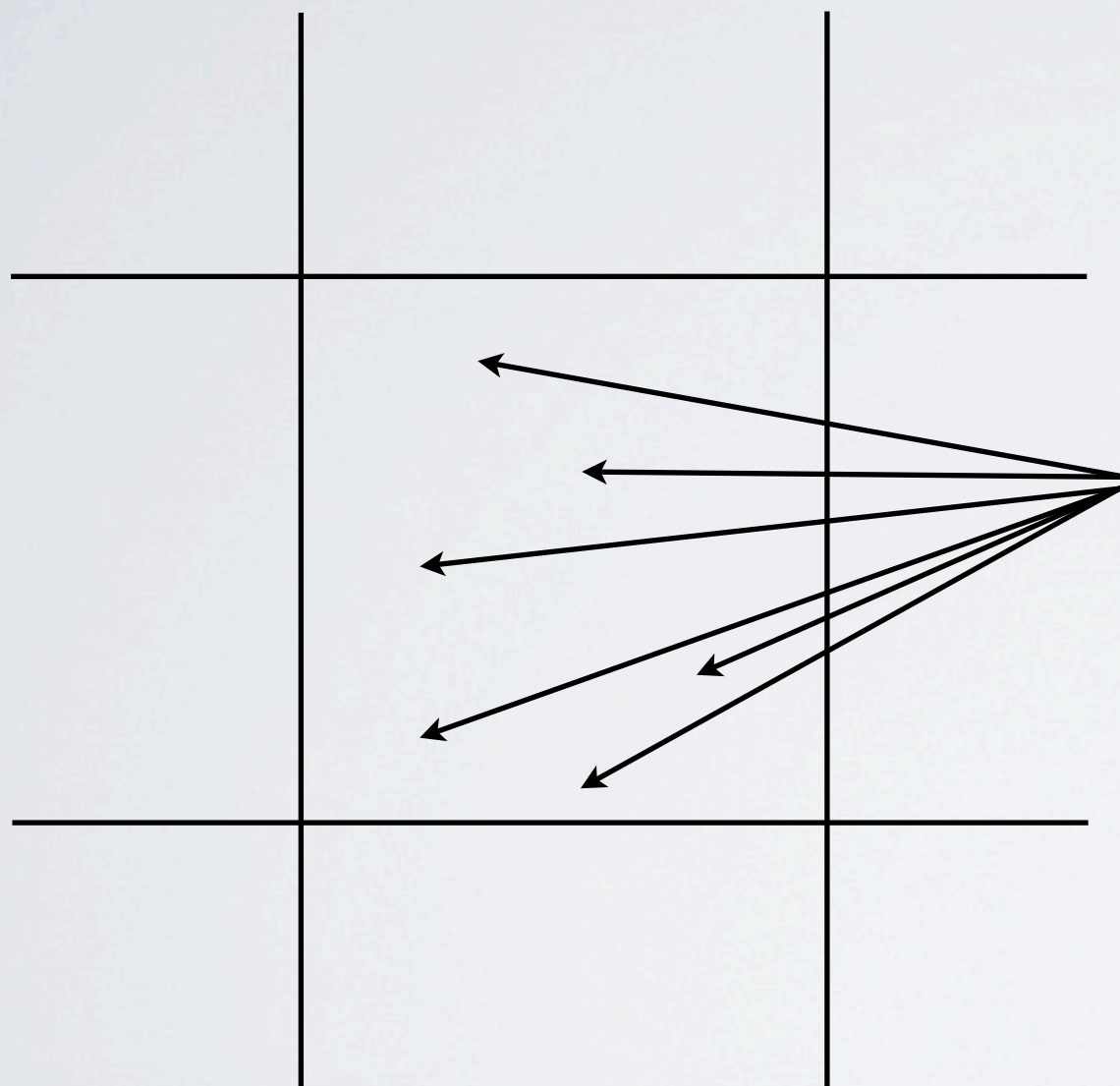
INCOMPRESSIBILITY: LOCKING



Elastic Energy

$$E = E_0 + \frac{\kappa}{2} \int_{\Omega} M^2(F) \delta X$$

INCOMPRESSIBILITY: LOCKING

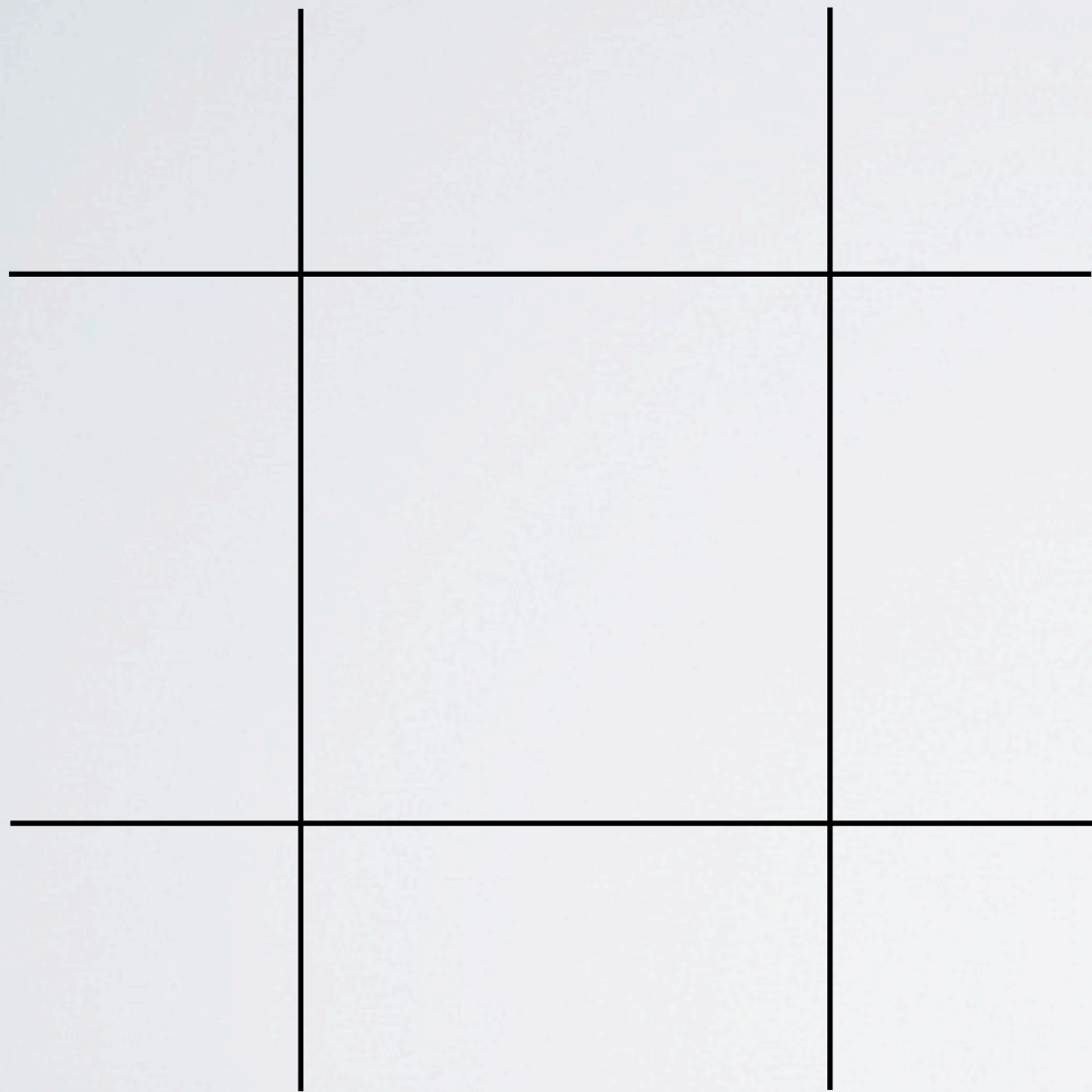


Require
Volume
Preservation
Everywhere

Elastic Energy

$$E = E_0 + \frac{\kappa}{2} \int_{\Omega} M^2(F) \delta X$$

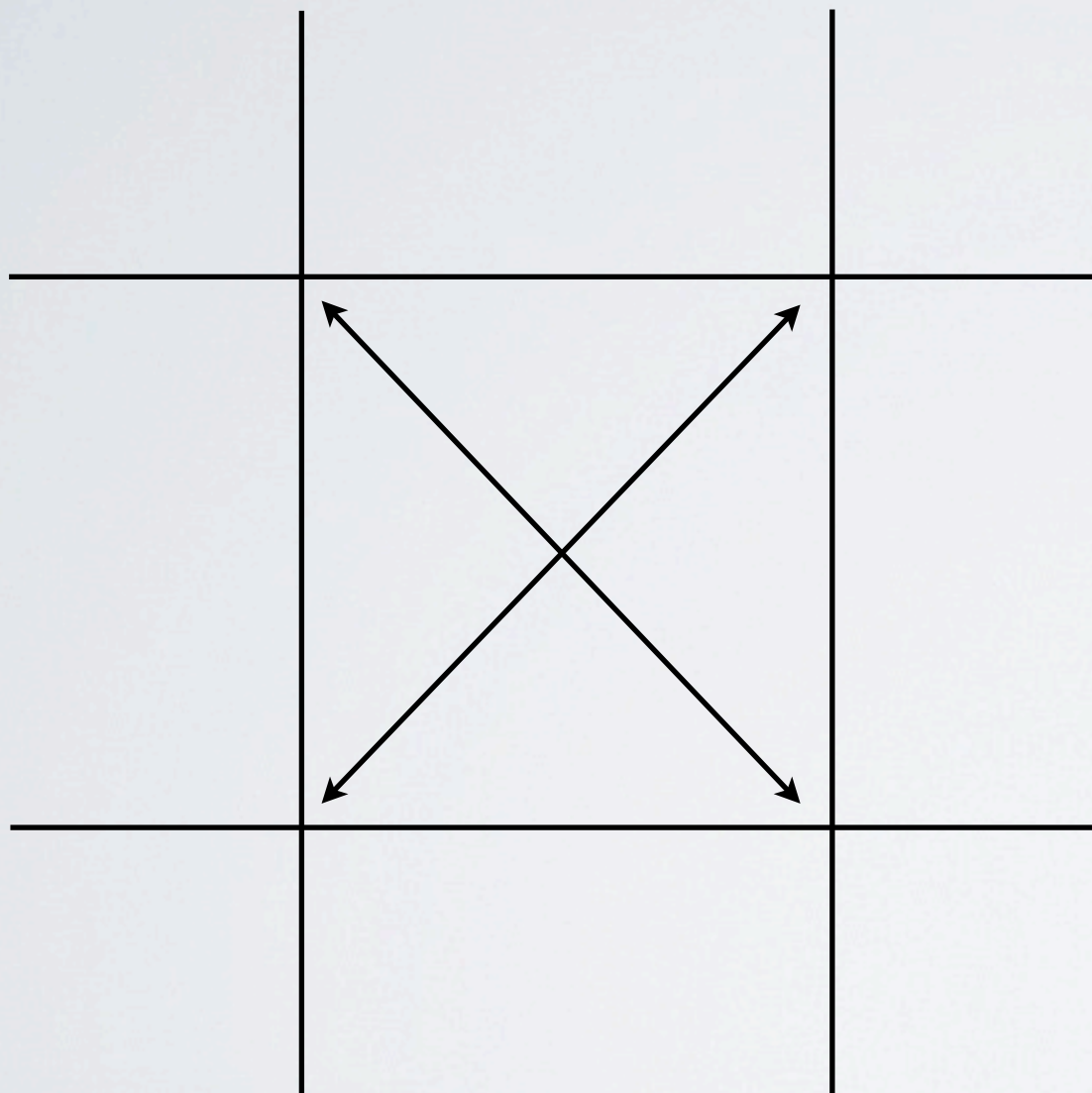
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Elastic Energy

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INCOMPRESSIBILITY: LOCKING



Require
Volume
Preservation
On Average

Elastic Energy

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INCOMPRESSIBILITY: CONDITIONING

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Apply Incompressibility Adjustment



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INCOMPRESSIBILITY: CONDITIONING

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No internal forces implies equilibrium after deformation

INCOMPRESSIBILITY: CONDITIONING

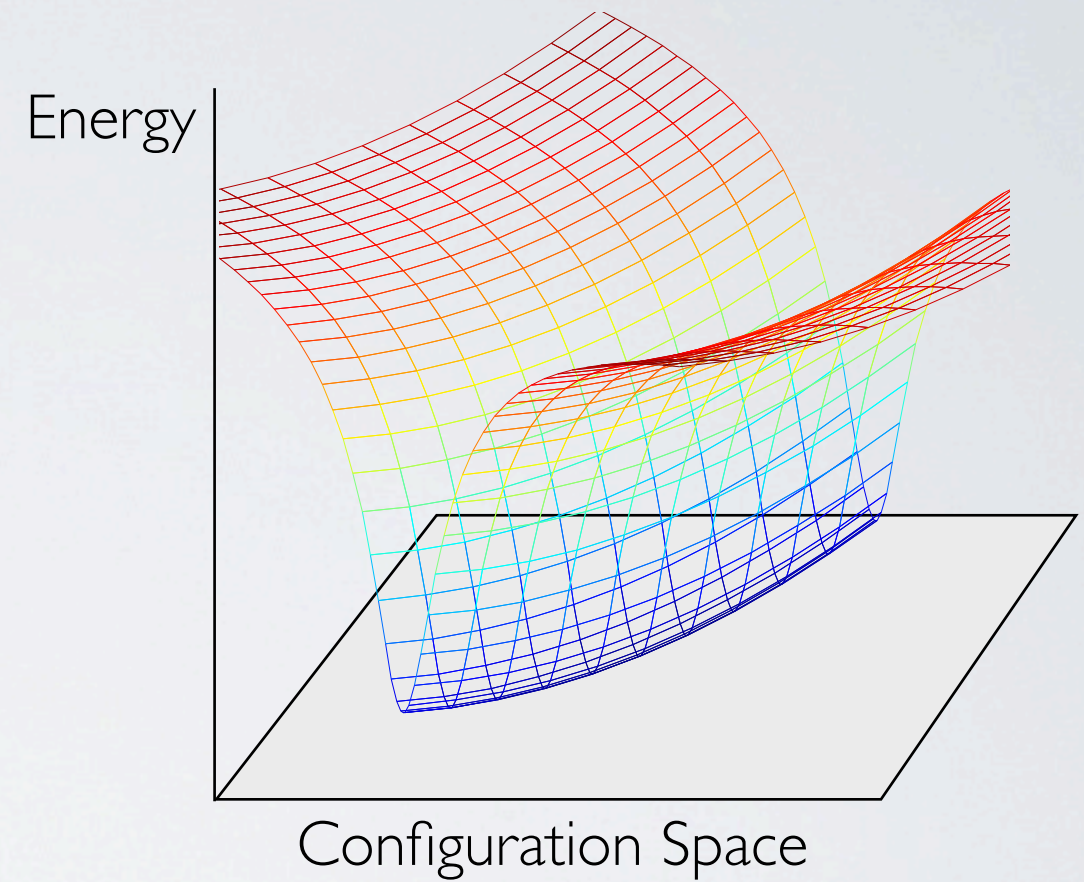
Find Equilibrium $f(x) = 0 \implies \min \hat{E}$

No internal forces implies equilibrium after deformation

Zero forces implies a minimum in the potential energy

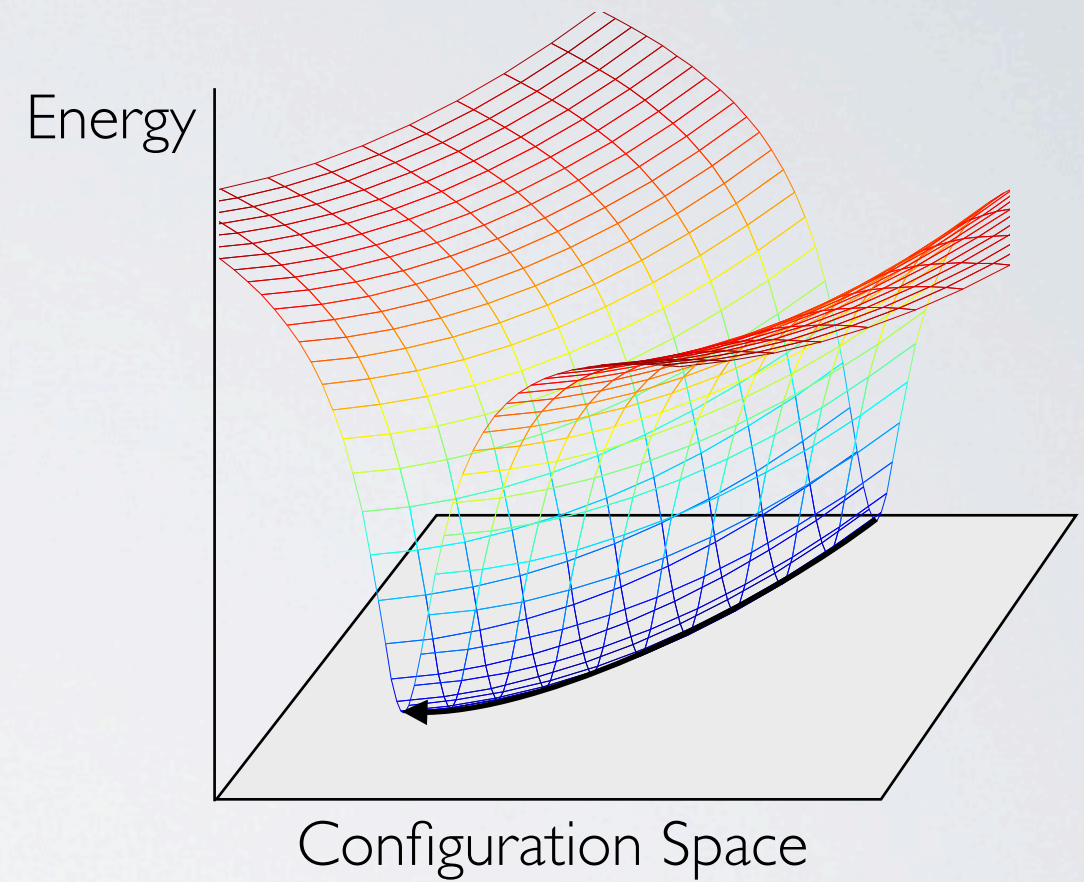
INCOMPRESSIBILITY: CONDITIONING

$$\Psi(F) = \Psi_0 + \frac{\kappa}{2} \overline{M}^2(F)$$



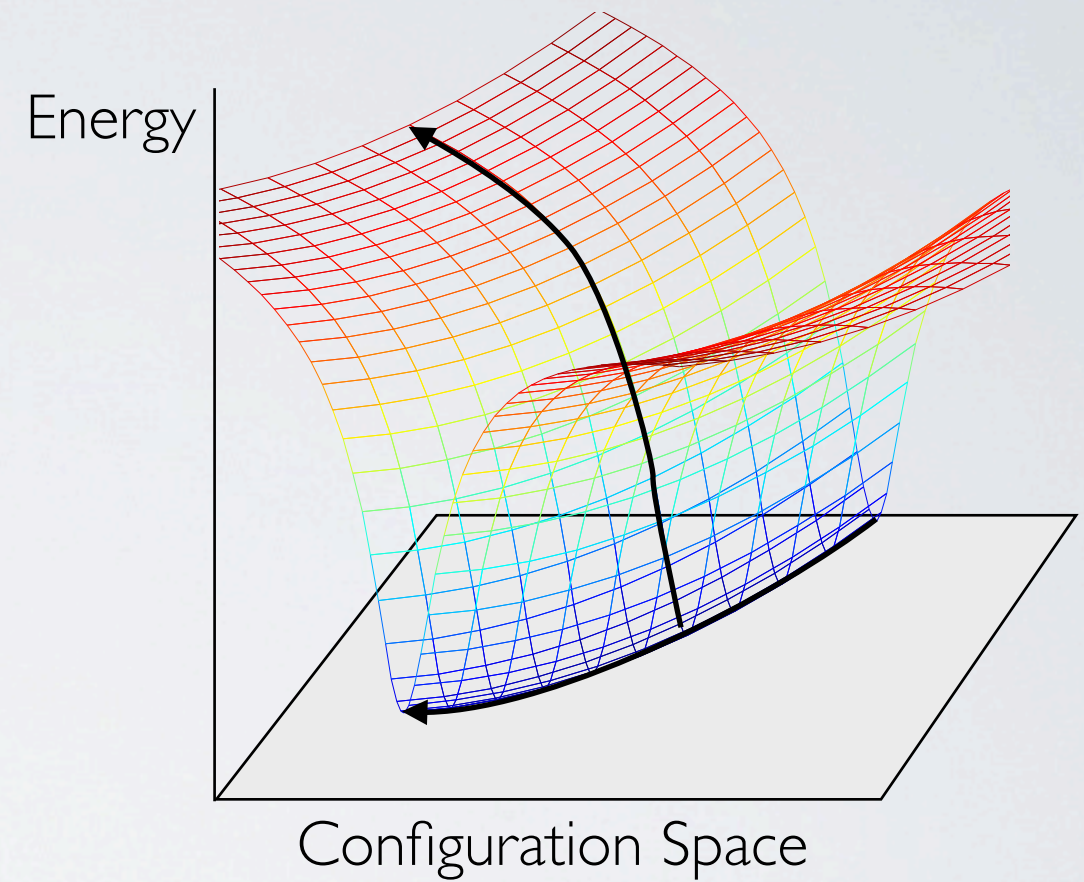
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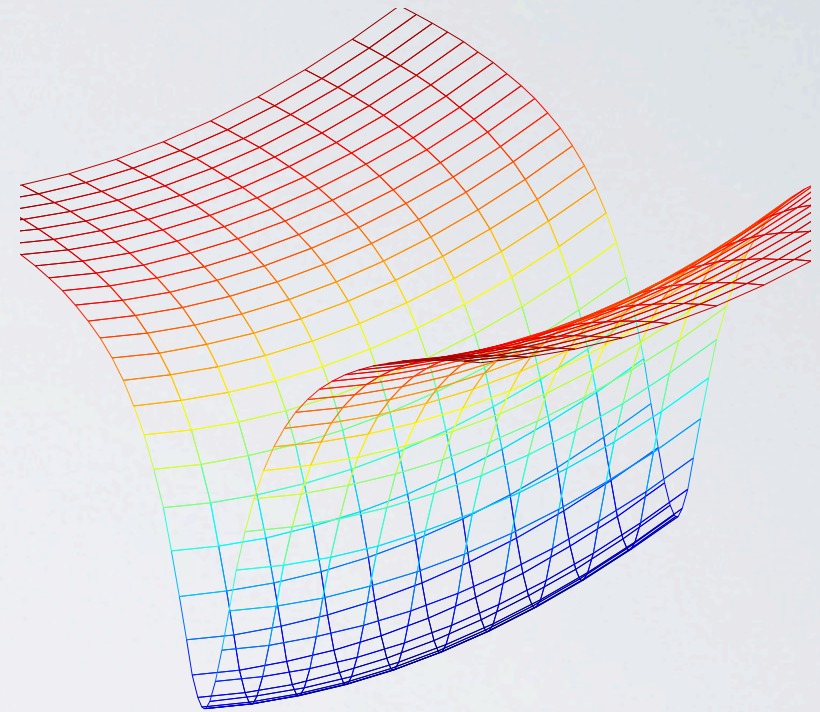
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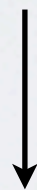
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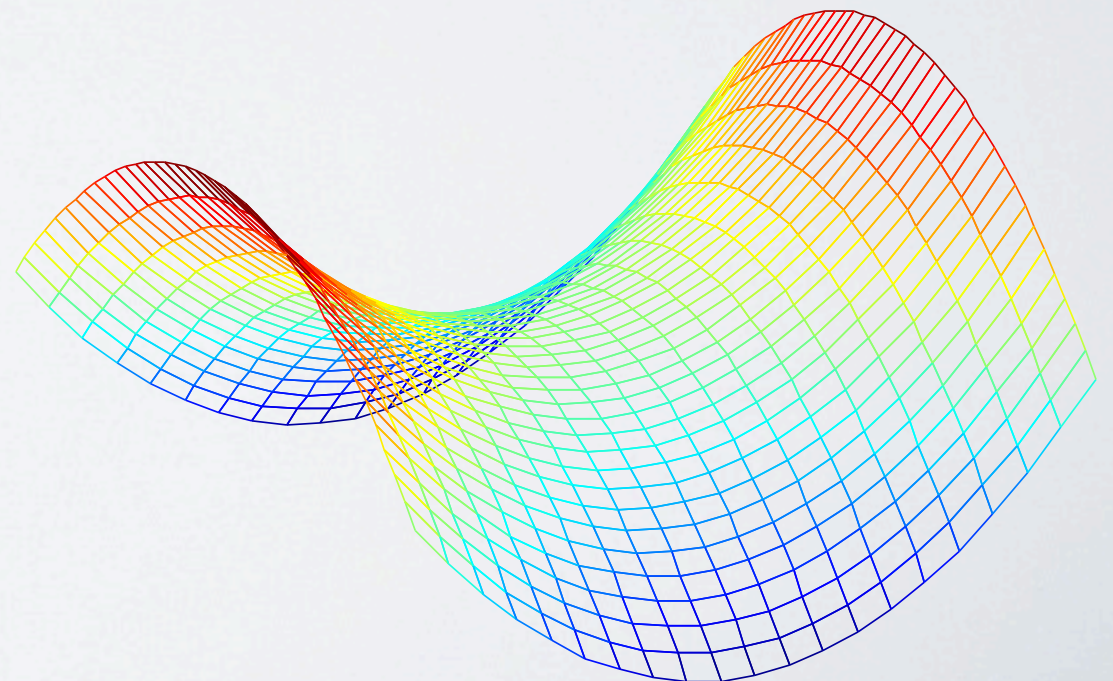
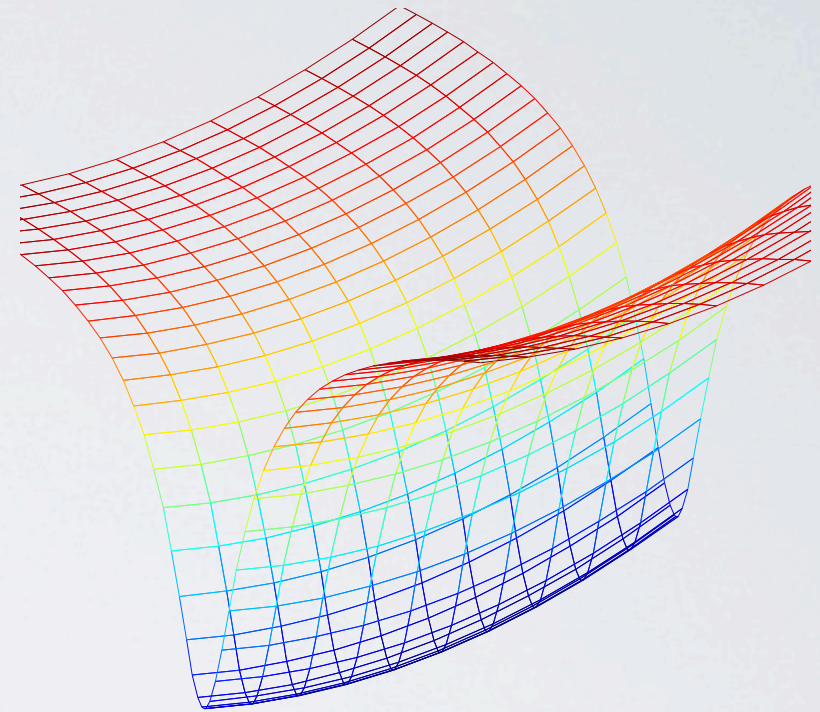


INCOMPRESSIBILITY: CONDITIONING

$$\Psi(F) = \Psi_0 + \frac{\kappa}{2} \overline{M}^2(F)$$



$$\Psi(F, p) = \Psi_0(F) + \alpha p \overline{M}(F) - \frac{\alpha^2 p^2}{2\kappa}$$

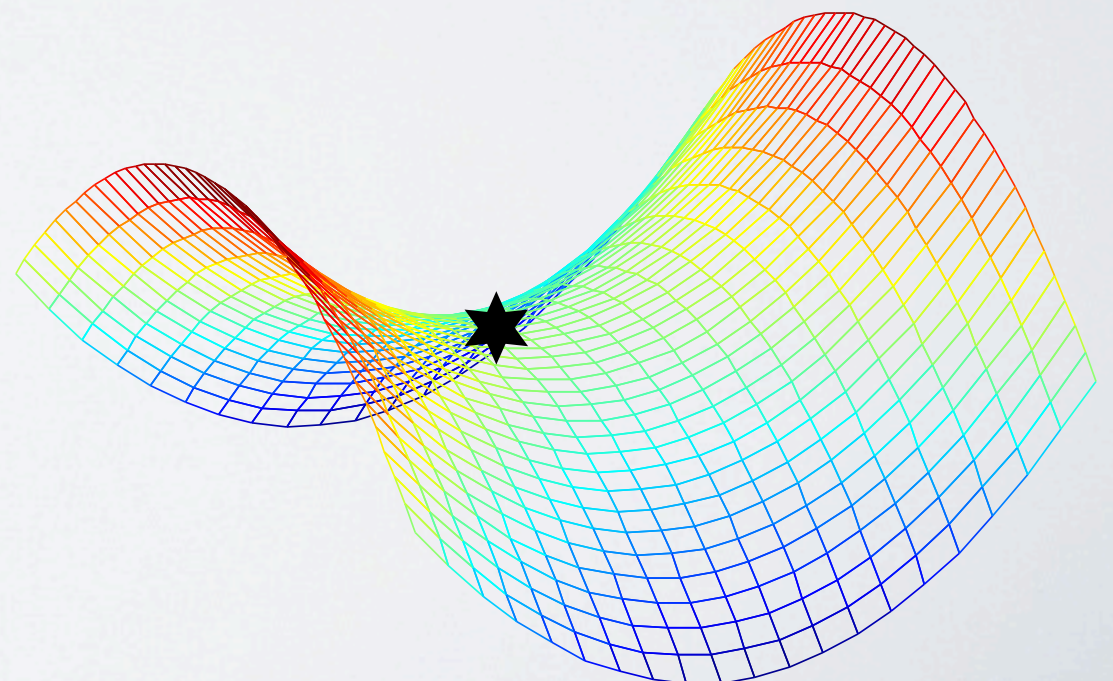
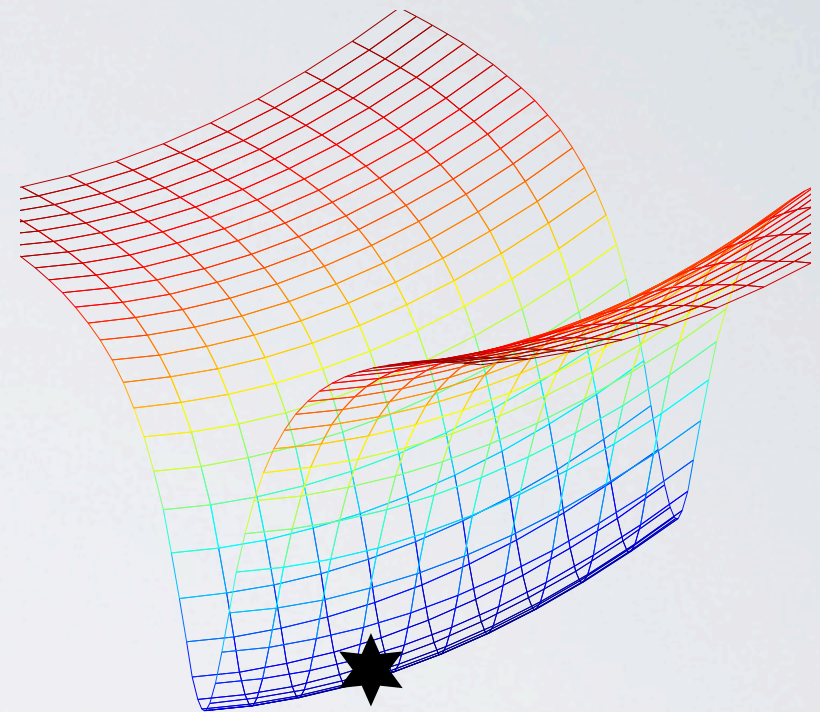


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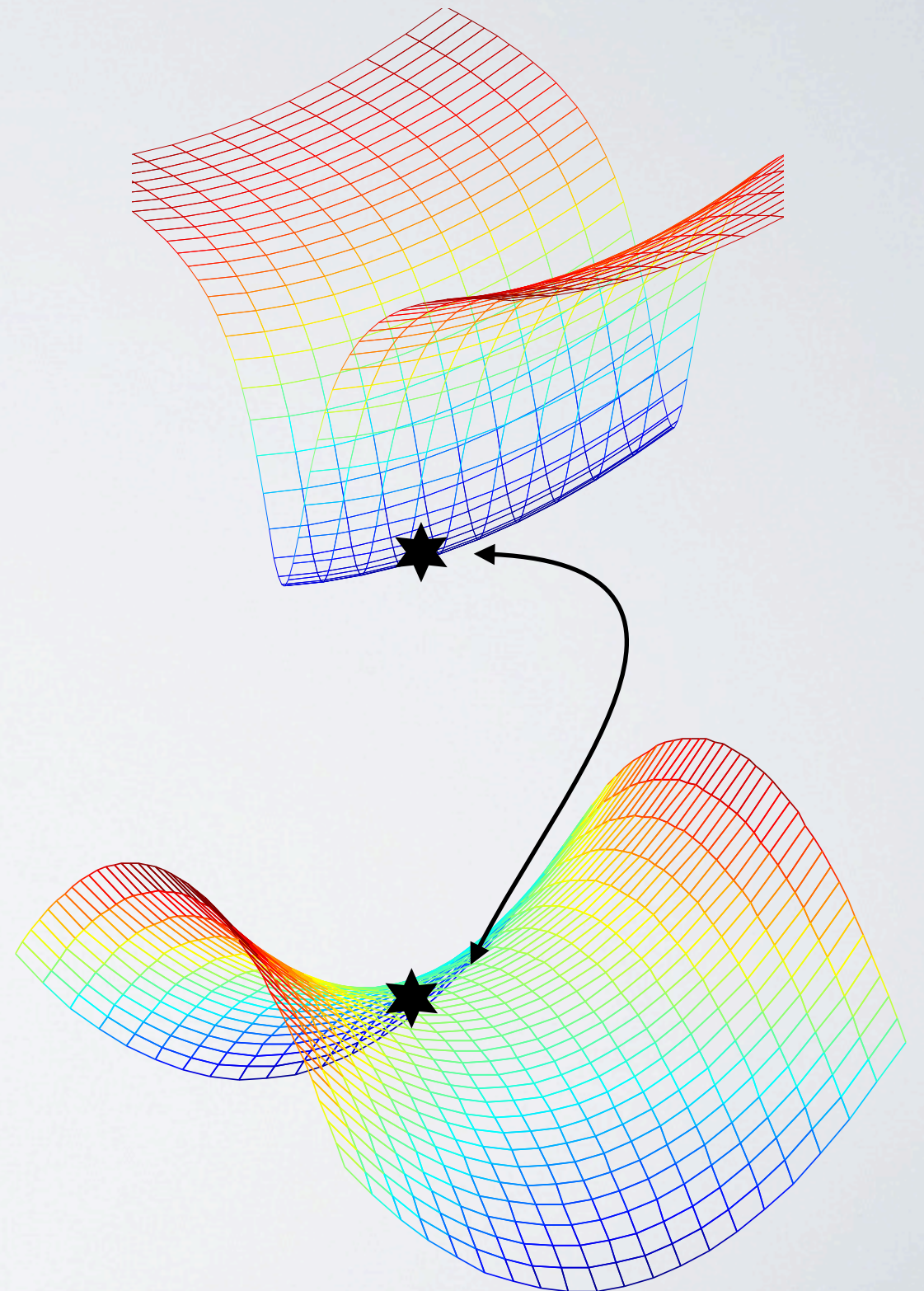


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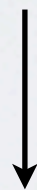


$$\Psi(F, p) = \Psi_0(F) + \alpha p \overline{M}(F) - \frac{\alpha^2 p^2}{2\kappa}$$

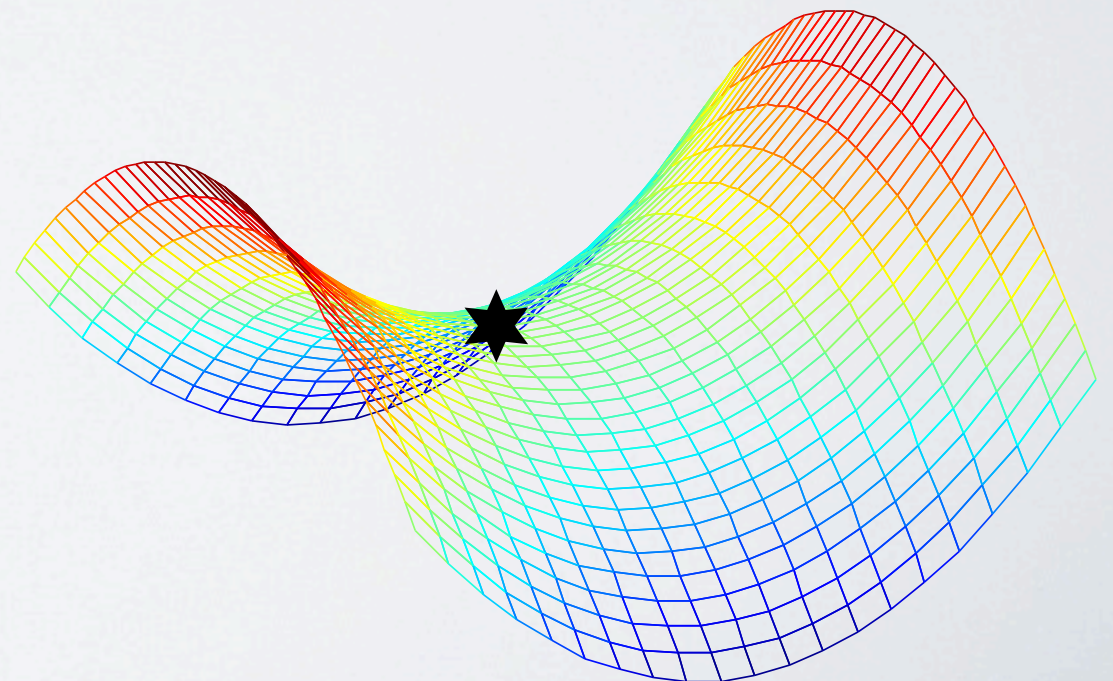
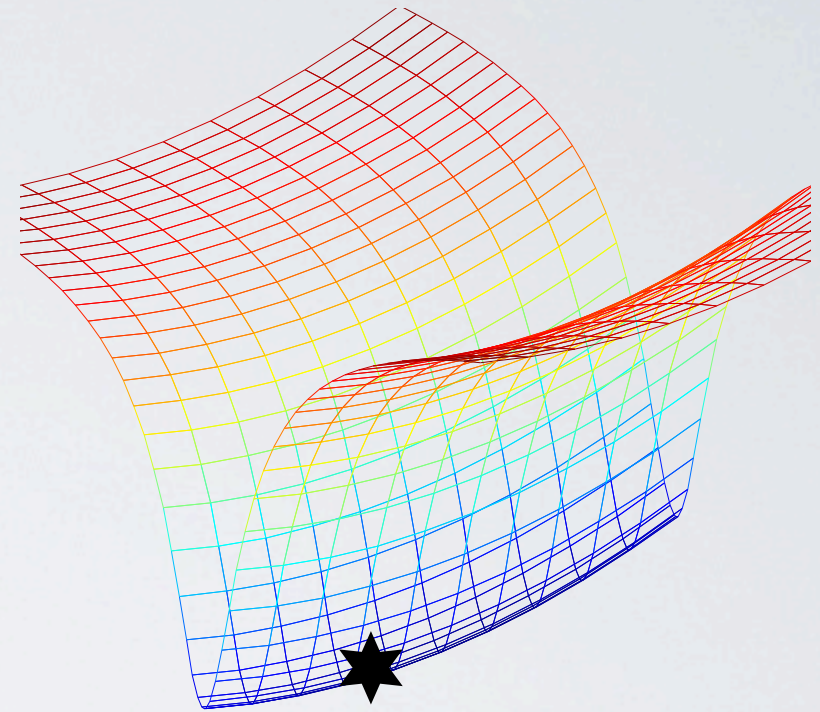


INCOMPRESSIBILITY: CONDITIONING

$$\Psi(F) = \Psi_0 + \frac{\kappa}{2} \overline{M}^2(F)$$

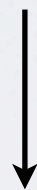


$$\Psi(F, p) = \Psi_0(F) + \alpha p \overline{M}(F) - \frac{\alpha^2 p^2}{2\kappa}$$

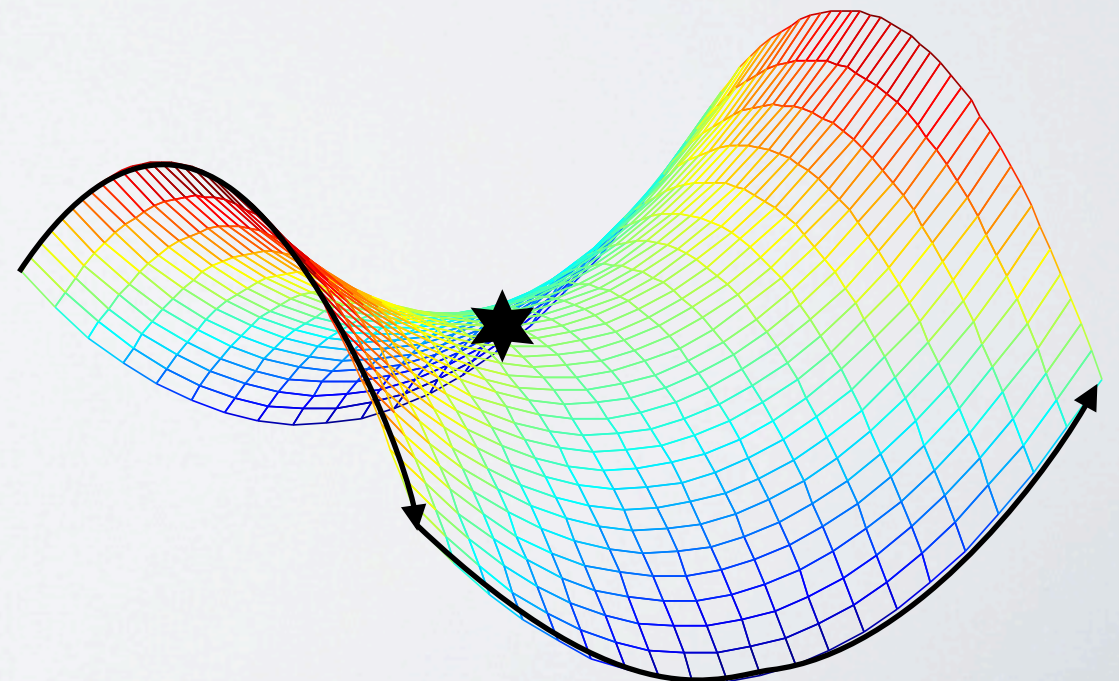
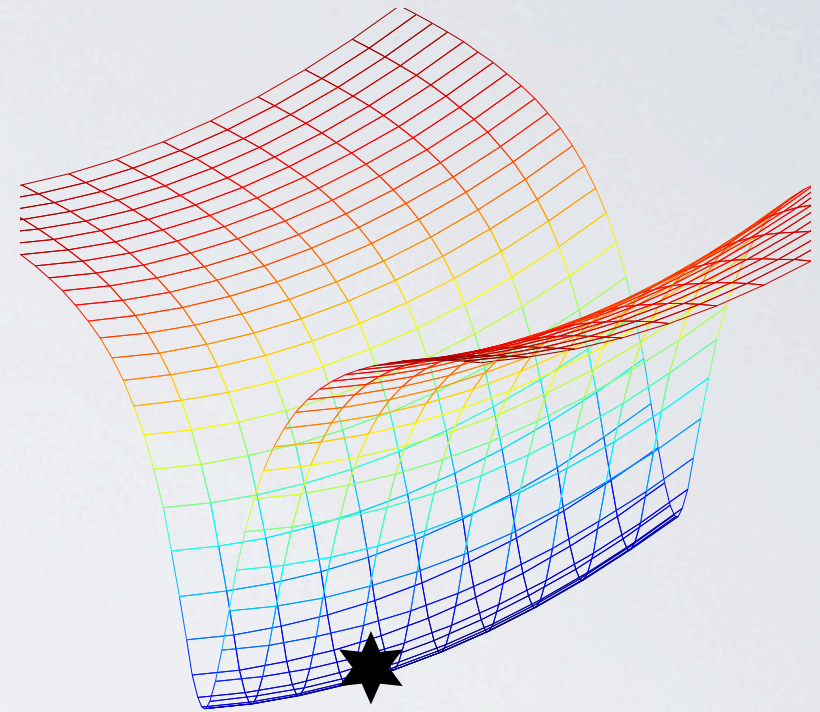


INCOMPRESSIBILITY: CONDITIONING

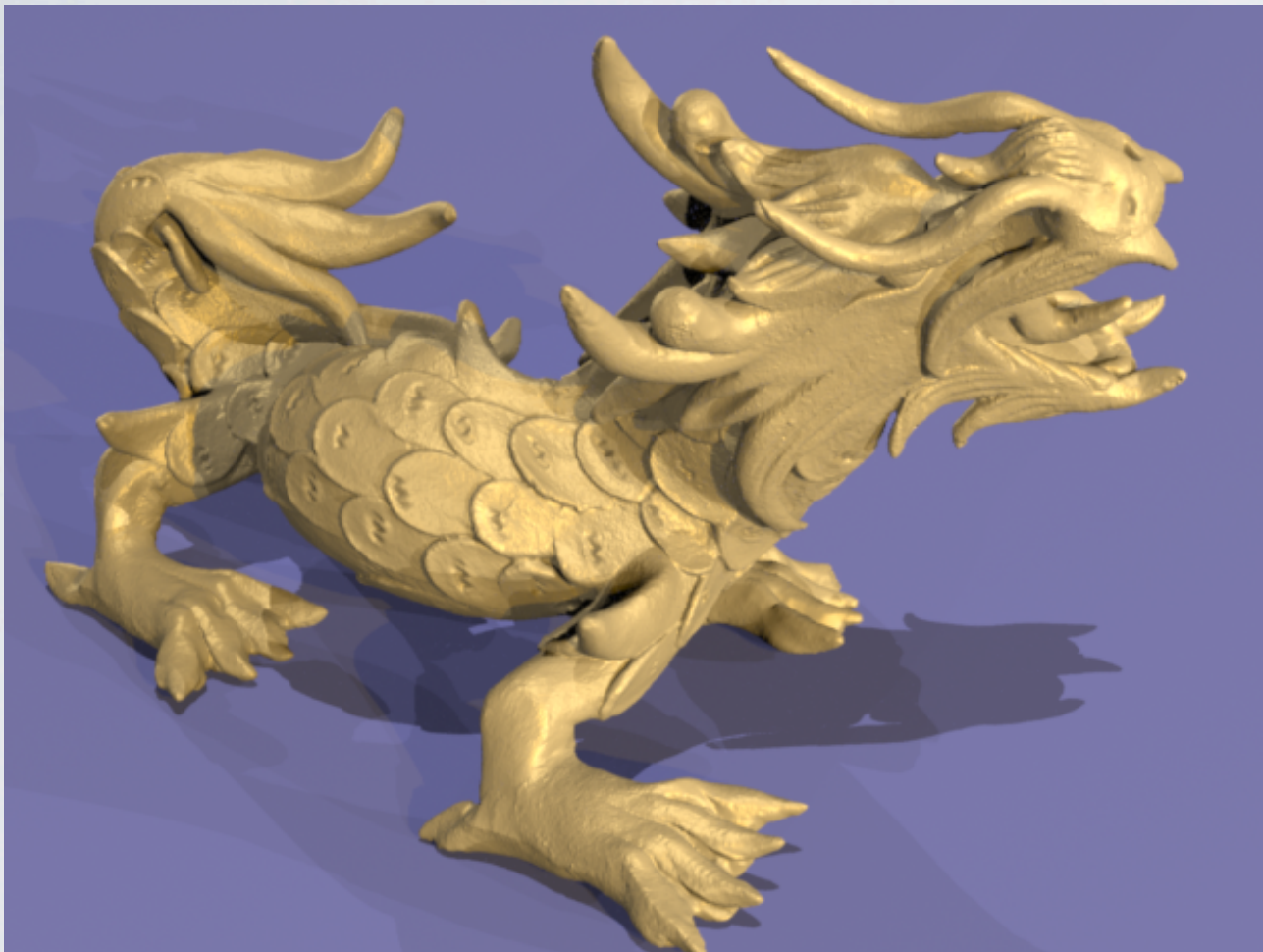
$$\Psi(F) = \Psi_0 + \frac{\kappa}{2} \overline{M}^2(F)$$



$$\Psi(F, p) = \Psi_0(F) + \alpha p \overline{M}(F) - \frac{\alpha^2 p^2}{2\kappa}$$



INCOMPRESSIBILITY: CONDITIONING



[Zhu et al. 2010]

Implemented at PDE level

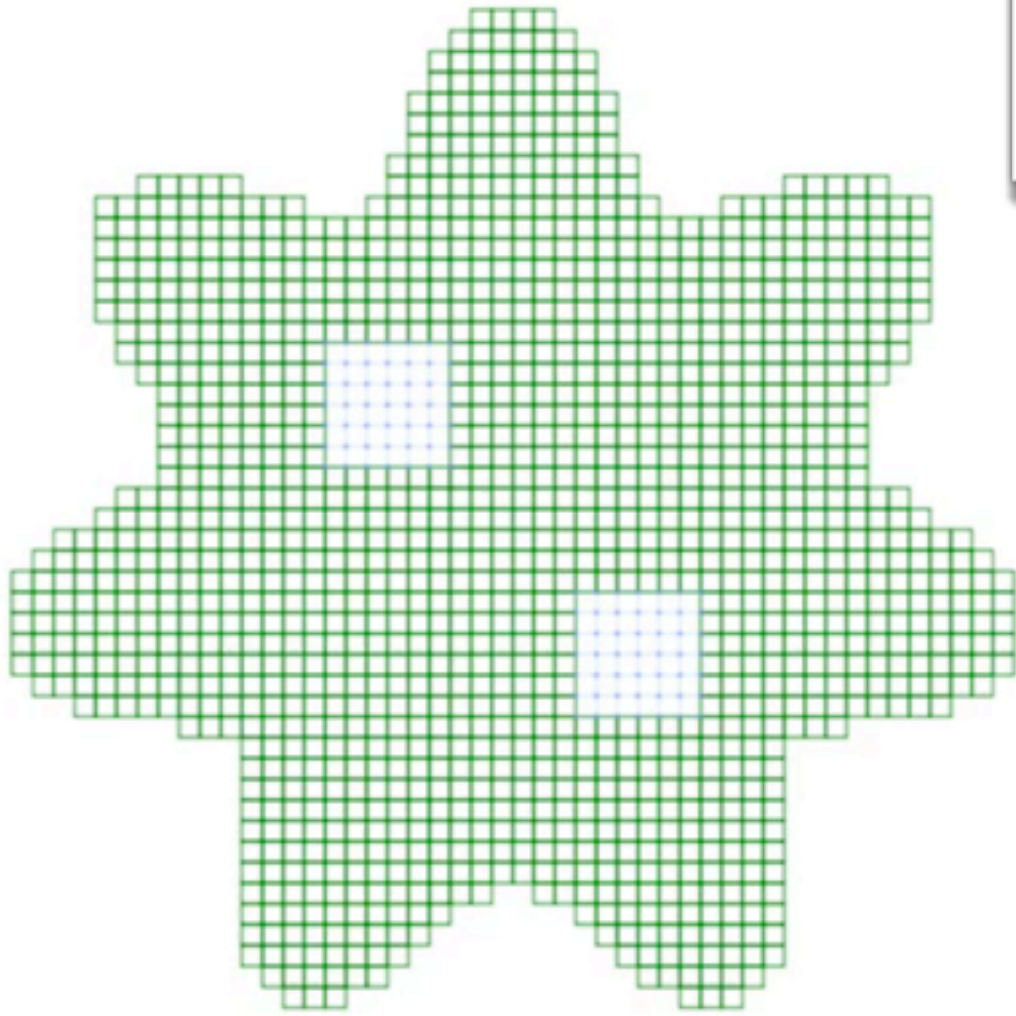
More flexibility at energy level

Limited set of materials

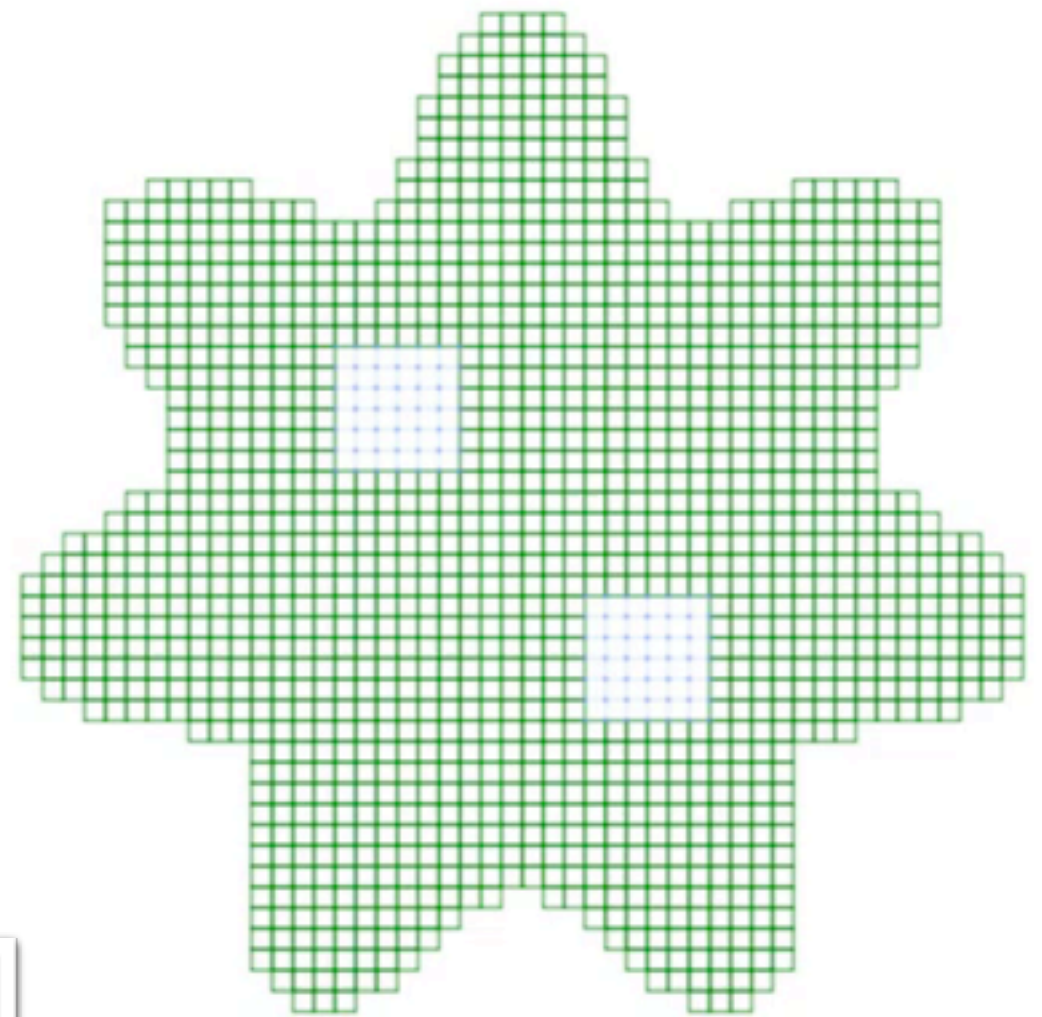
Using conventional
minimization formulation

Using saddle
point formulation

Using conventional
minimization formulation



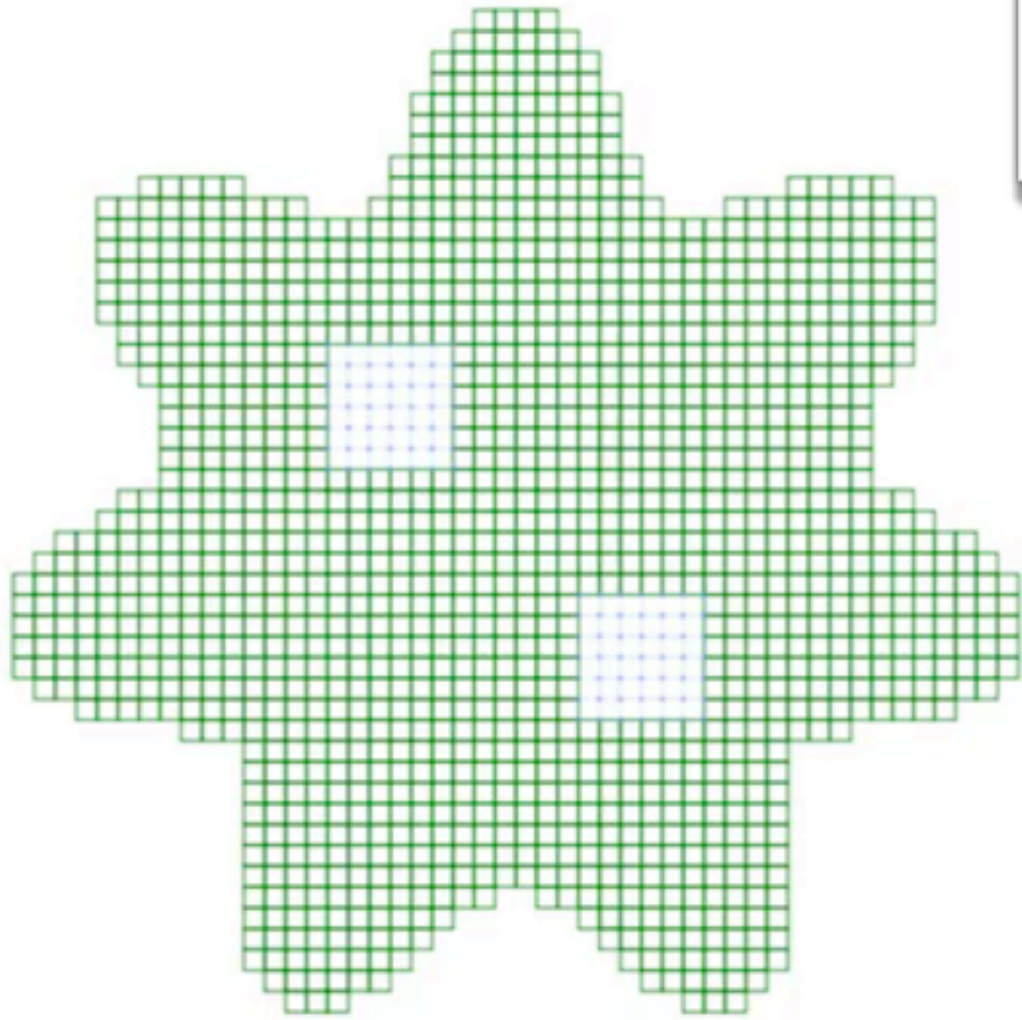
Using saddle
point formulation



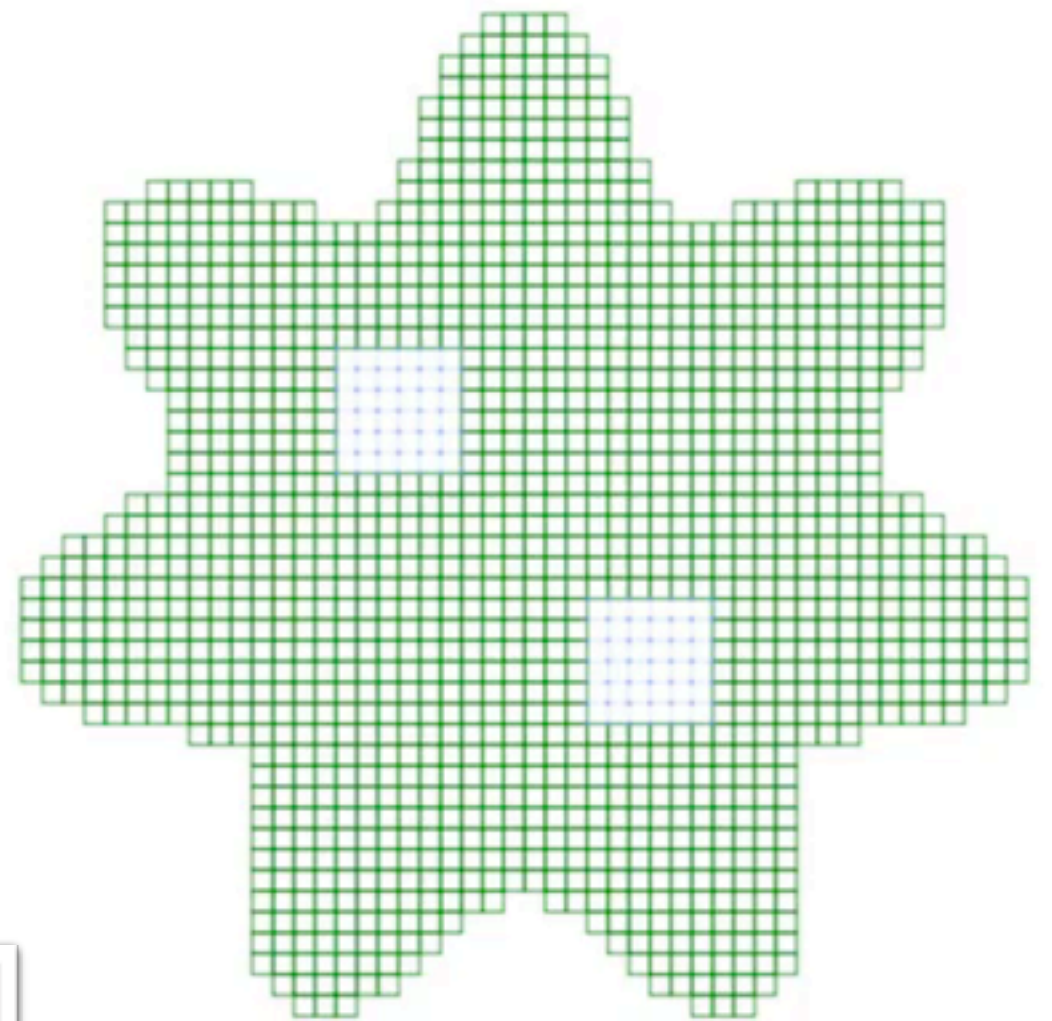
Using conventional
minimization formulation

Using saddle
point formulation

Using conventional
minimization formulation



Using saddle
point formulation



FEATURES

Arbitrary Materials

Incompressibility

Sub-voxel Precision

Robust

Parallelism

FEATURES

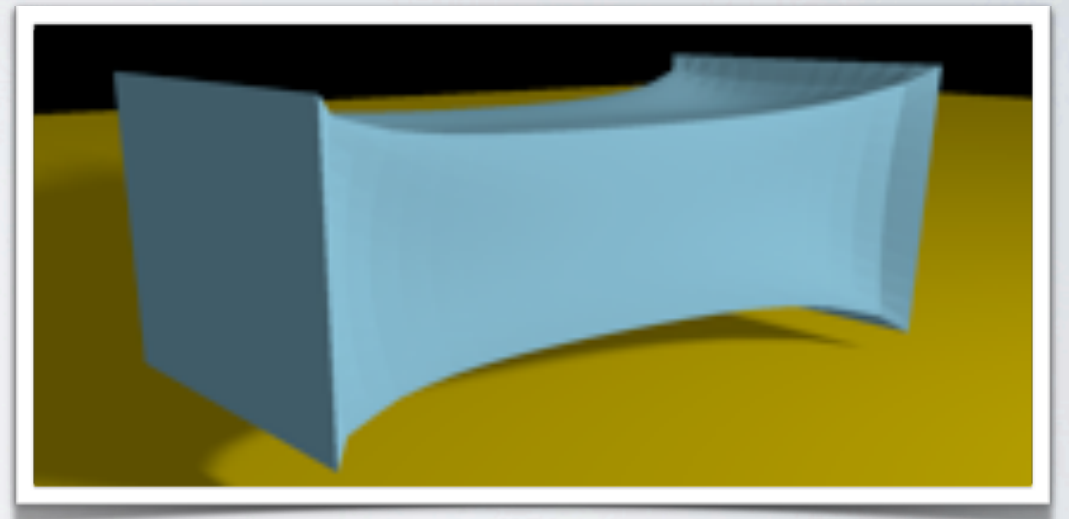
Arbitrary Materials

Incompressibility

Sub-voxel Precision

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Parallelism



FEATURES

Arbitrary Materials



Incompressibility

Sub-voxel Precision

Robust

Parallelism

FEATURES

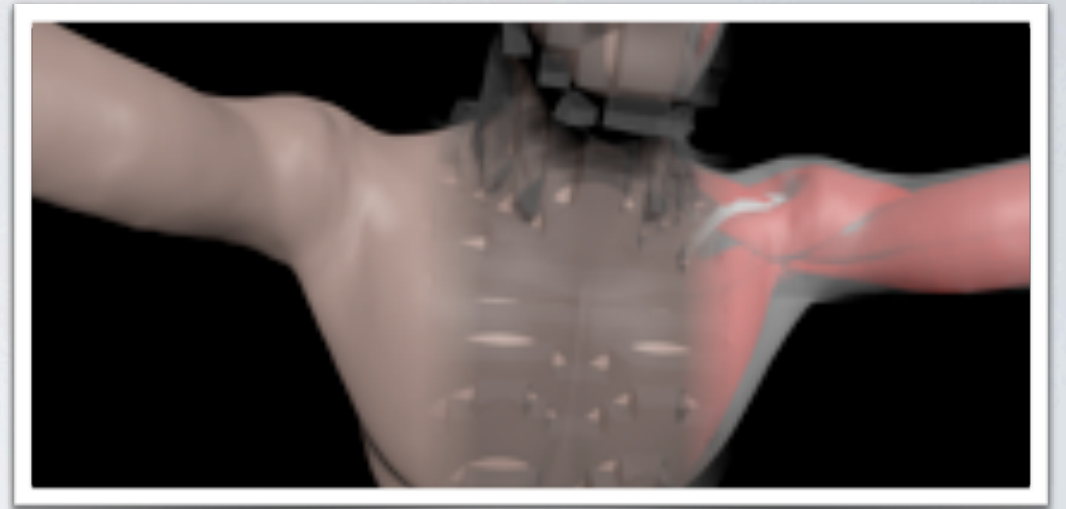
Arbitrary Materials

✓ Incompressibility

Sub-voxel Precision

Robust

Parallelism



FEATURES

✓ Arbitrary Materials

✓ Incompressibility

Sub-voxel Precision

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Parallelism

FEATURES

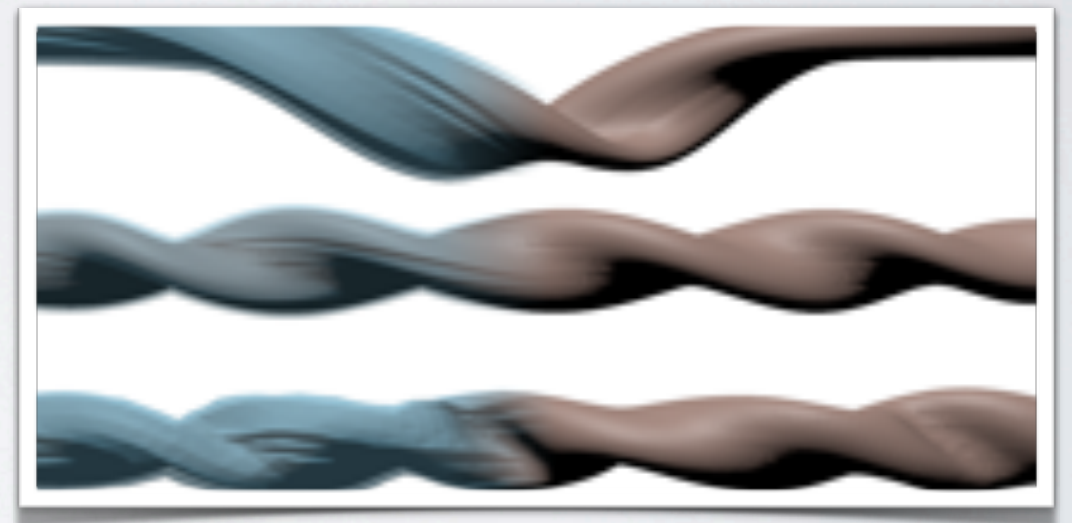
✓ Arbitrary Materials

✓ Incompressibility

Sub-voxel Precision

Robust

Parallelism



BOUNDARY CELLS

Start with Energy Density



Apply Incompressibility Adjustment



Compute Discrete Energy \hat{E}



Derive Nodal Forces $f(x)$



Find Equilibrium $f(x) = 0 \implies \min \hat{E}$

BOUNDARY CELLS

Compute Discrete Energy \hat{E}



Derive Nodal Forces $f(x)$

Boundary Cell Treatment

BOUNDARY CELLS: MOTIVATION

Importance

BOUNDARY CELLS: MOTIVATION

Importance

Objects are not made of cubes

BOUNDARY CELLS: MOTIVATION

Importance

Objects are not made of cubes

Visible grid artifacts (discontinuities)

BOUNDARY CELLS: MOTIVATION

Importance

Objects are not made of cubes

~~Visible grid artifacts (discontinuities)~~

Interpolation
discontinuities can be
avoided by using
tricubic interpolation

BOUNDARY CELLS: MOTIVATION

Importance

Objects are not made of cubes

~~Visible grid artifacts (discontinuities)~~

Challenges

BOUNDARY CELLS: MOTIVATION

Importance

Objects are not made of cubes

~~Visible grid artifacts (discontinuities)~~

Challenges

How accurate are we?

BOUNDARY CELLS: MOTIVATION

Importance

Objects are not made of cubes

~~Visible grid artifacts (discontinuities)~~

Challenges

How accurate are we?

Can we make it go fast?

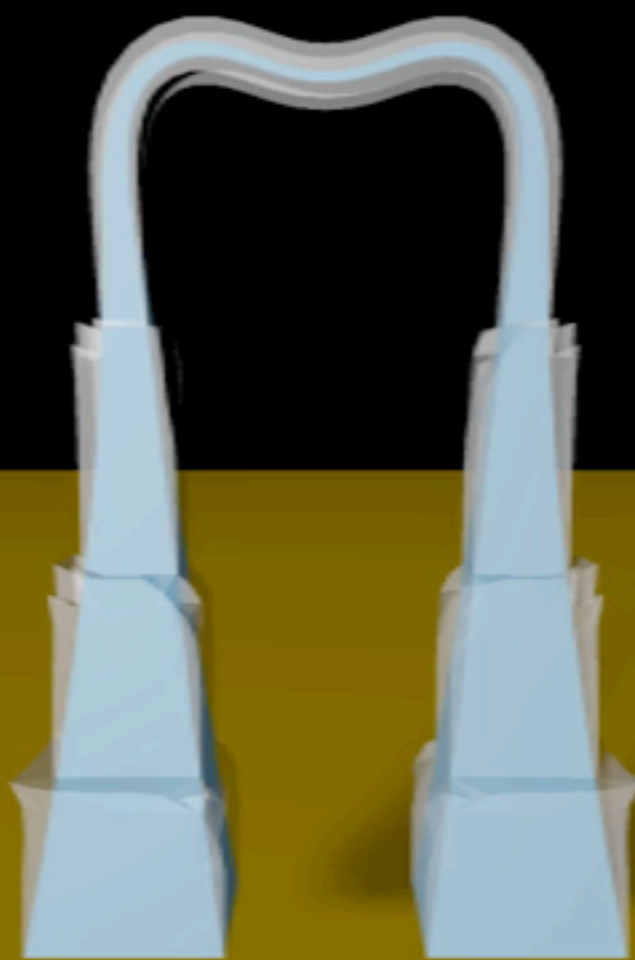
Reference

Treated

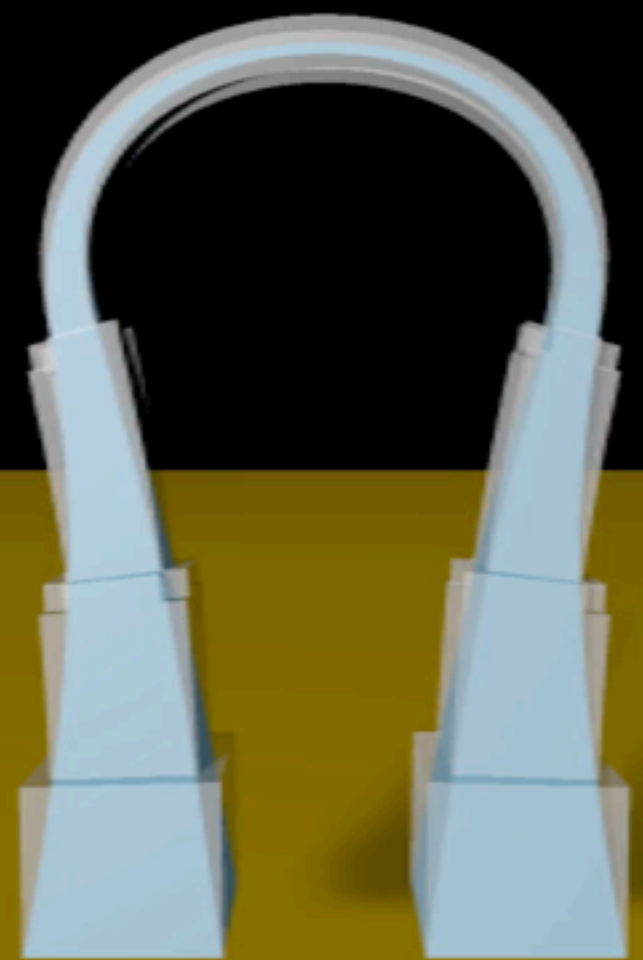
Not Treated



Reference



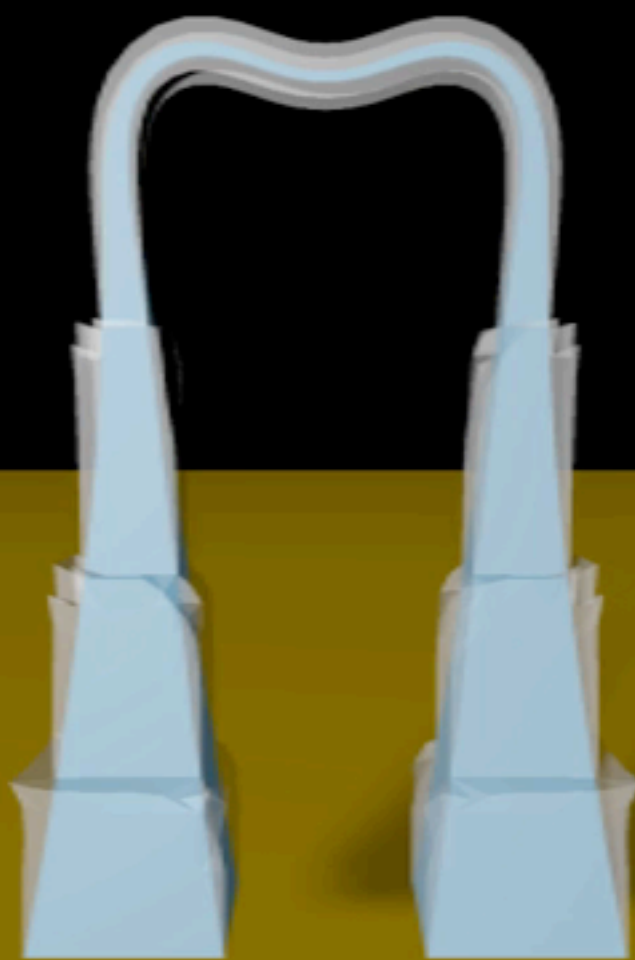
Treated



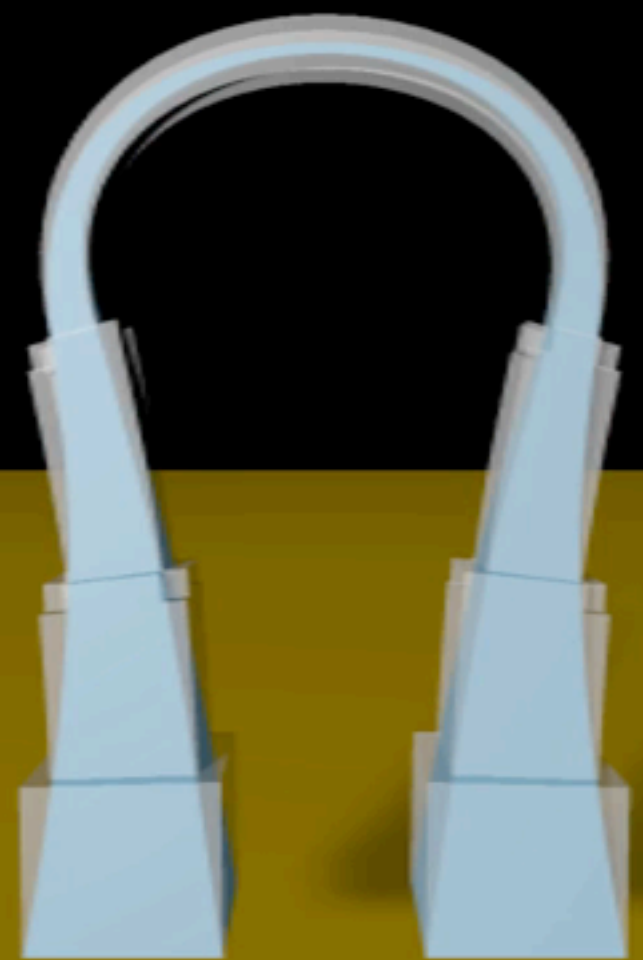
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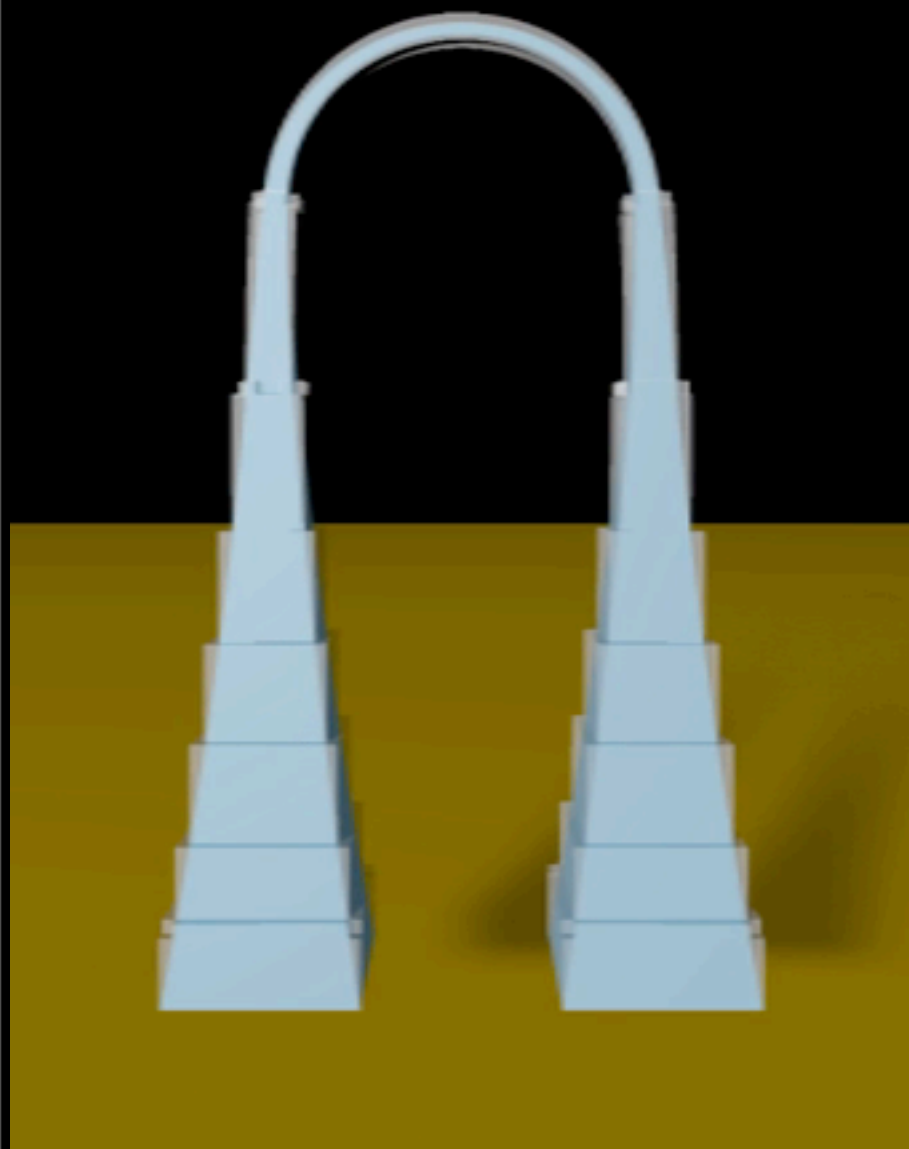
Reference



Treated



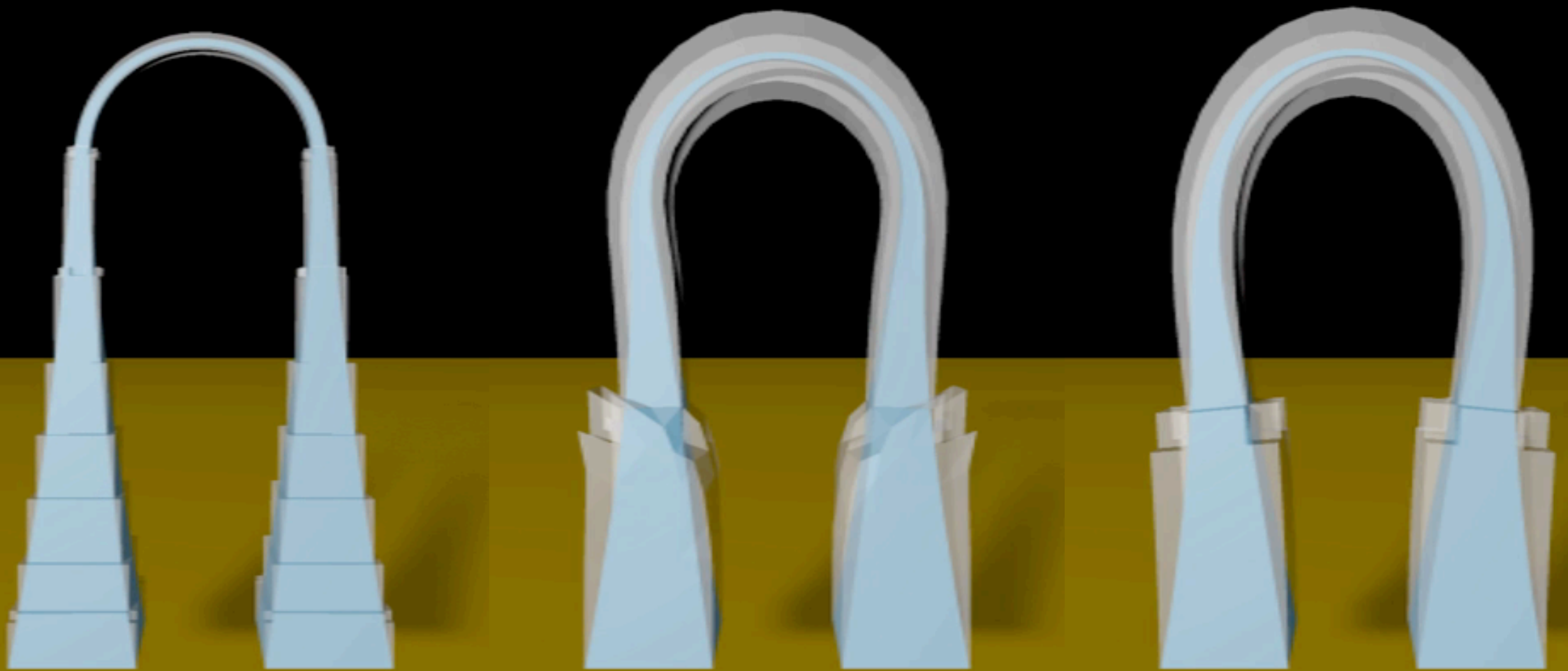
Not Treated



Reference

Treated

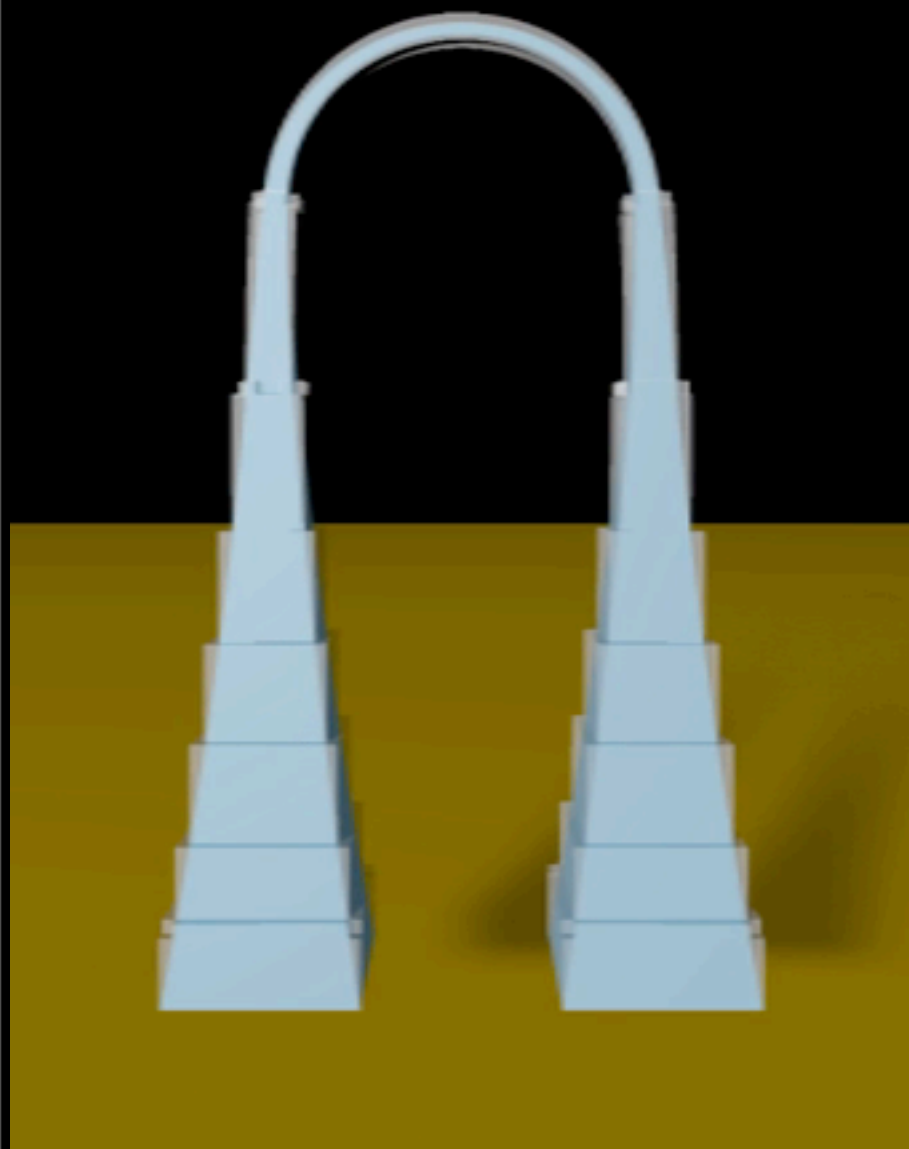
Not Treated



Reference

Treated

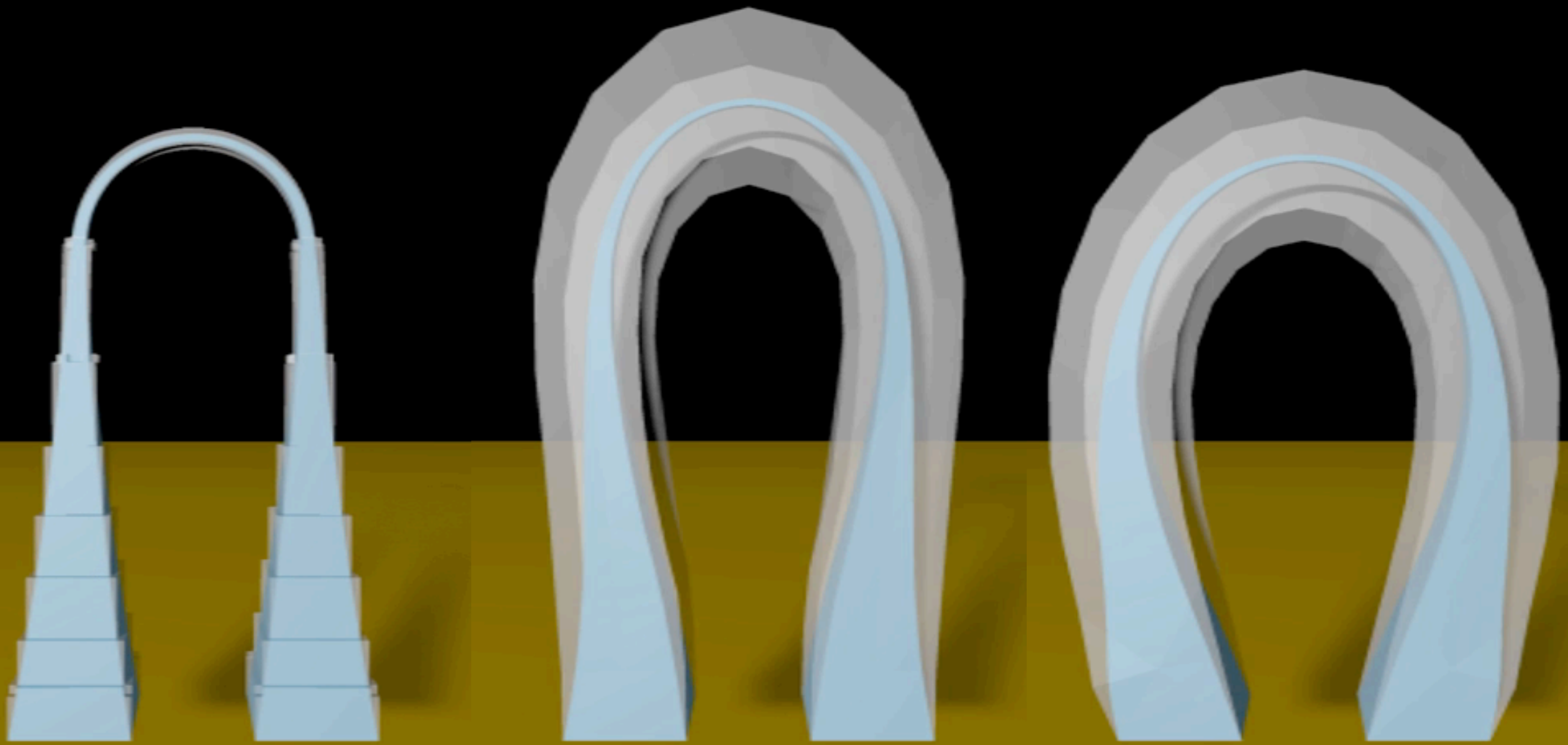
Not Treated



Reference

Treated

Not Treated



Reference

Treated

Not Treated

BOUNDARY CELL TREATMENT

Start with Energy Density



Apply Incompressibility Adjustment



Compute Discrete Energy \hat{E}



Derive Nodal Forces $f(x)$



Find Equilibrium $f(x) = 0 \implies \min \hat{E}$

BOUNDARY CELL TREATMENT

Start with Energy Density



Apply Incompressibility Adjustment



Compute Discrete Energy \hat{E}

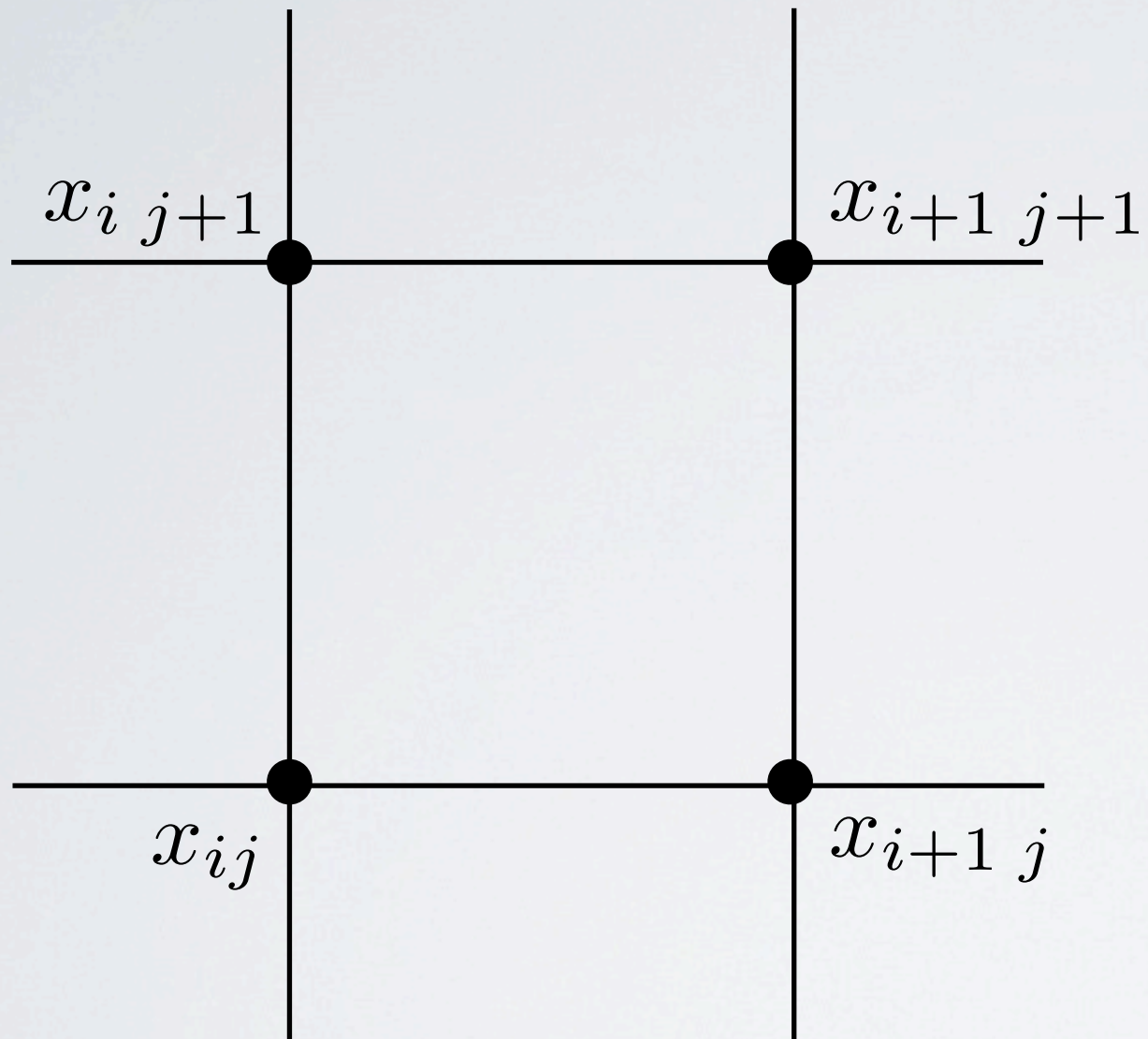


Derive Nodal Forces $f(x)$



Find Equilibrium $f(x) = 0 \implies \min \hat{E}$

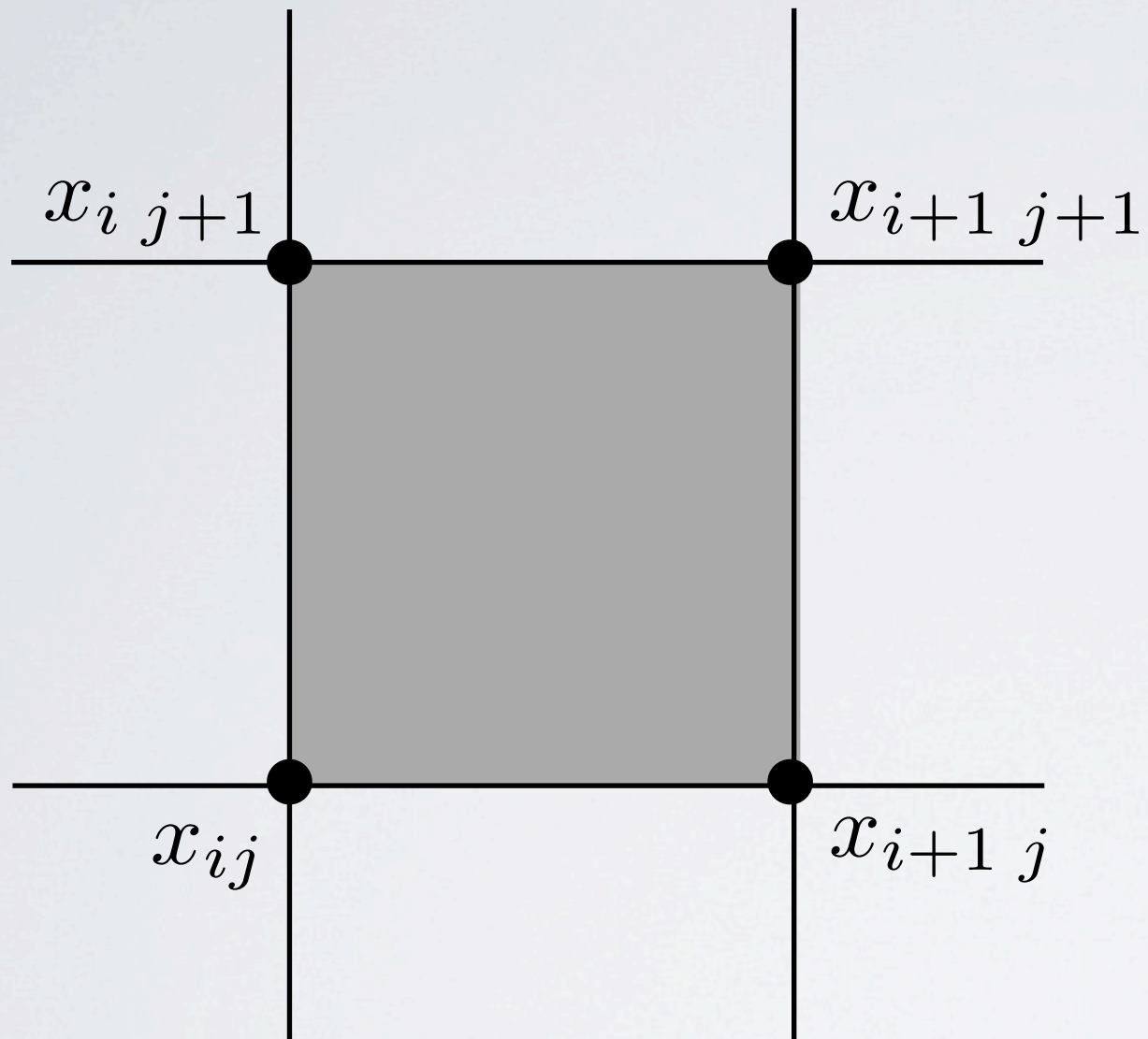
BOUNDARY CELL TREATMENT



$$E_{obj} = \sum E_{cell}$$

$$E_{cell} = \int_{cell} \Psi(F) \partial X$$

BOUNDARY CELL TREATMENT

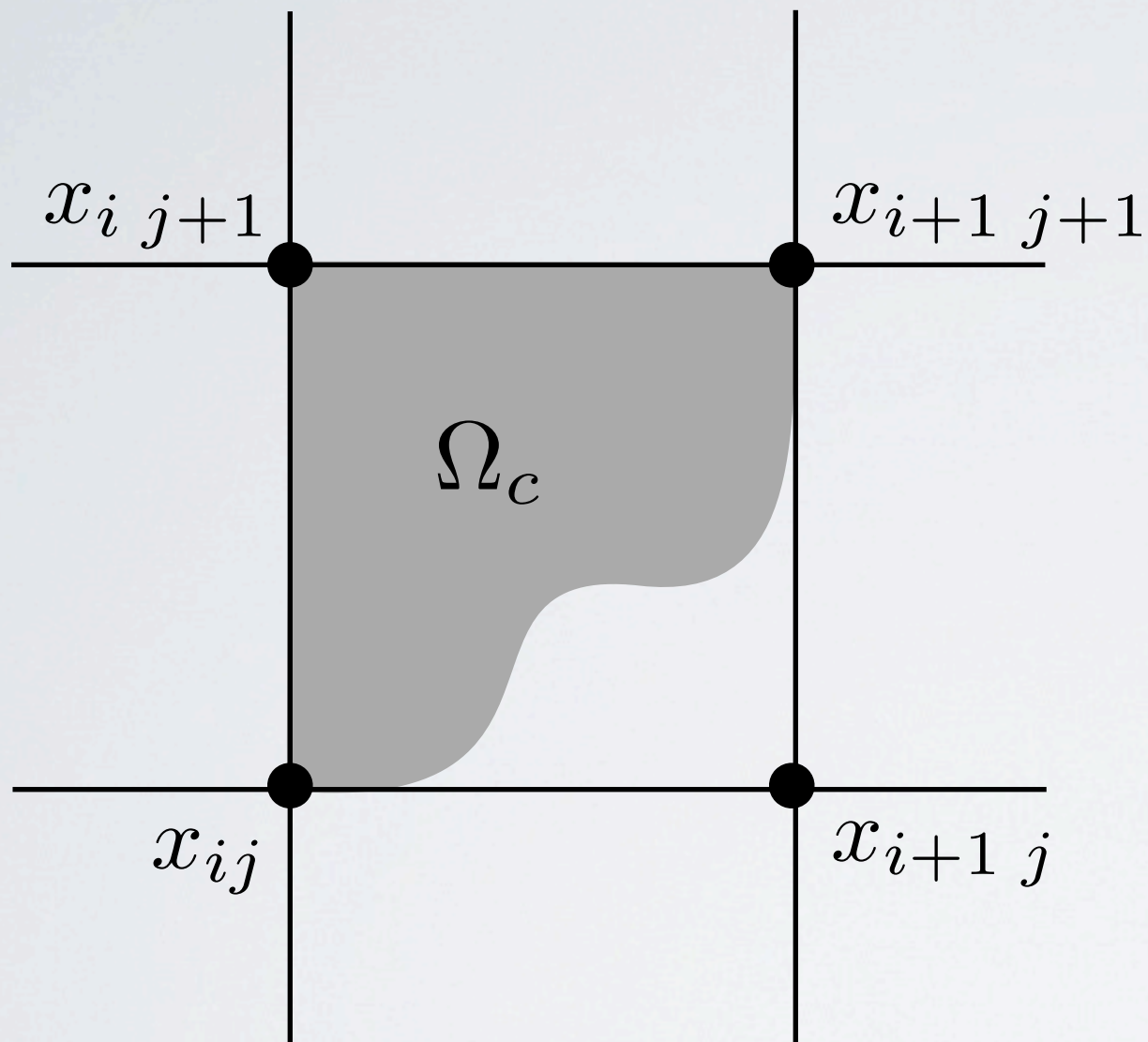


$$E_{obj} = \sum E_{cell}$$

Whole cells are straight-forward.

$$E_{cell} = \int_{[0,h]^3} \Psi(F) \partial X$$

BOUNDARY CELL TREATMENT



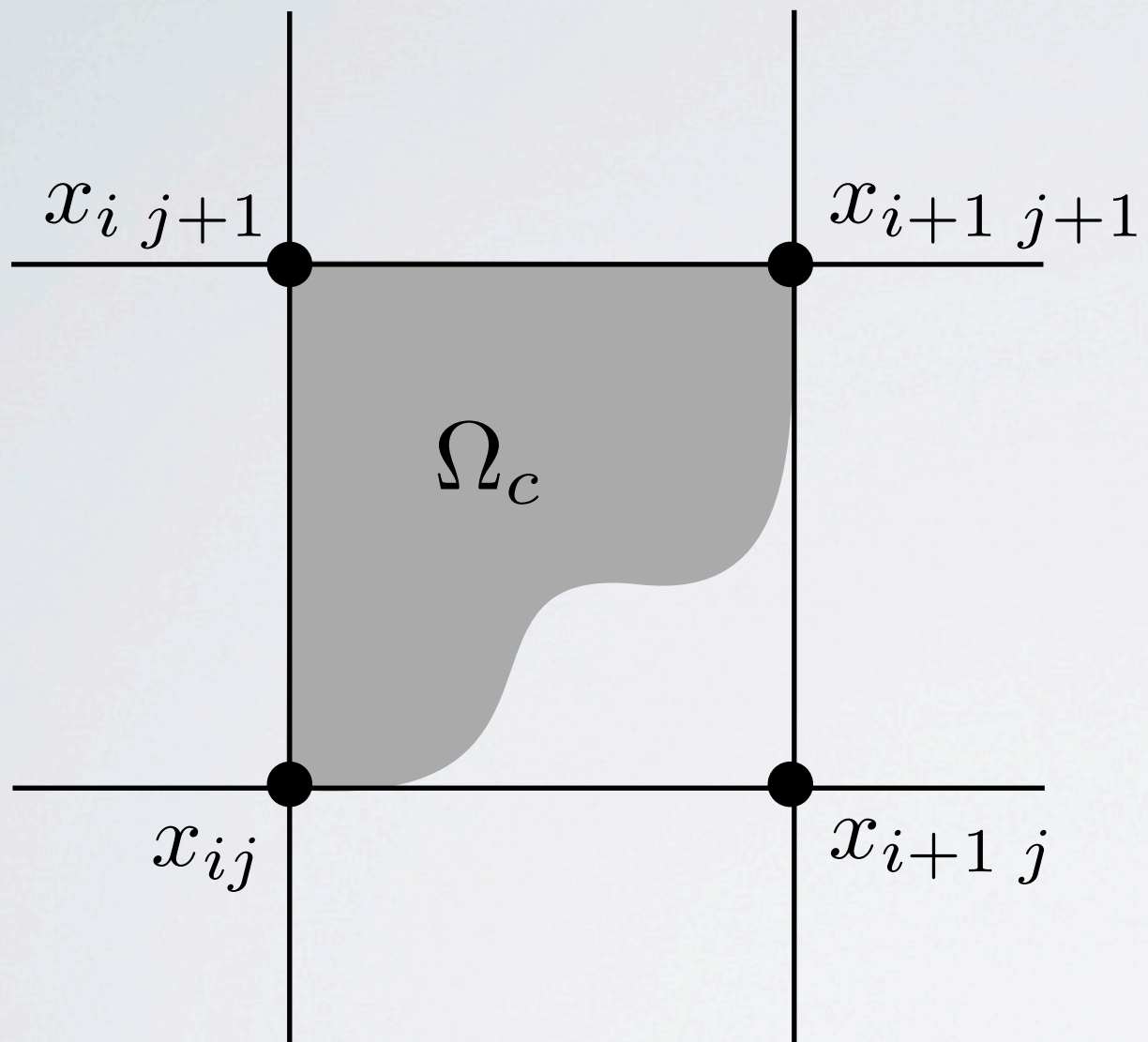
$$E_{obj} = \sum E_{cell}$$

Fractional cells are tricky.

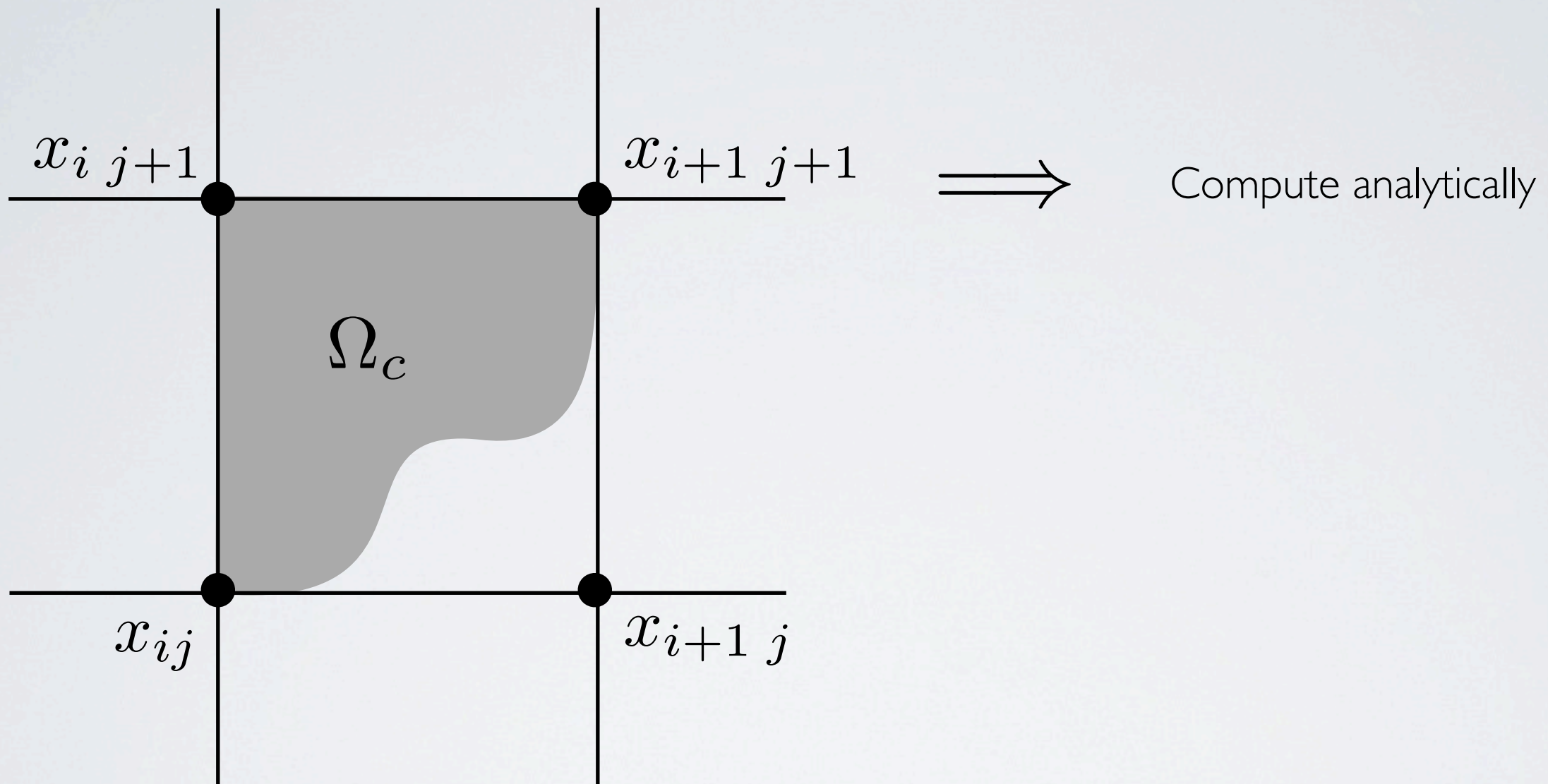
$$E_{cell} = \int_{\Omega_c} \Psi(F) \partial X$$

$$= ???$$

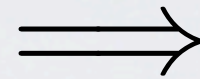
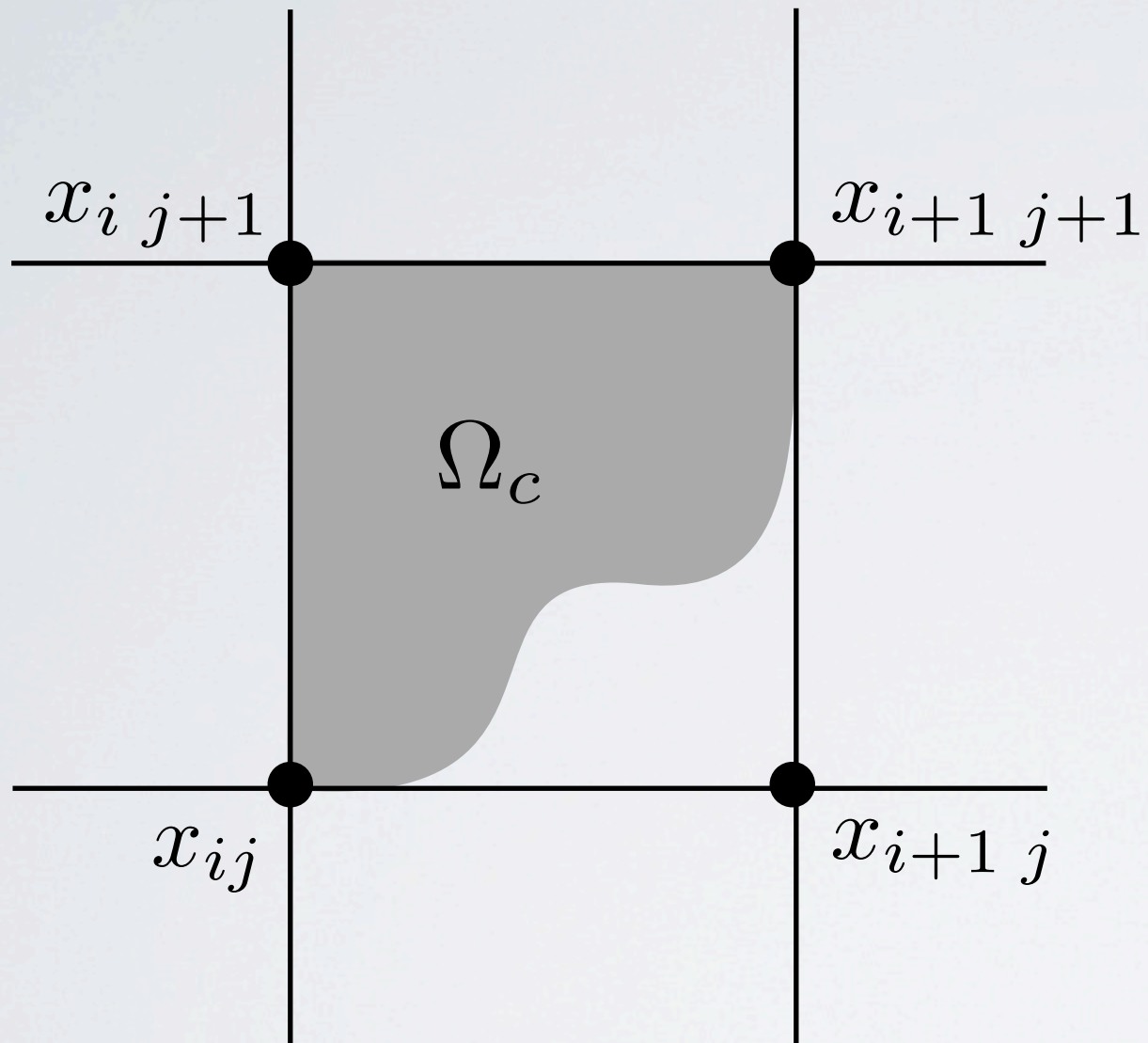
BOUNDARY CELL TREATMENT



BOUNDARY CELL TREATMENT



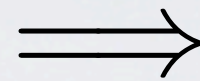
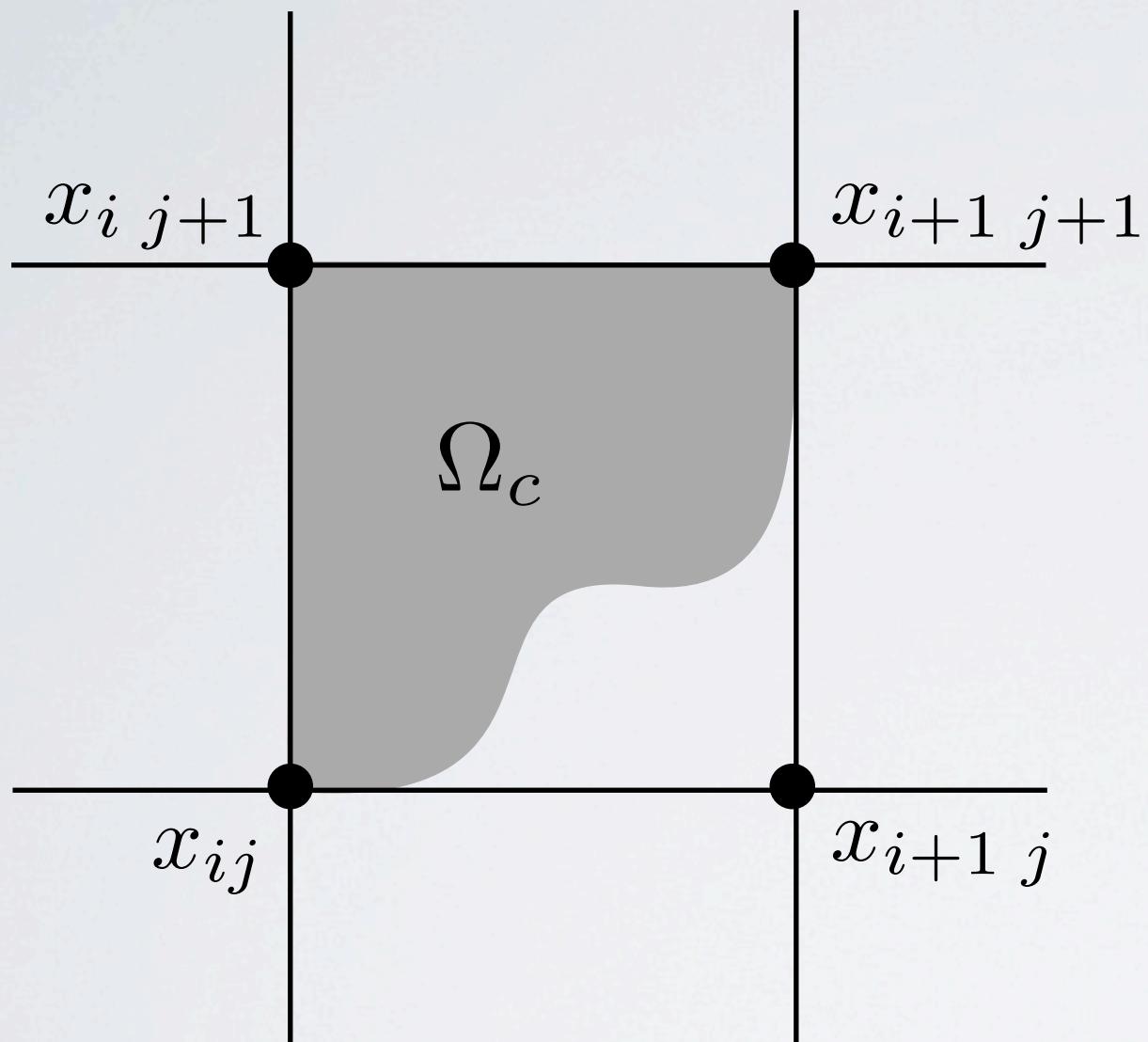
BOUNDARY CELL TREATMENT



Compute analytically

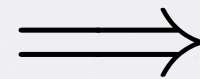
Very simple Ψ' s only

BOUNDARY CELL TREATMENT



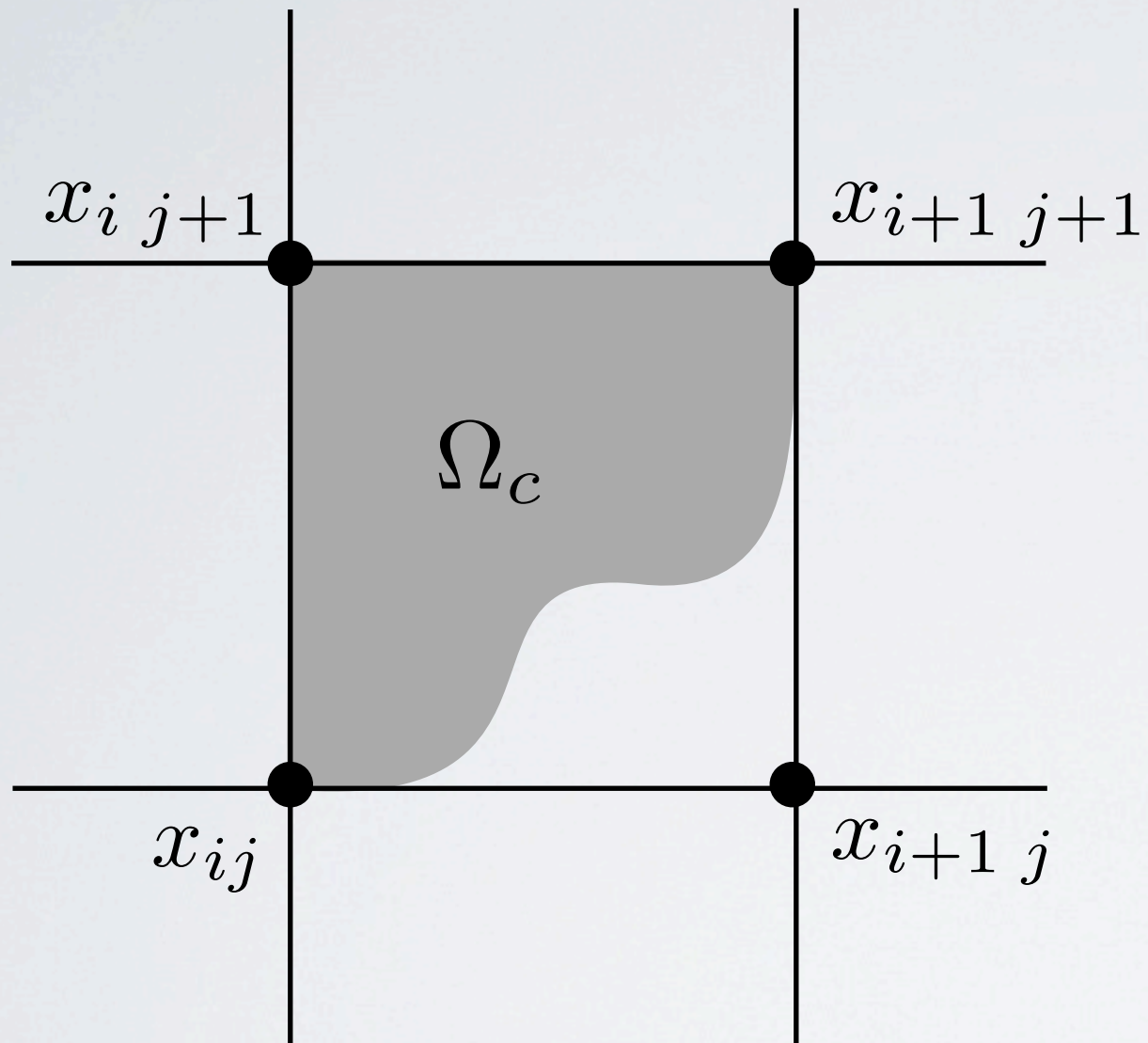
Compute analytically

Very simple Ψ' s only



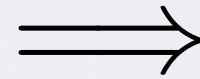
Monte-Carlo

BOUNDARY CELL TREATMENT



Compute analytically

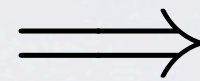
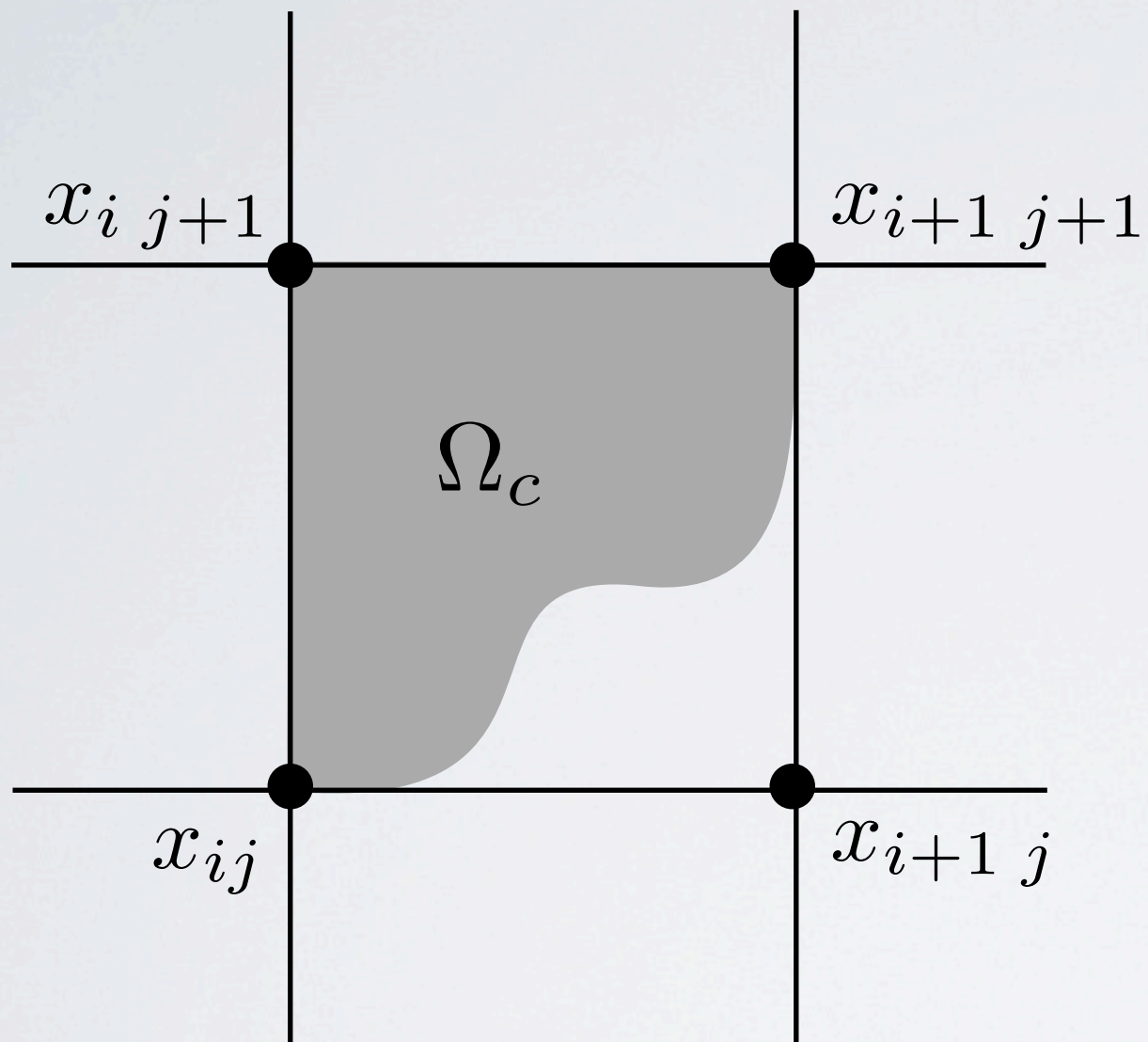
Very simple Ψ' s only



Monte-Carlo

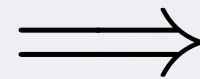
Expensive

BOUNDARY CELL TREATMENT



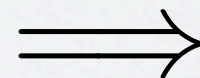
Compute analytically

Very simple Ψ' s only



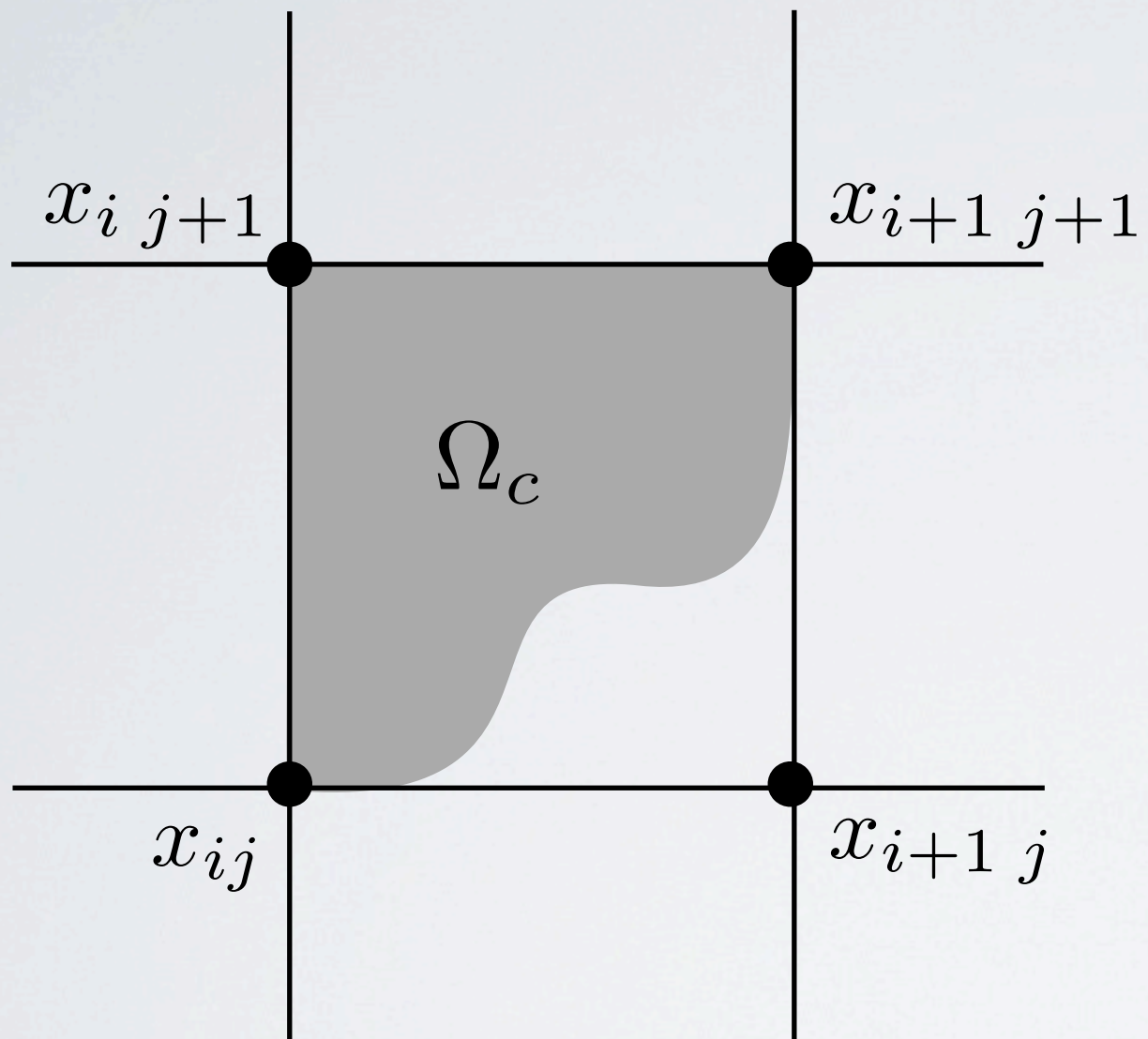
Monte-Carlo

Expensive

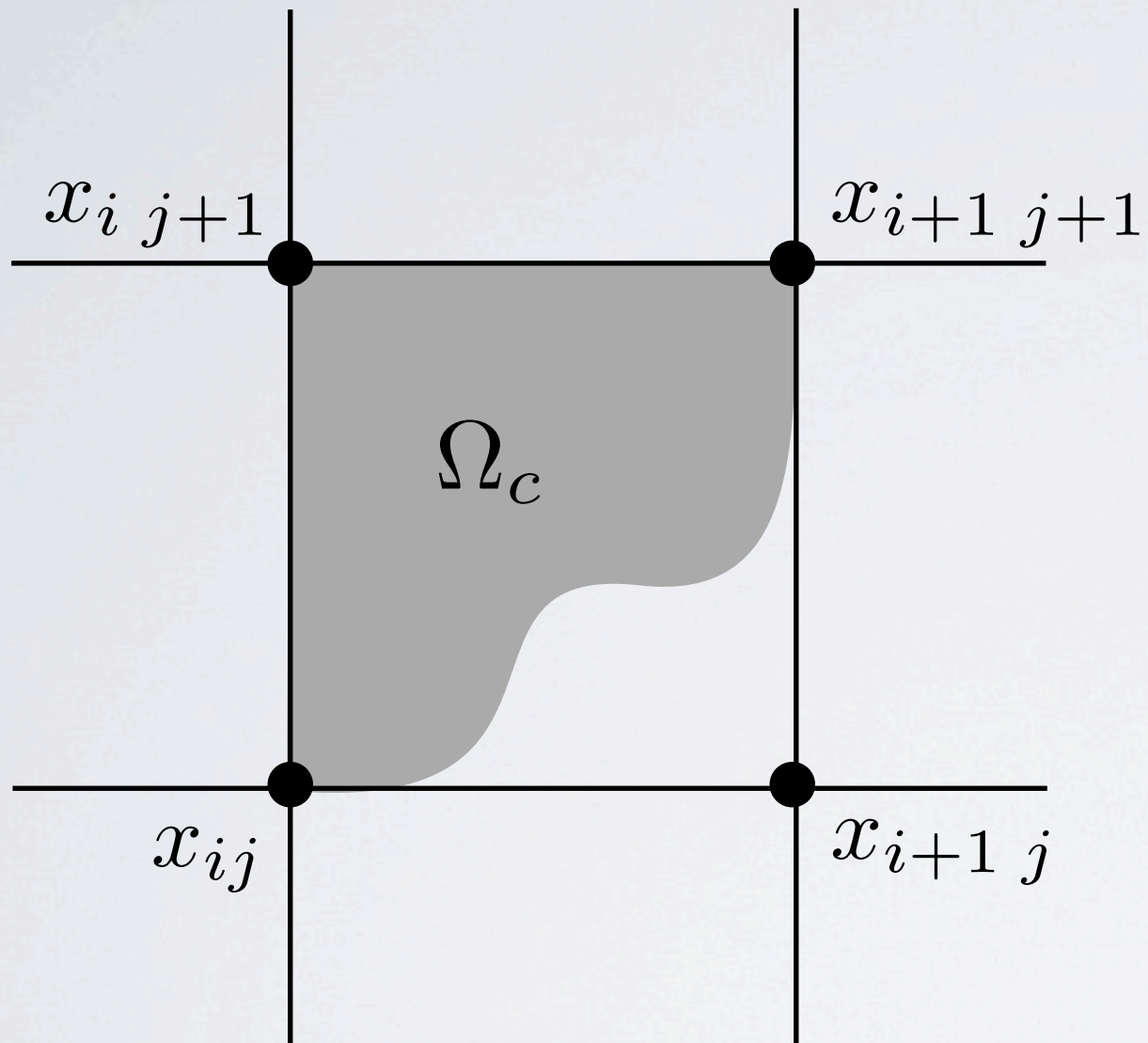


Our solution:
Efficient quadrature scheme

BOUNDARY CELL TREATMENT

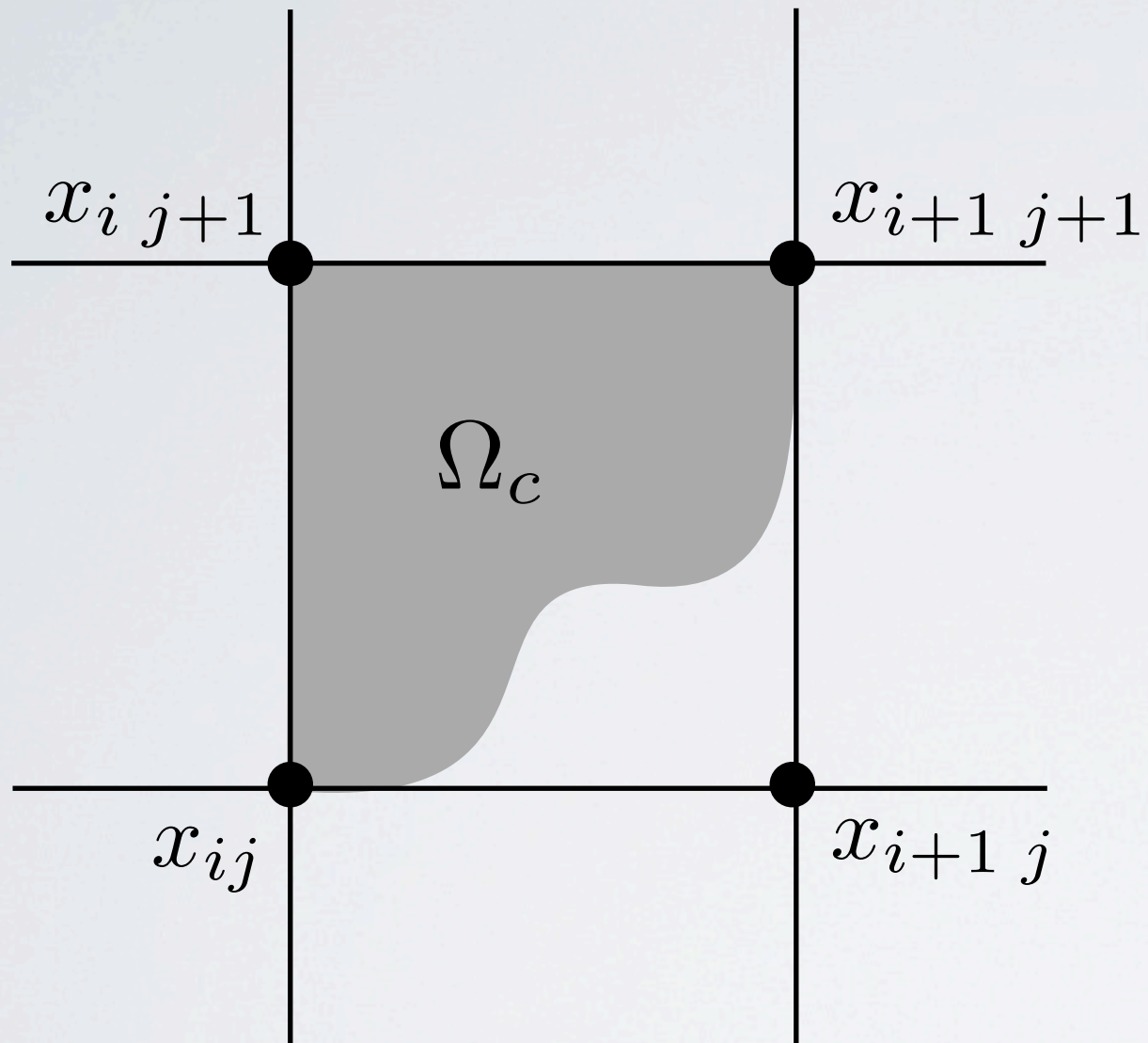


BOUNDARY CELL TREATMENT



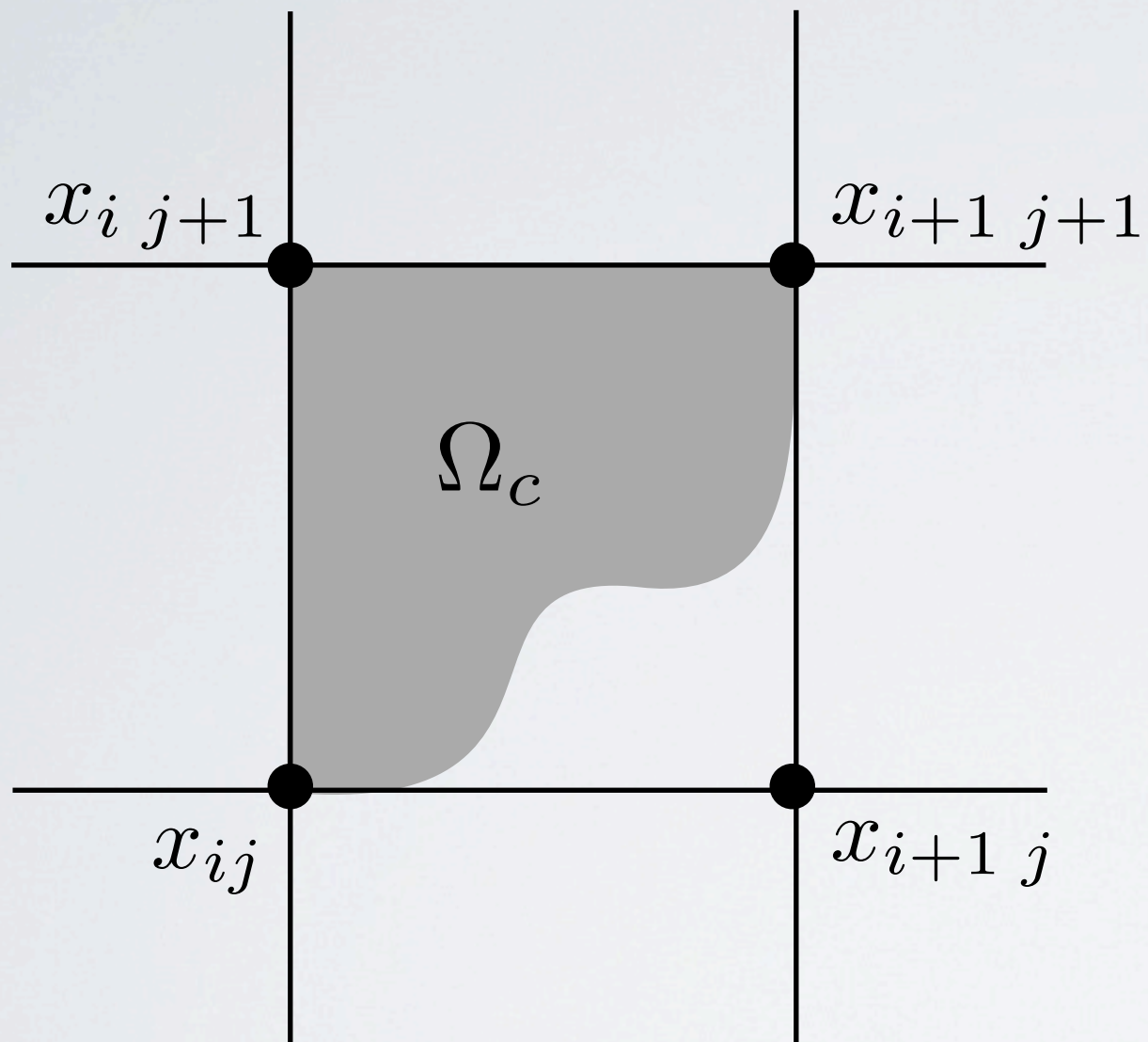
$$E_{cell} = \int_{\Omega_c} \Psi(F) \partial X$$

BOUNDARY CELL TREATMENT



$$E_{cell} = \int_{\Omega_c} \Psi(F) \partial X$$
$$\approx \sum_{i=1}^k c_i \Psi(X_i)$$

BOUNDARY CELL TREATMENT

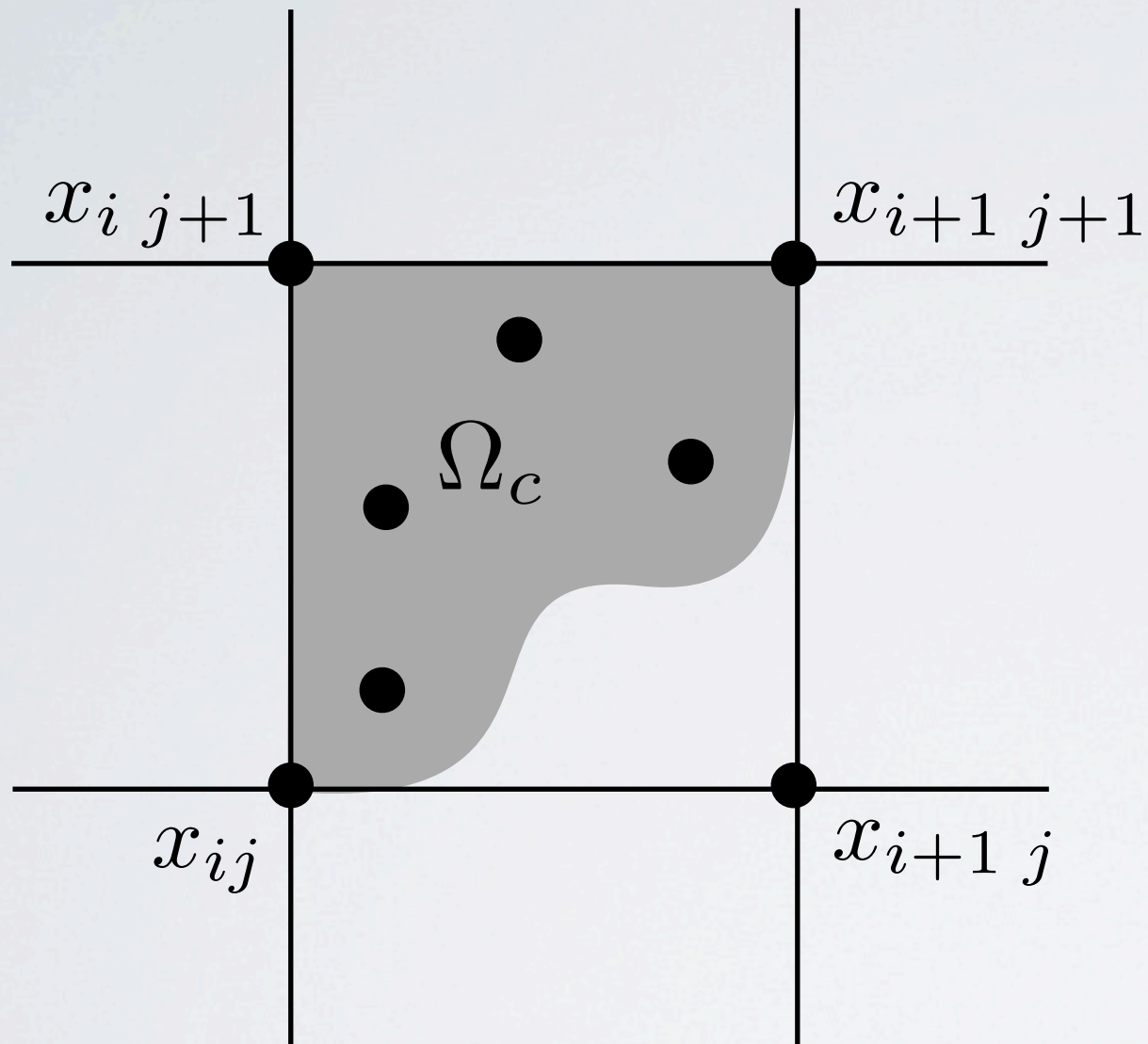


$$E_{cell} = \int_{\Omega_c} \Psi(F) \partial X$$

$$\approx \sum_{i=1}^k c_i \Psi(X_i)$$

$$\sum c_i = \text{vol}(\Omega_c)$$

BOUNDARY CELL TREATMENT

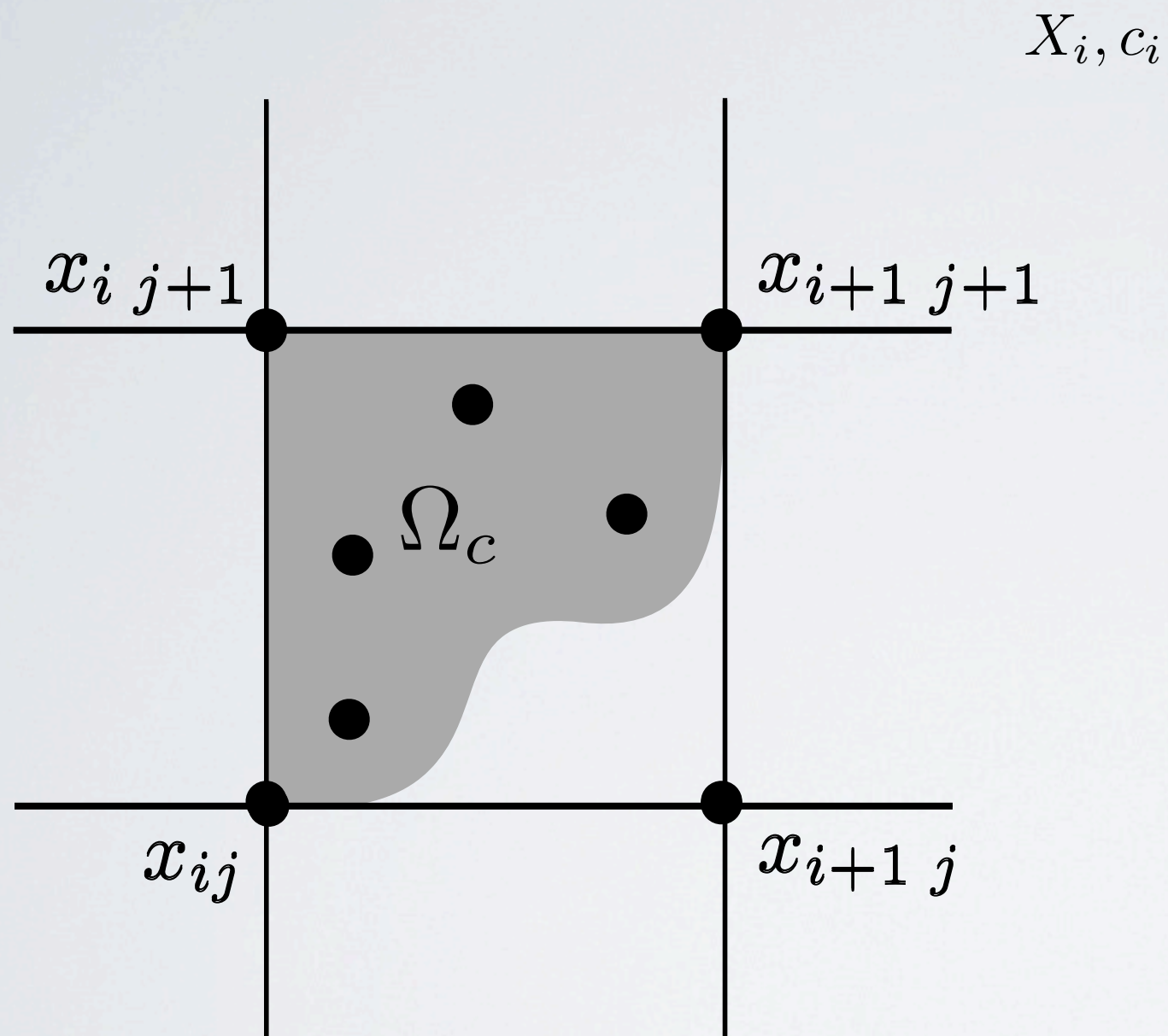


$$E_{cell} = \int_{\Omega_c} \Psi(F) \partial X$$
$$\approx \sum_{i=1}^k c_i \Psi(X_i)$$

$$\sum c_i = \text{vol}(\Omega_c)$$

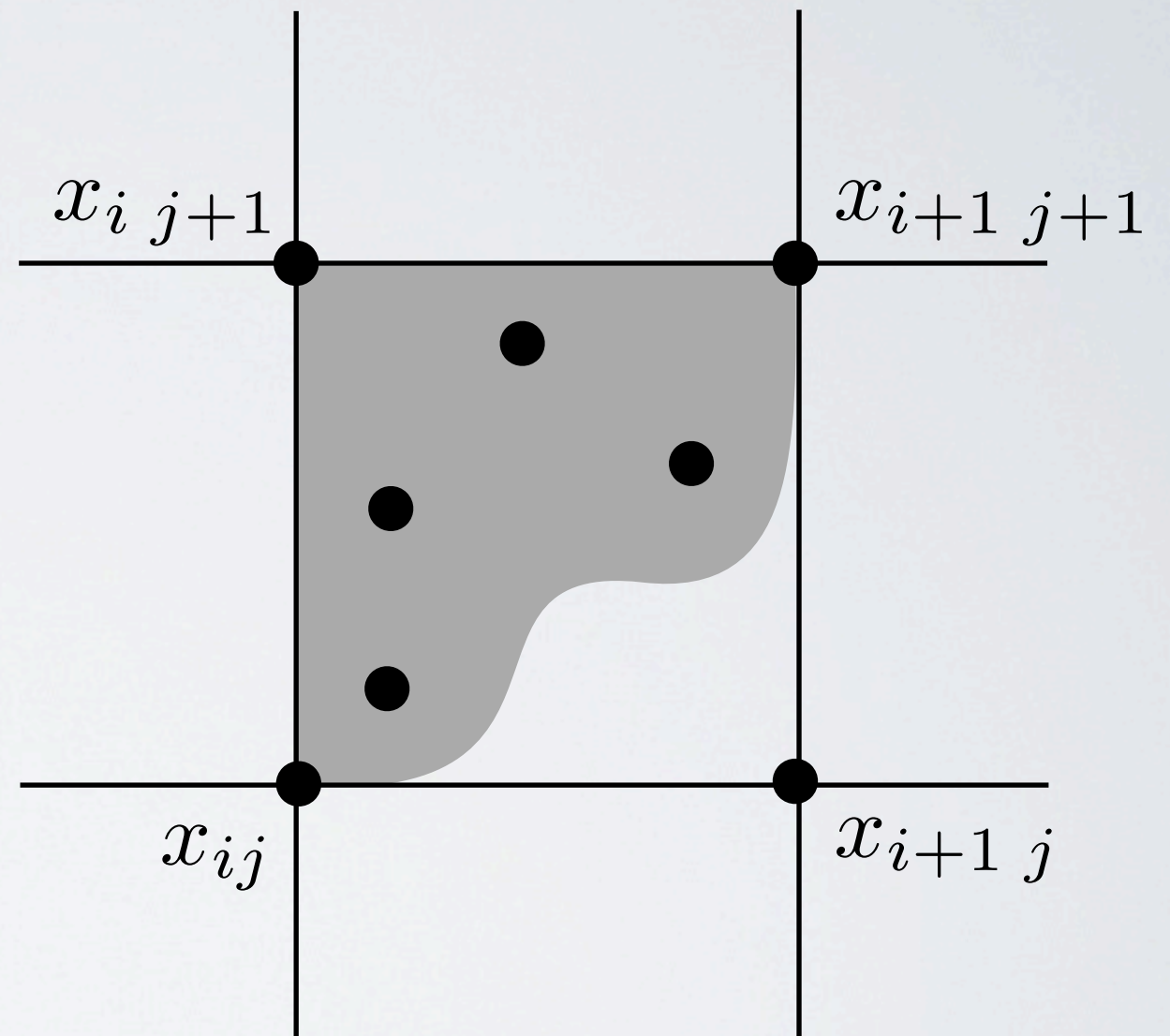
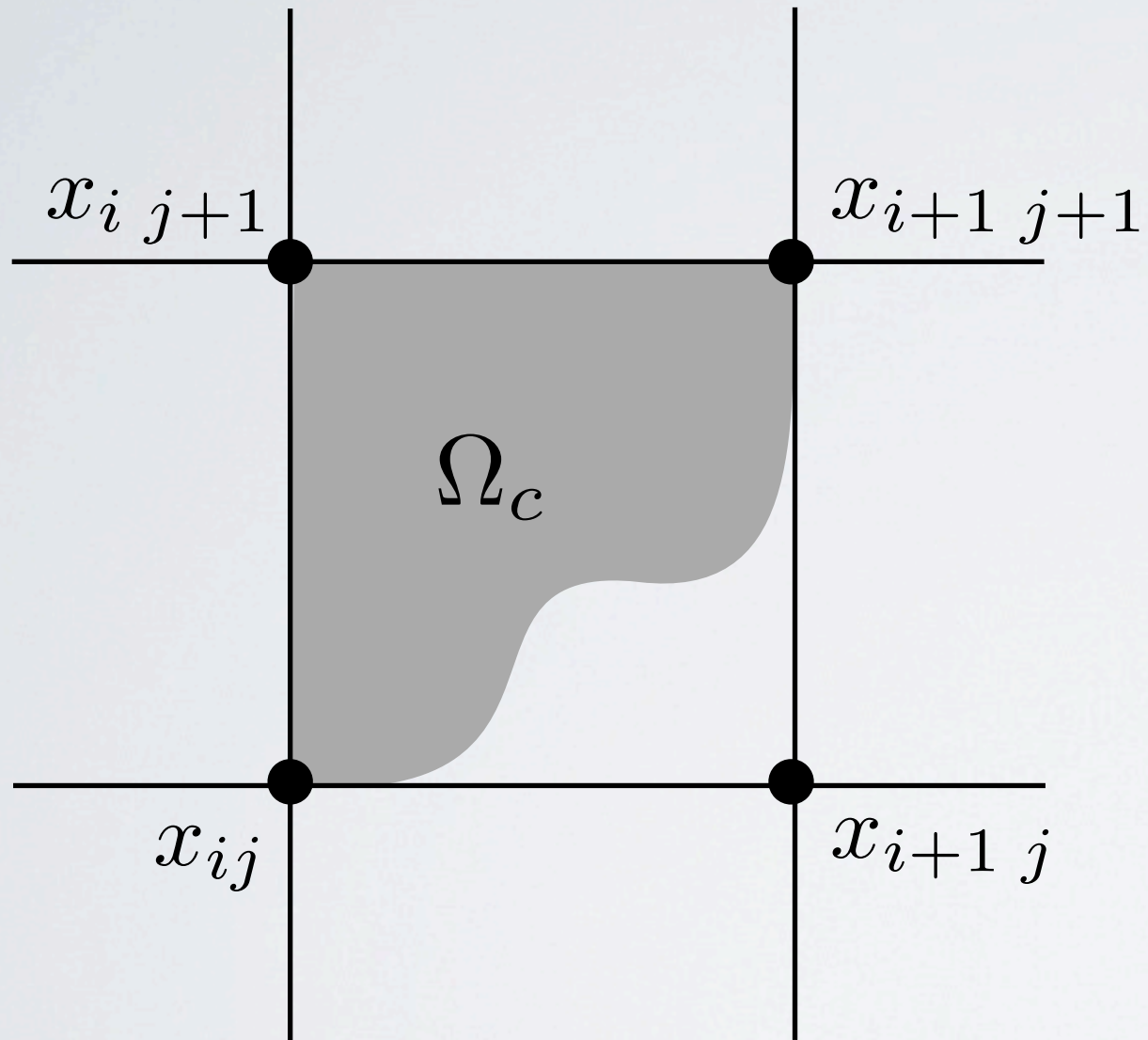
Note: $k = 4$ suffices for second order accuracy!

BOUNDARY CELL TREATMENT



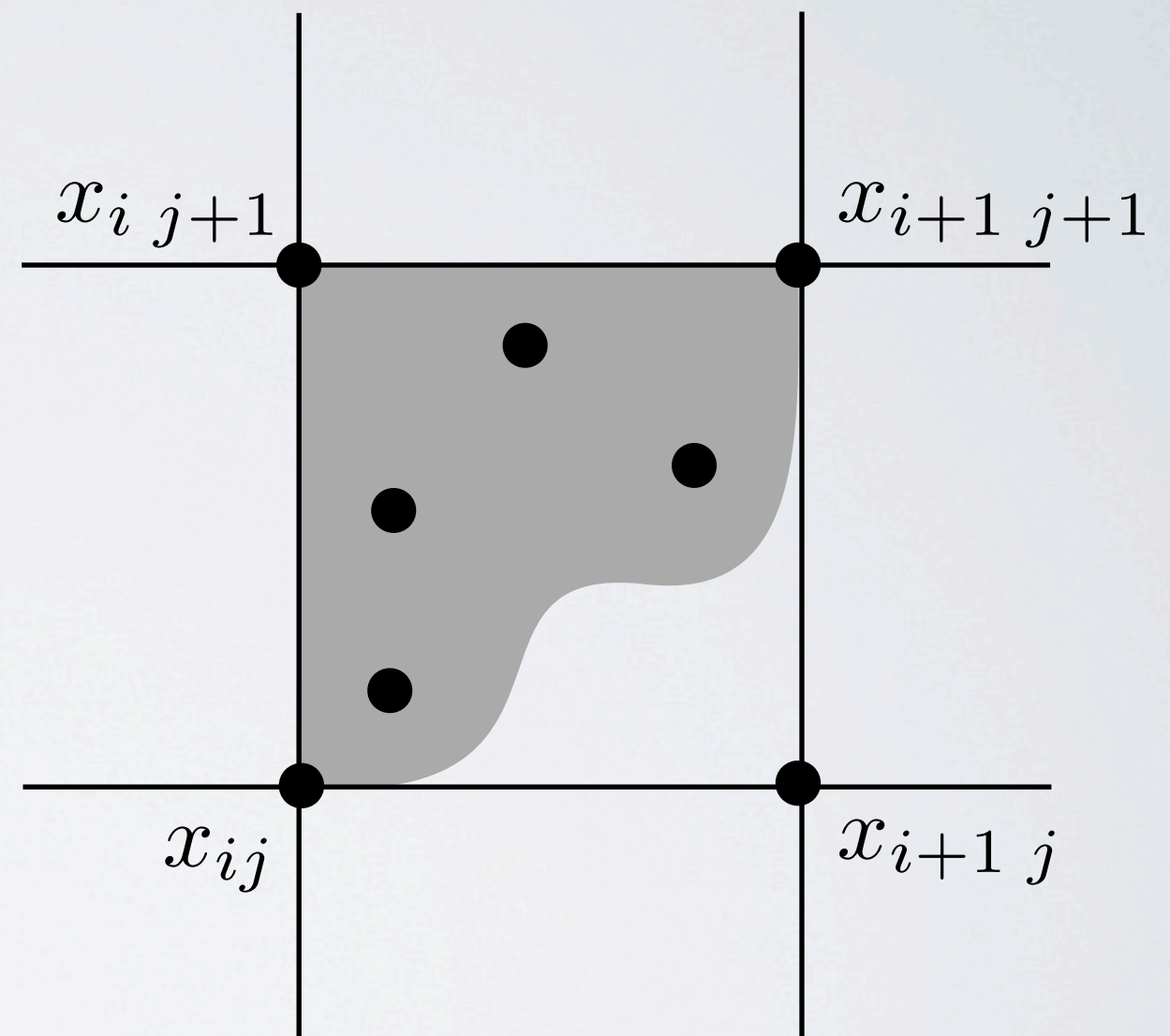
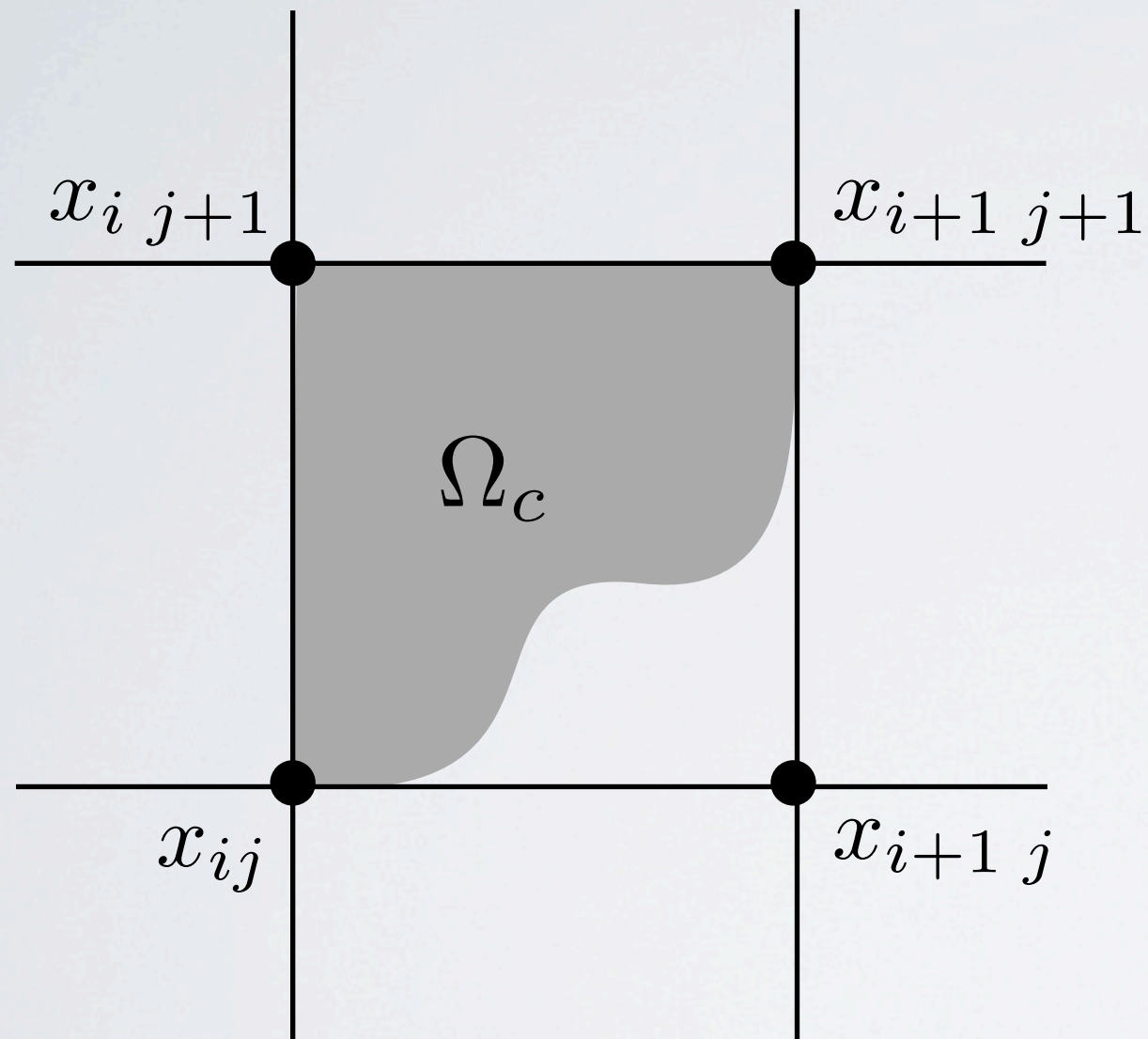
BOUNDARY CELL TREATMENT

Choose X_i, c_i such that



BOUNDARY CELL TREATMENT

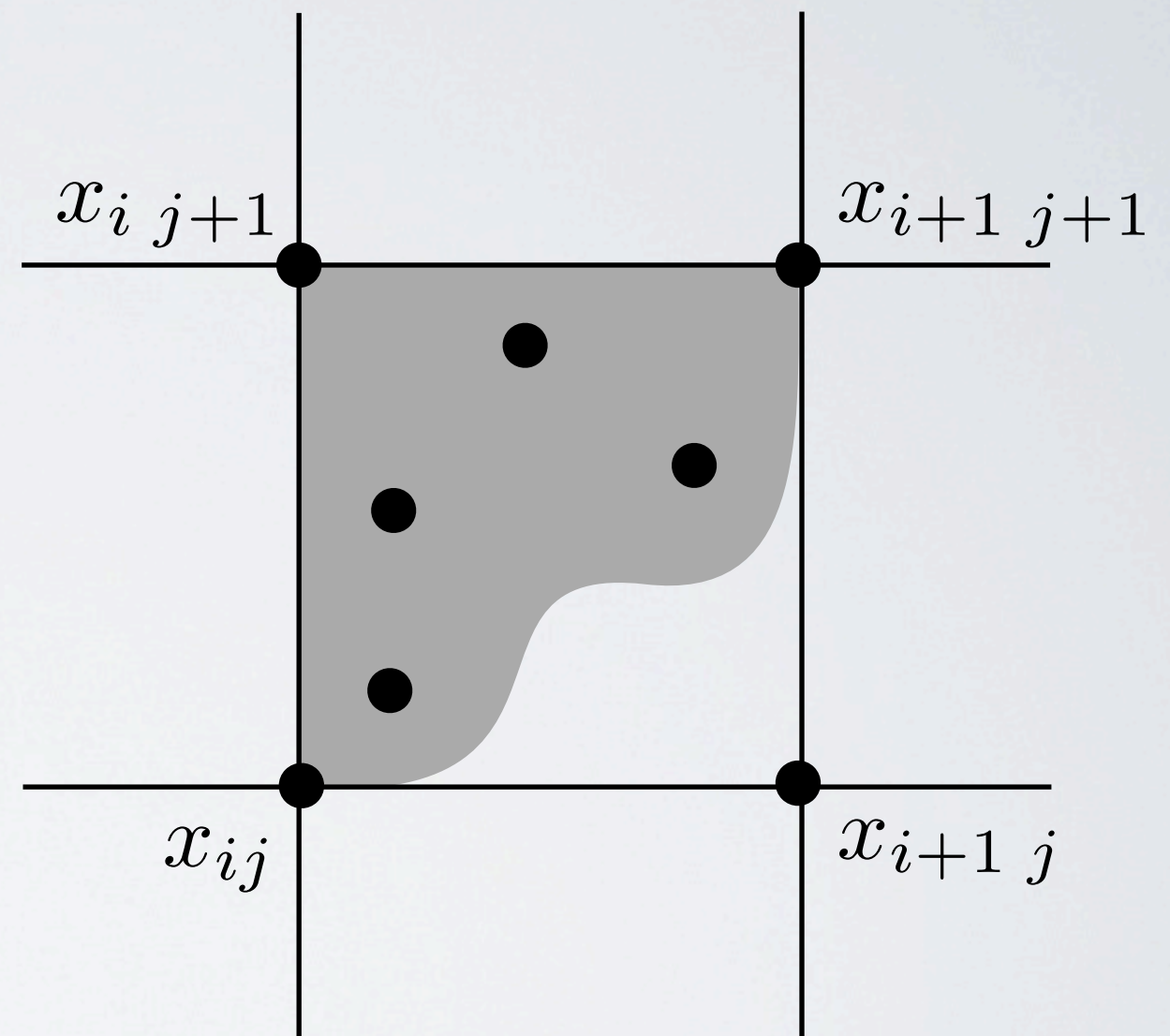
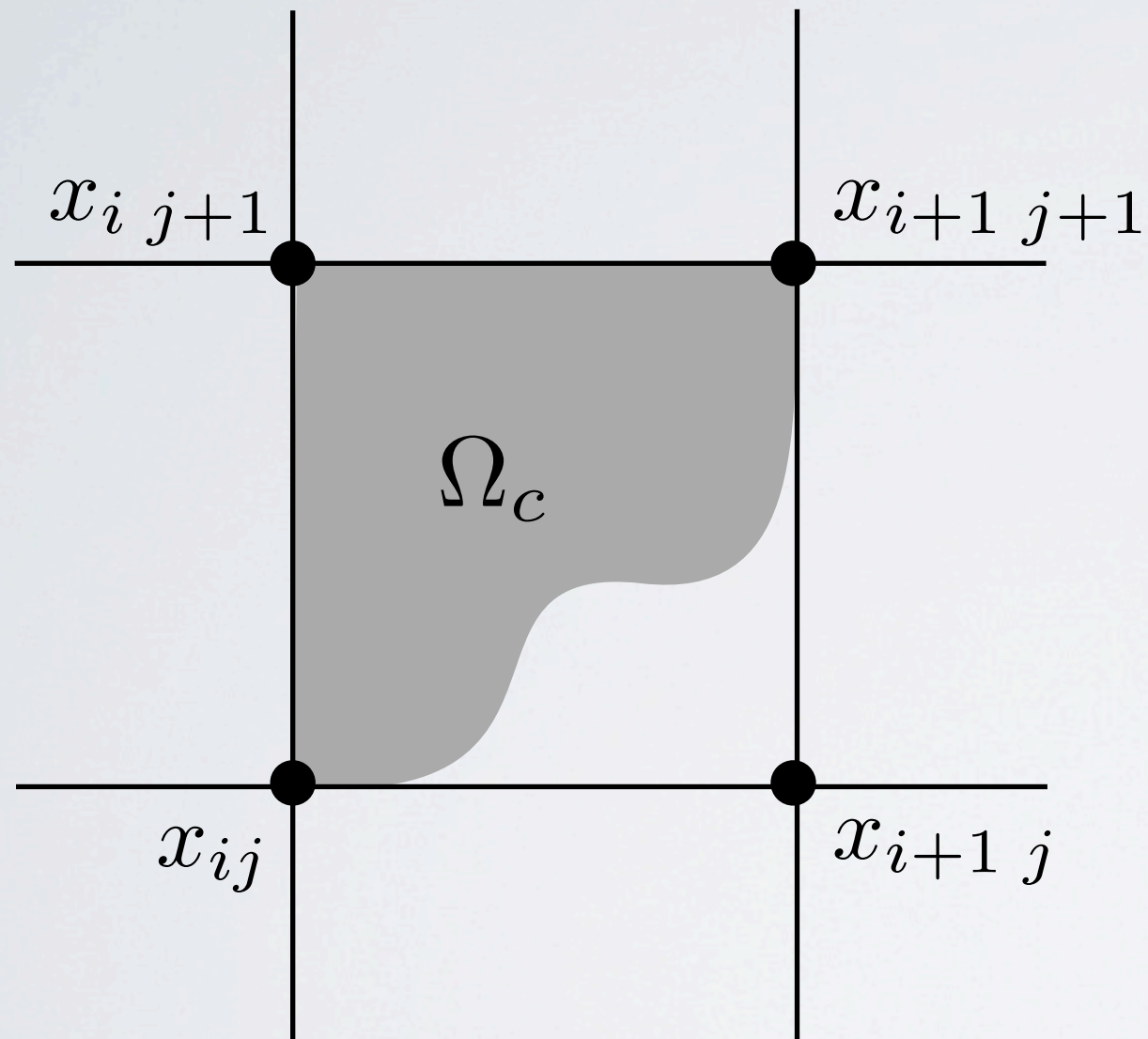
Choose X_i, c_i such that



Continuous Distribution Average = Discrete Distribution Average

BOUNDARY CELL TREATMENT

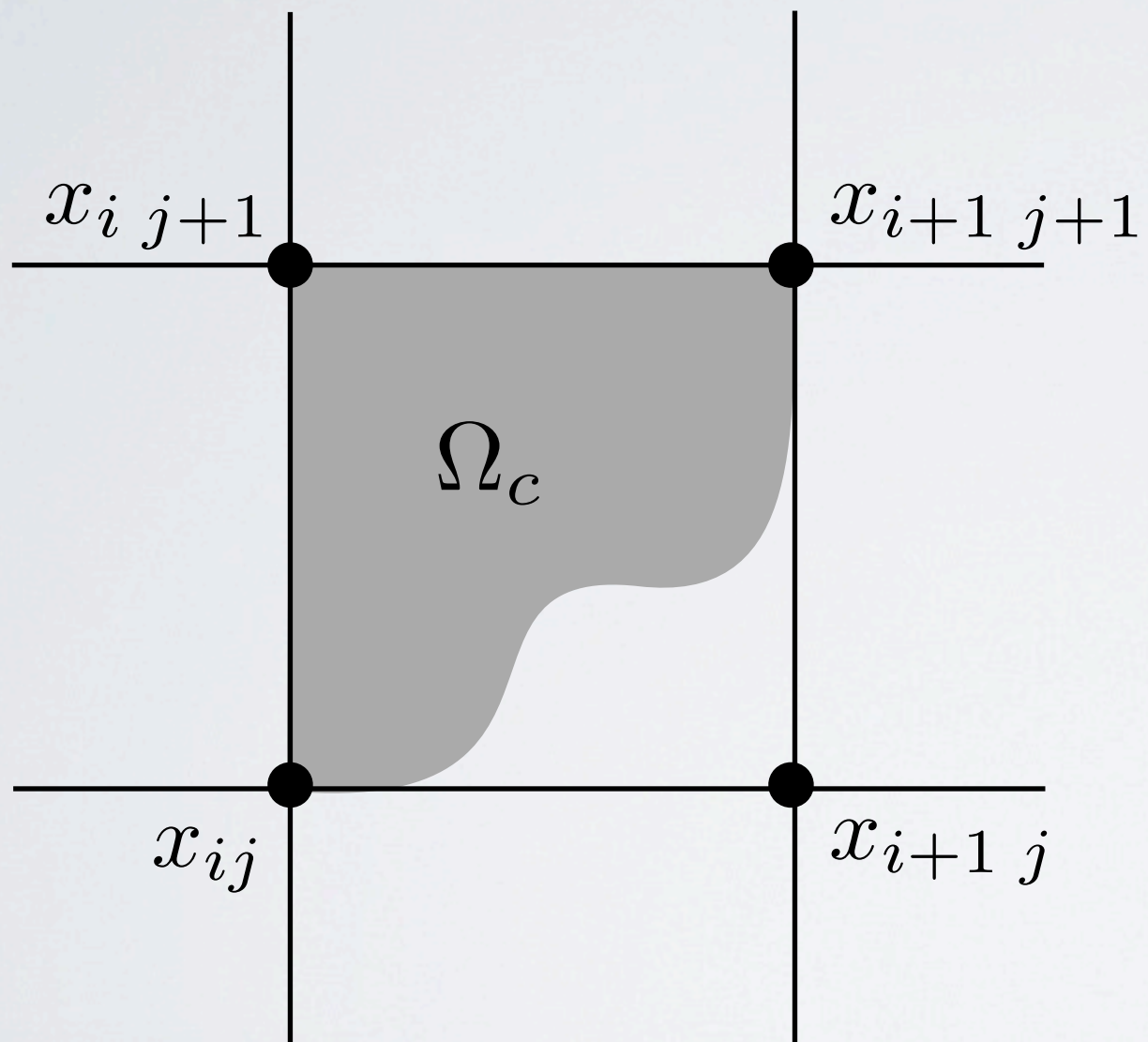
Choose X_i, c_i such that



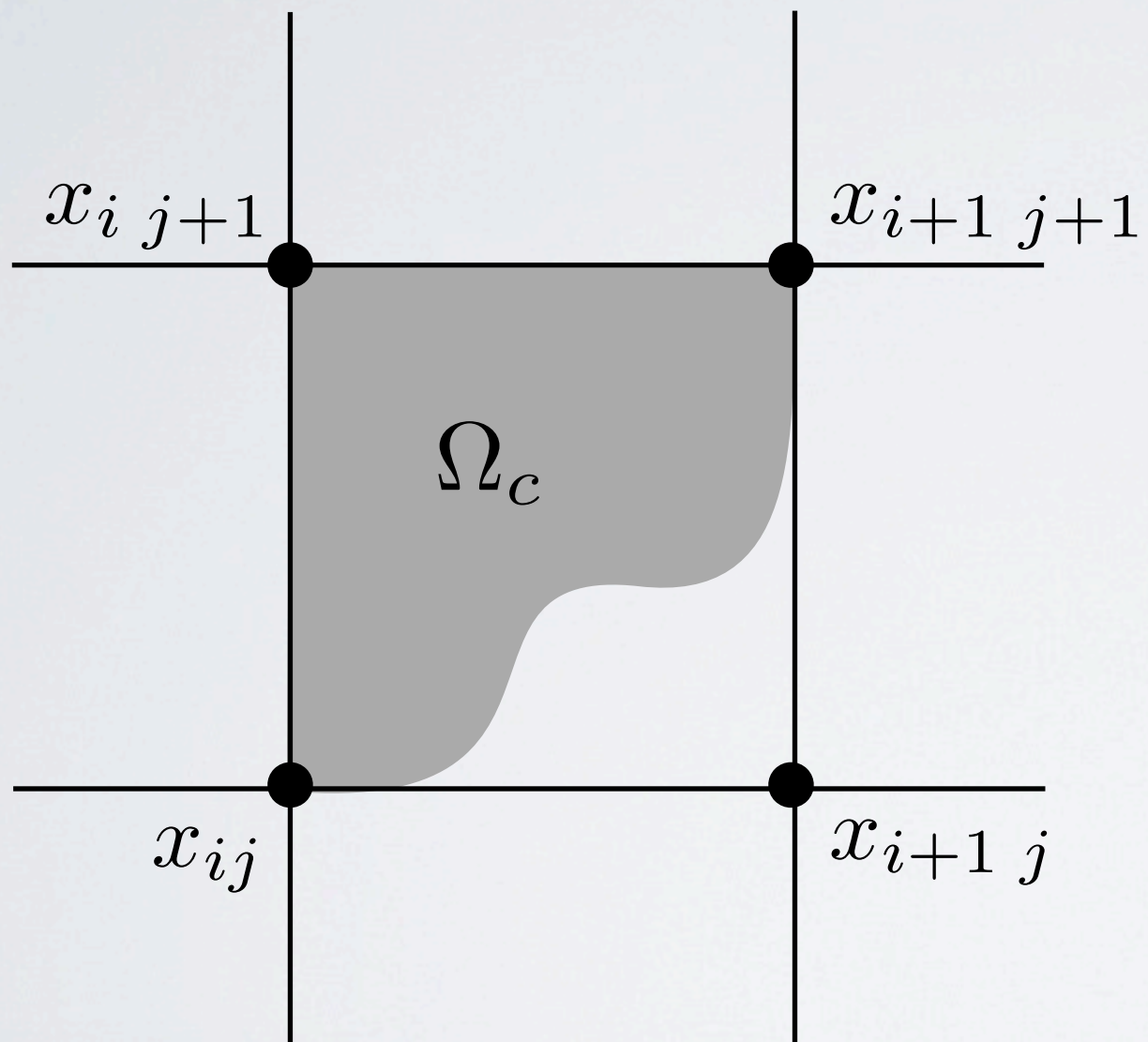
Continuous Distribution Average = Discrete Distribution Average

Continuous Distribution Variance = Discrete Distribution Variance

BOUNDARY CELL TREATMENT

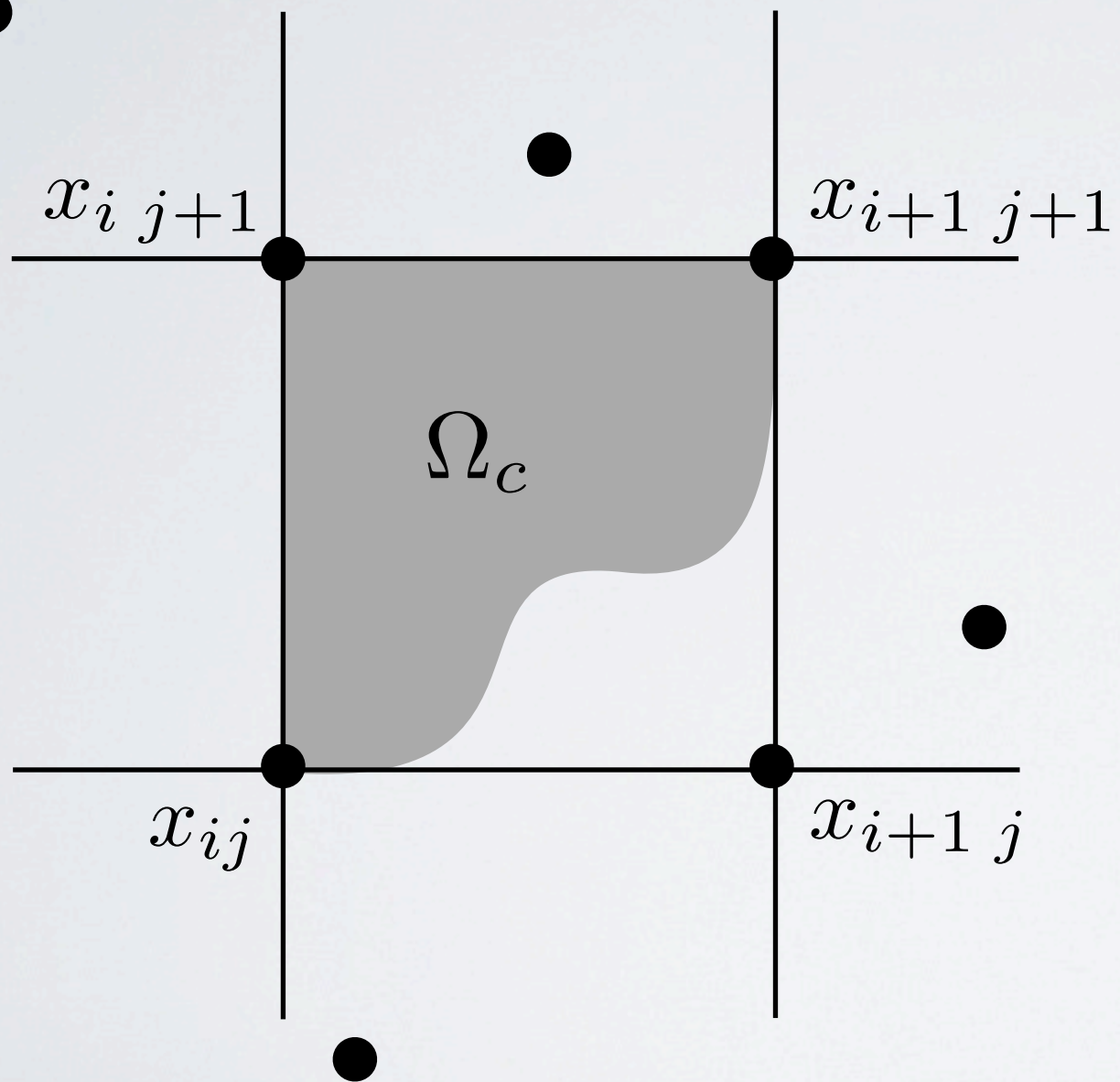


BOUNDARY CELL TREATMENT



Monte Carlo to determine Ω_c

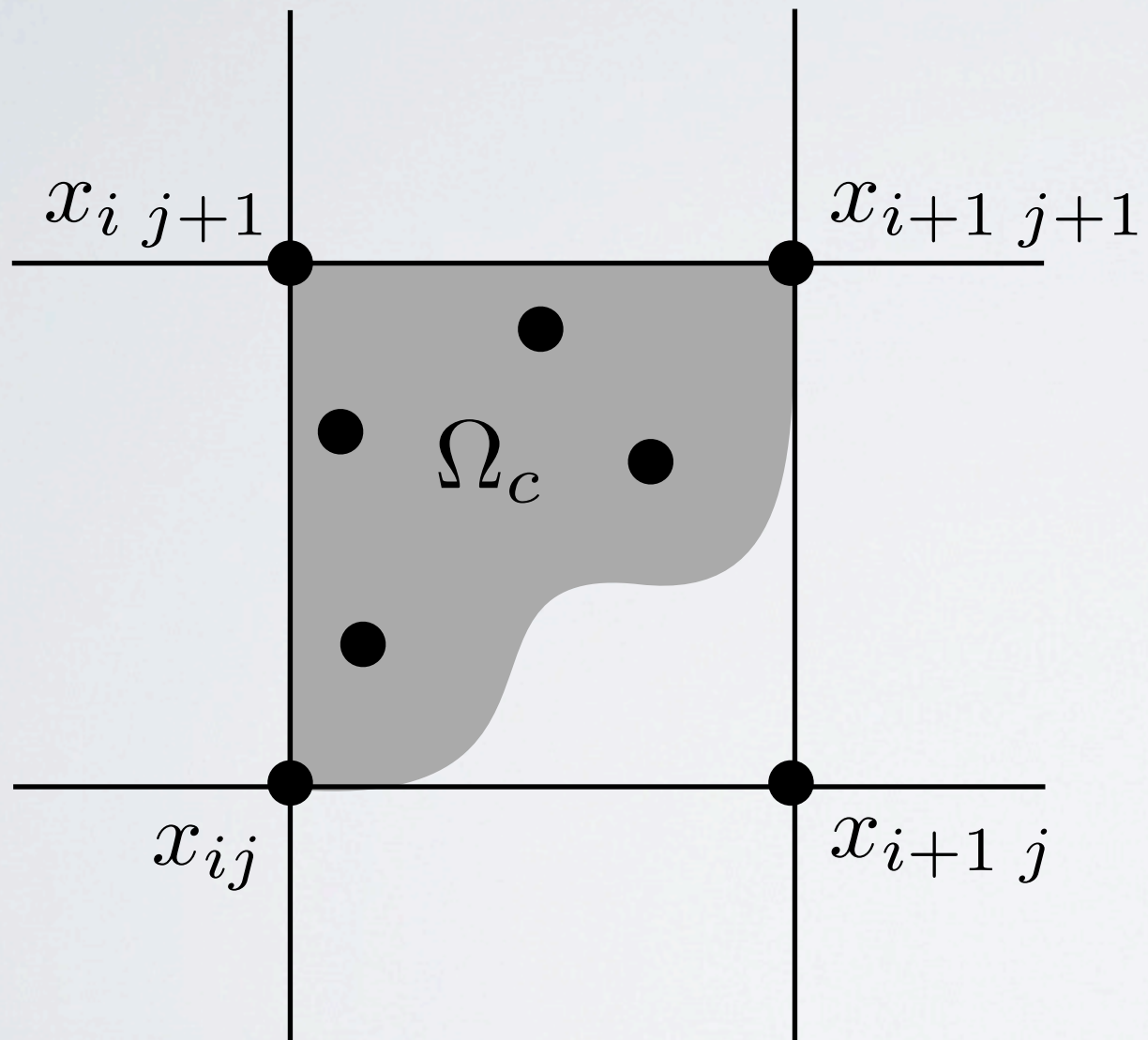
BOUNDARY CELL TREATMENT



Monte Carlo to determine Ω_c

Compute 4 representative points

BOUNDARY CELL TREATMENT

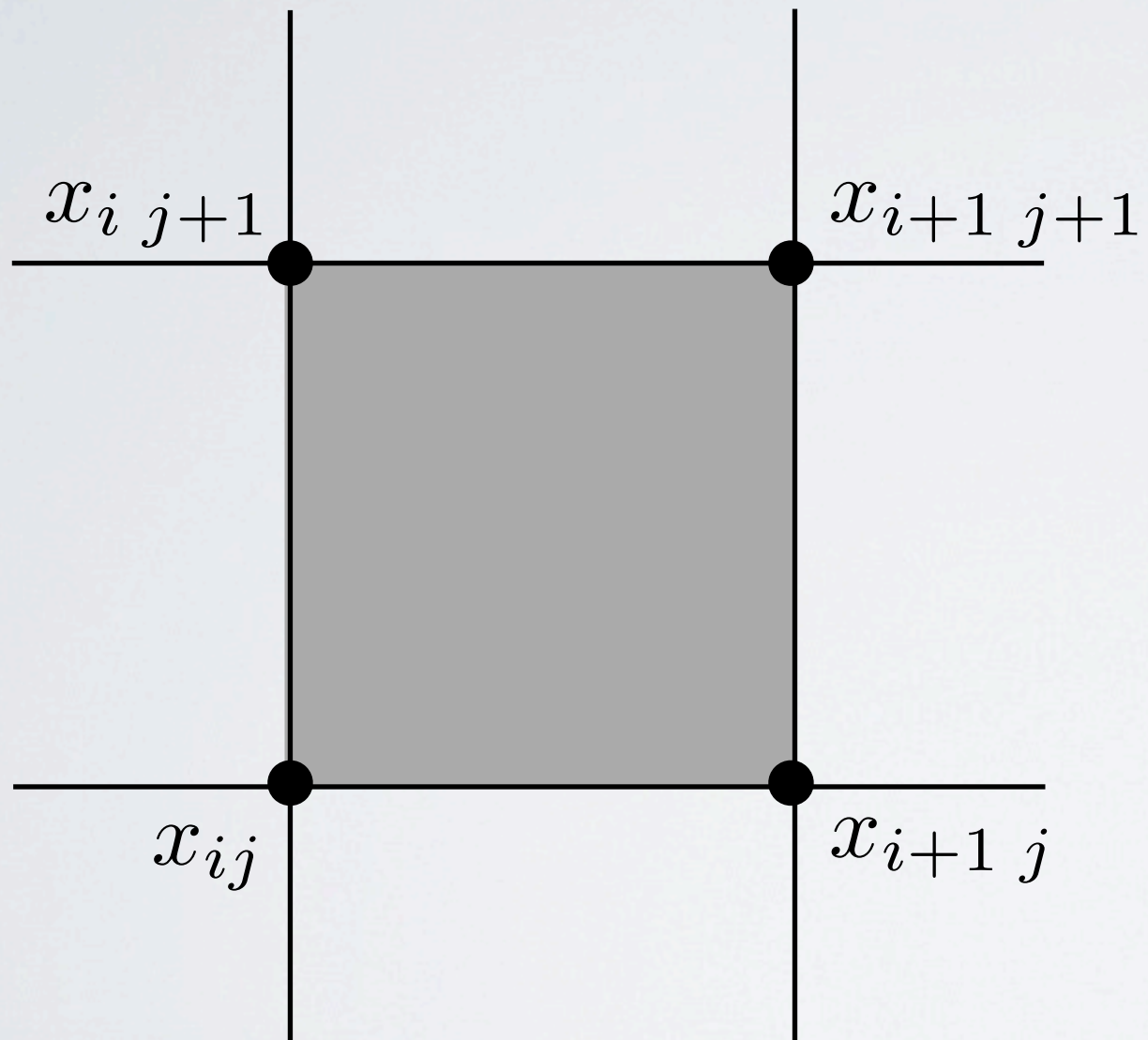


Monte Carlo to determine Ω_c

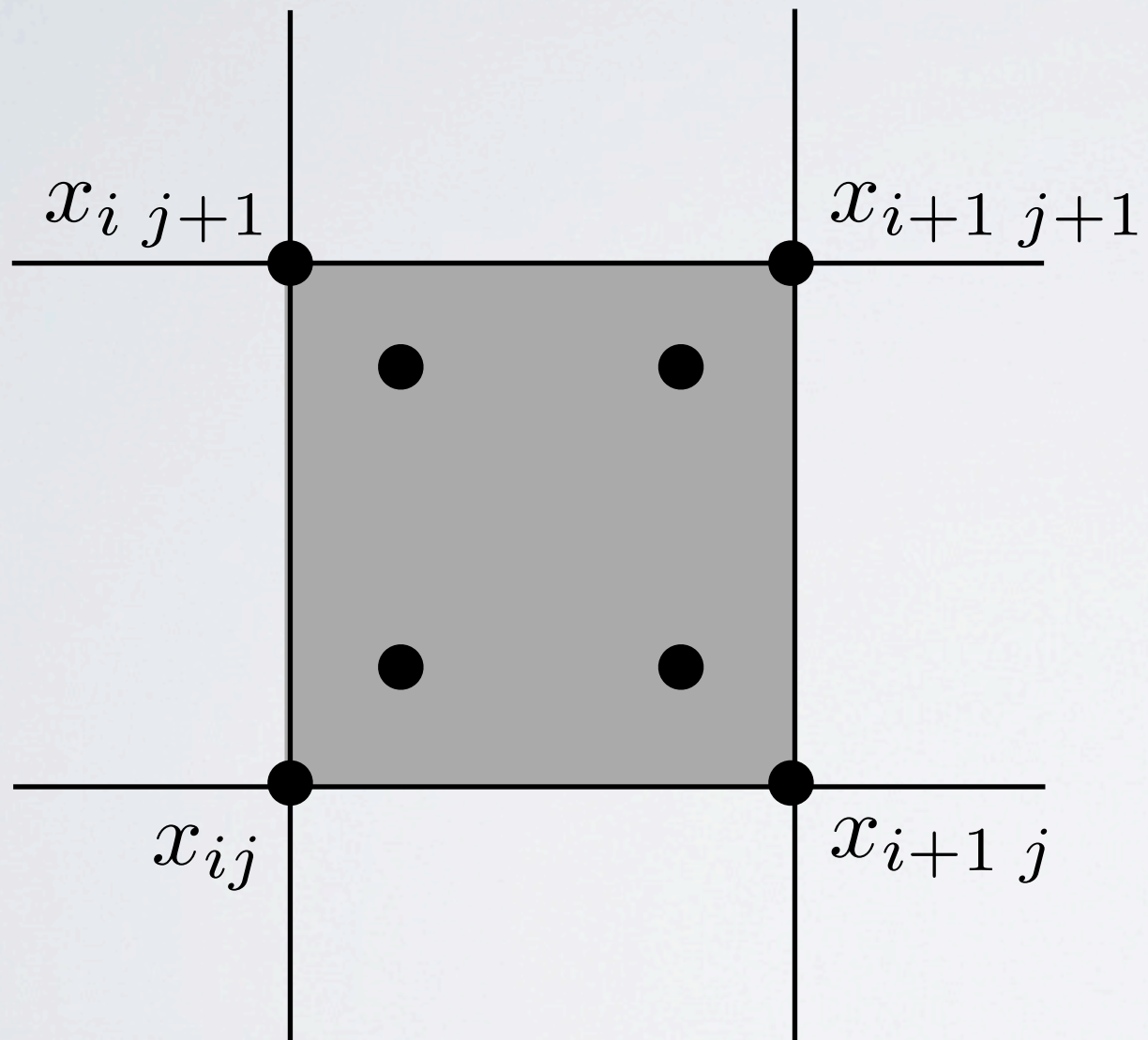
Compute 4 representative points

Ensure interior to the material

BOUNDARY CELL TREATMENT



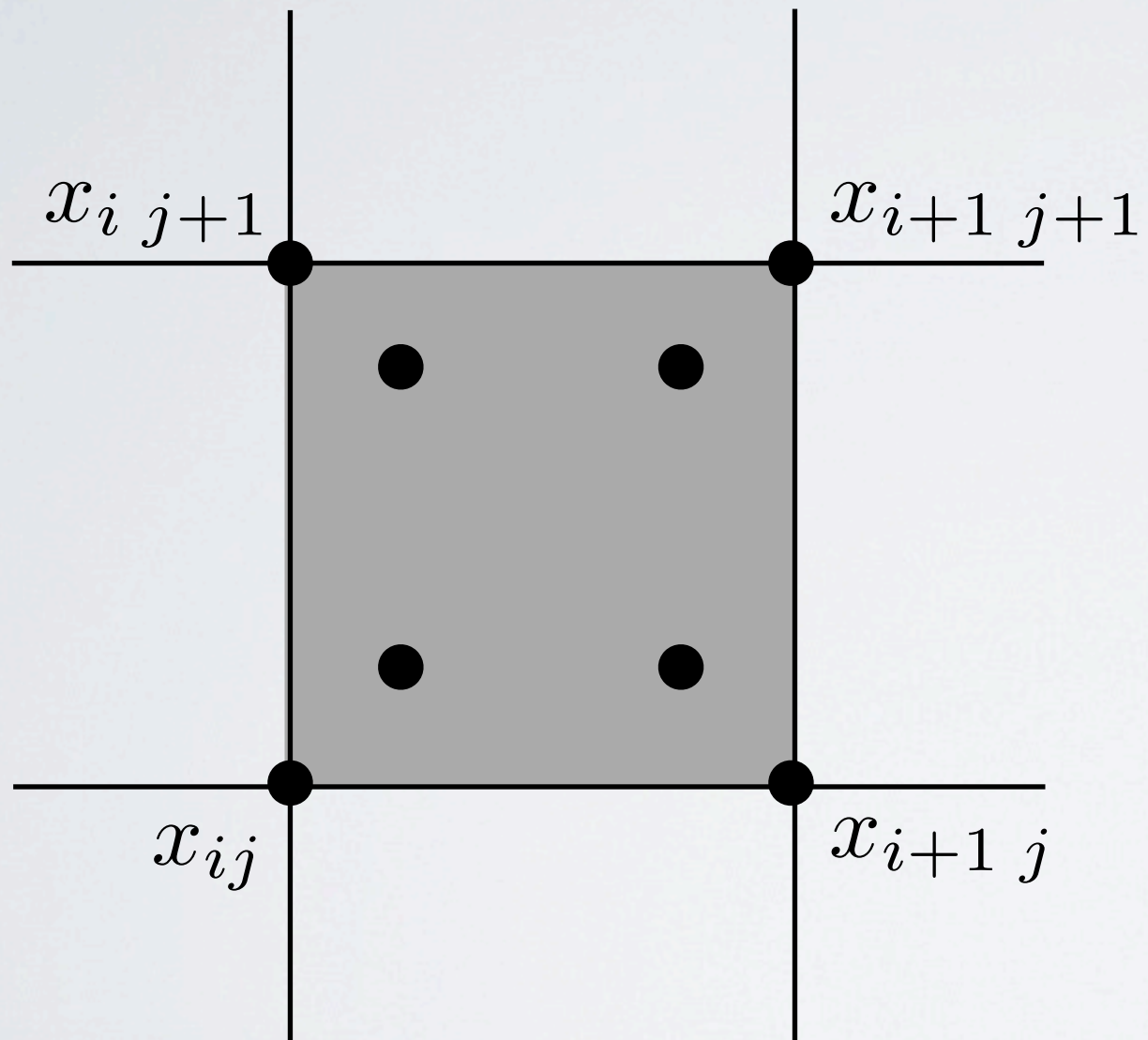
BOUNDARY CELL TREATMENT



Identical positions

Identical weights

BOUNDARY CELL TREATMENT

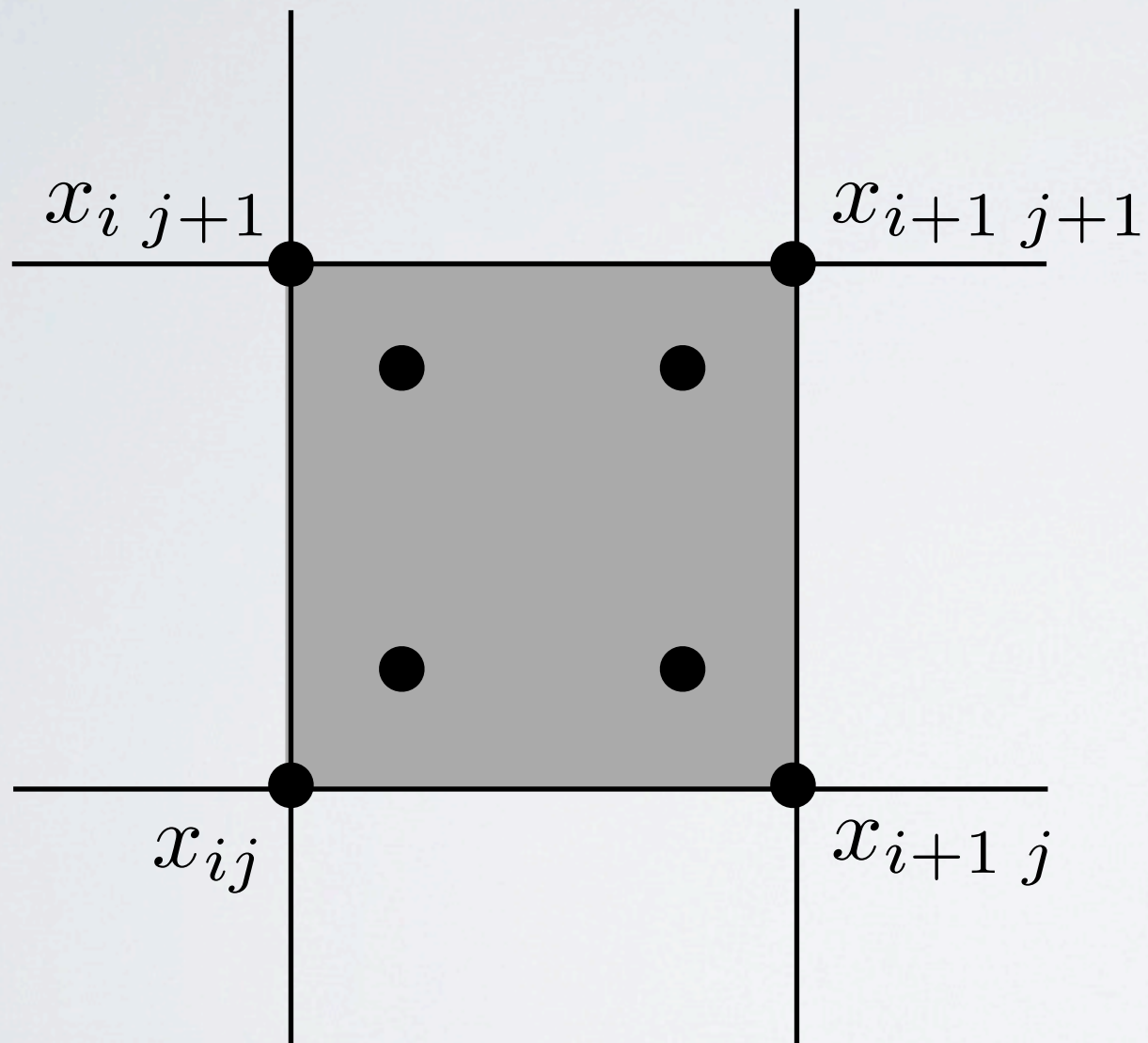


Identical positions

Identical weights

Preprocessing procedure
done once for all cells

BOUNDARY CELL TREATMENT



Identical positions

Identical weights

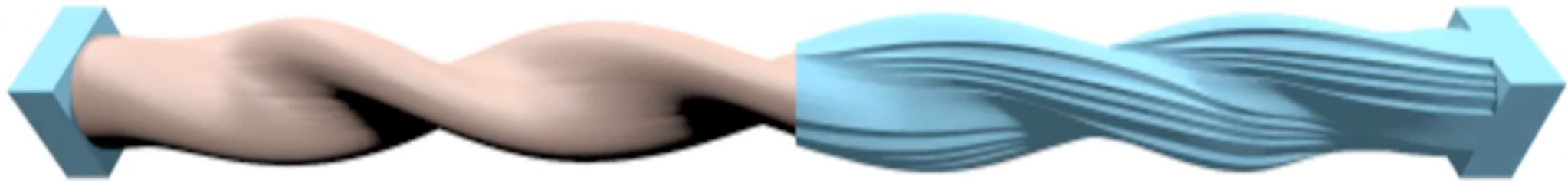
Preprocessing procedure
done once for all cells

Same data for all cells

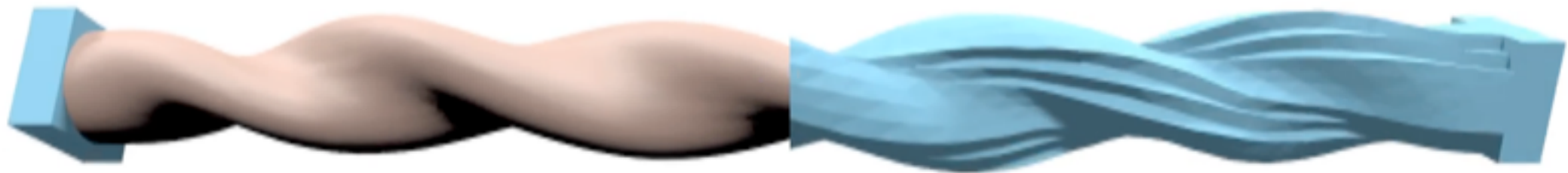
Reference Simulation (16×16)

Boundary Cells Treated with Our Method (8×8)

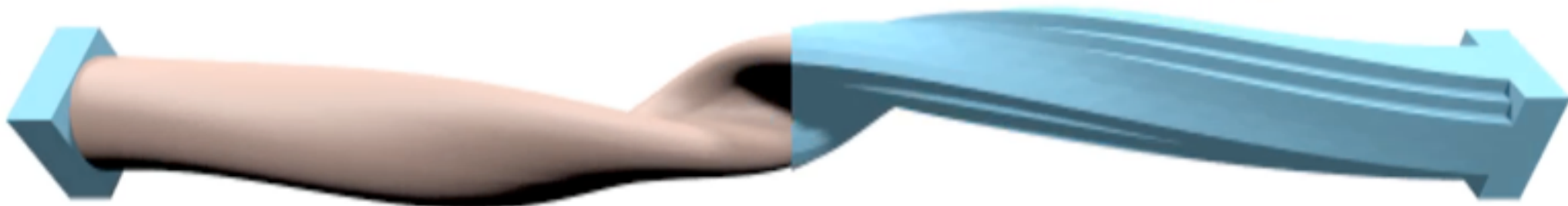
Boundary Cells as Full Cells (8×8)



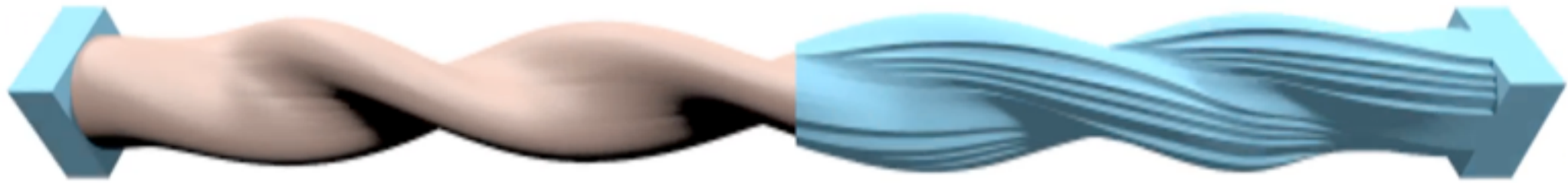
Reference Simulation (16×16)



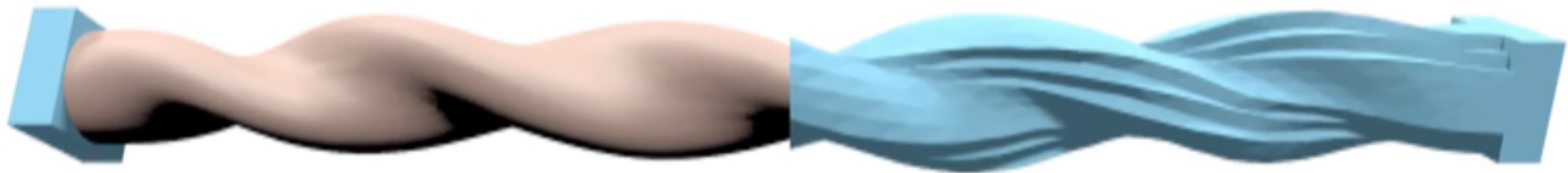
Boundary Cells Treated with Our Method (8×8)



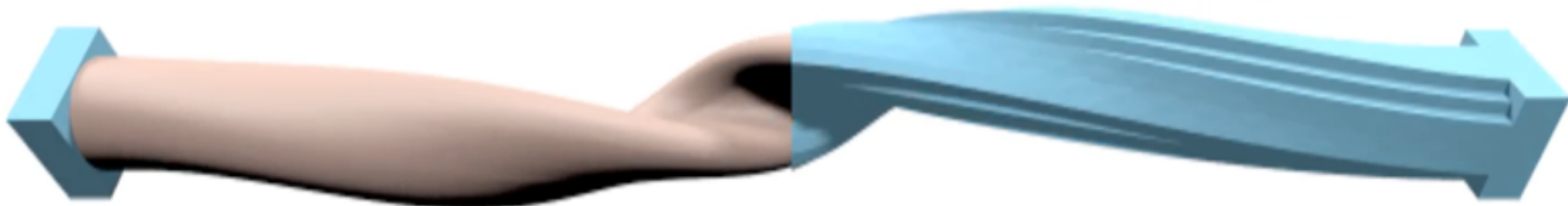
Boundary Cells as Full Cells (8×8)



Reference Simulation (16×16)



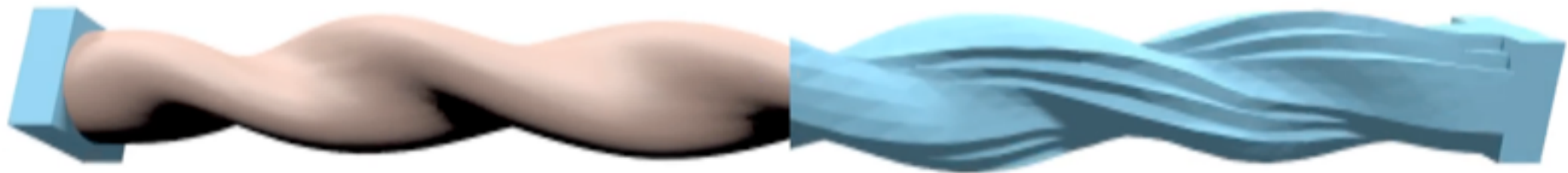
Boundary Cells Treated with Our Method (8×8)



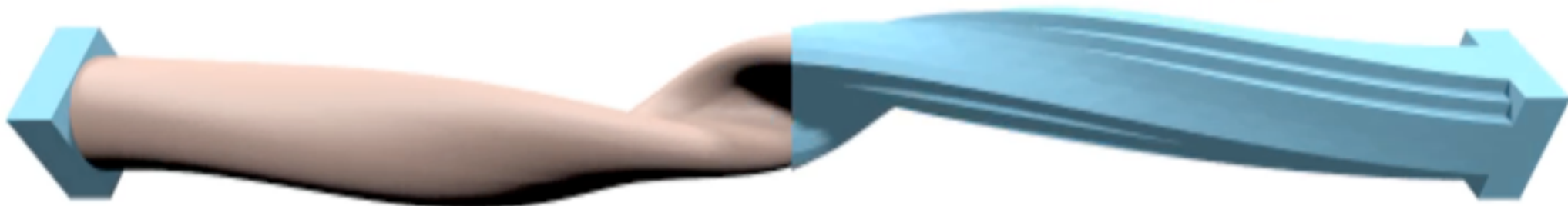
Boundary Cells as Full Cells (8×8)



Reference Simulation (16×16)

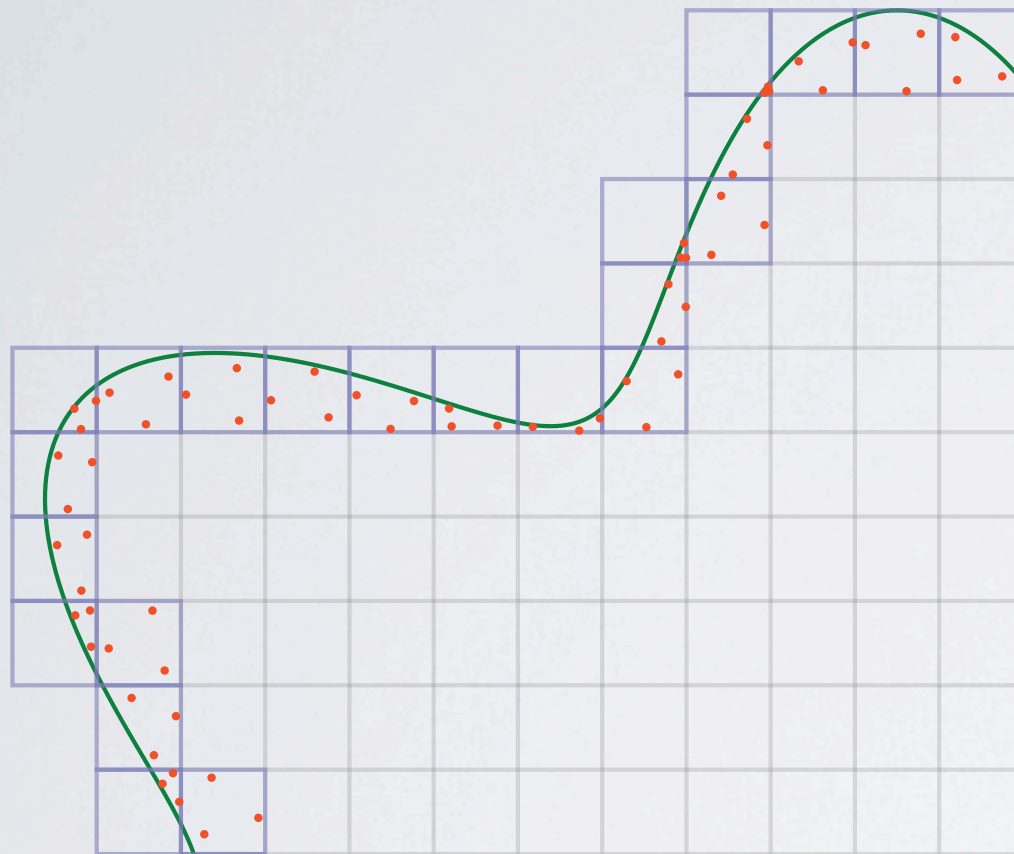


Boundary Cells Treated with Our Method (8×8)

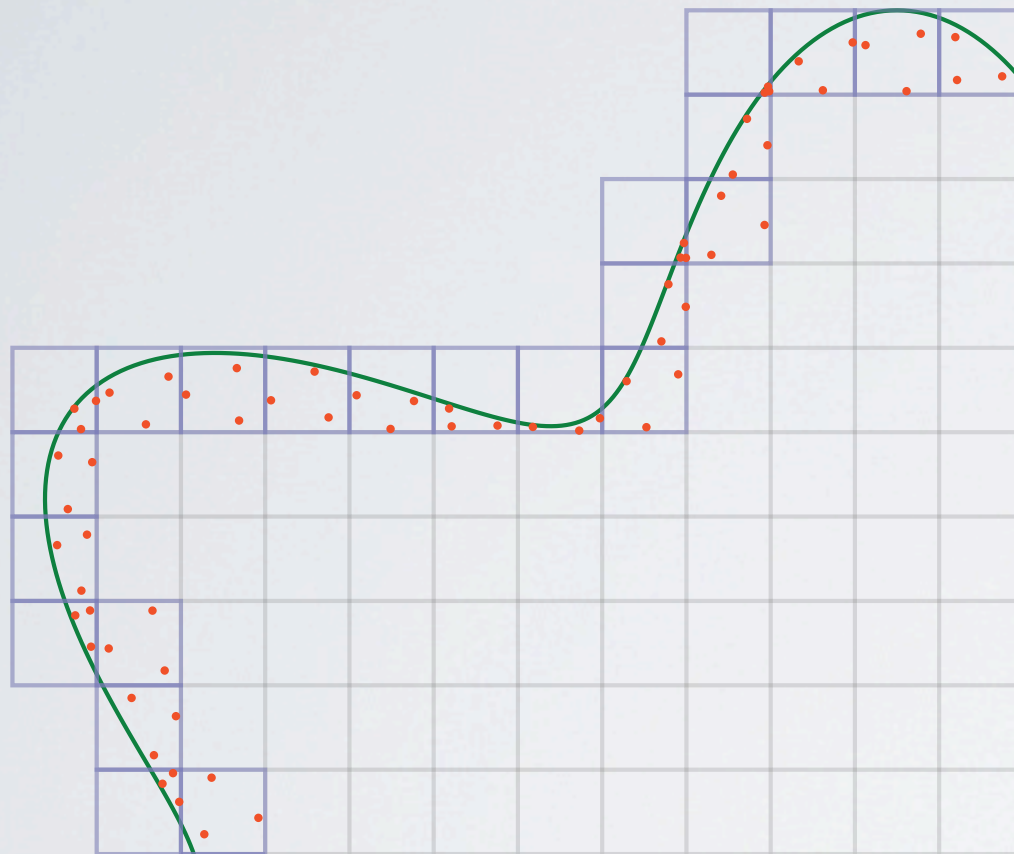


Boundary Cells as Full Cells (8×8)

Boundary Cell Treatment: Recap

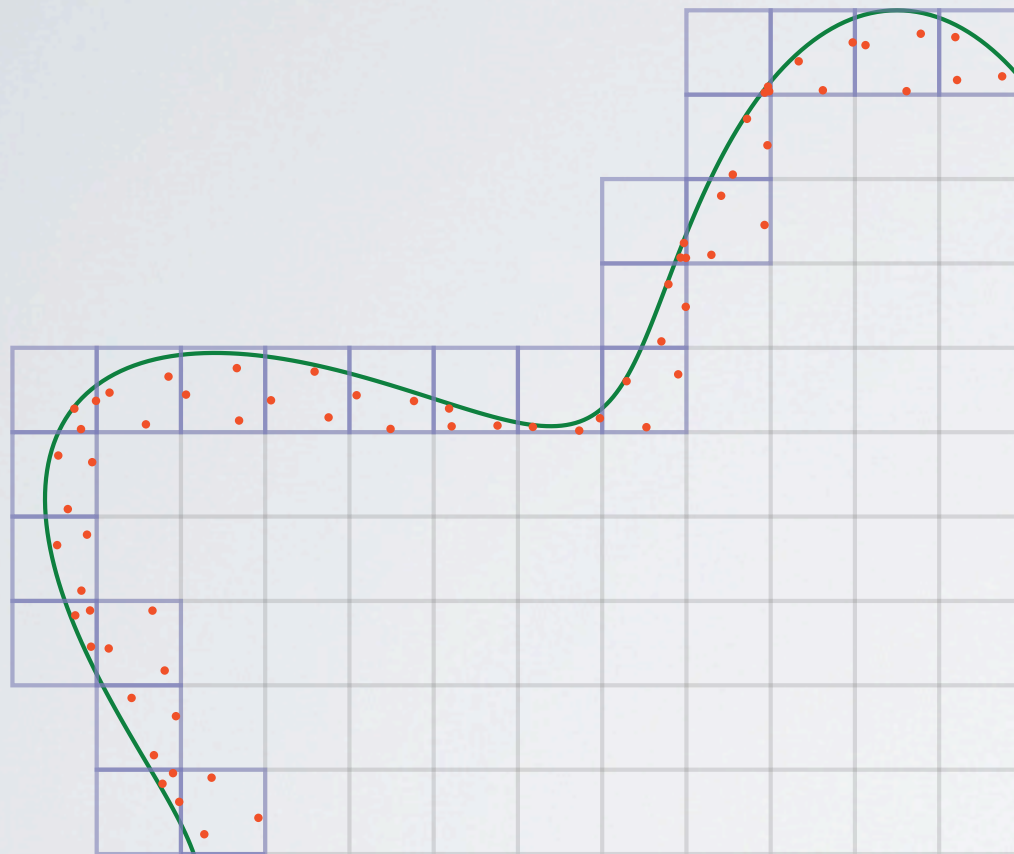


Boundary Cell Treatment: Recap



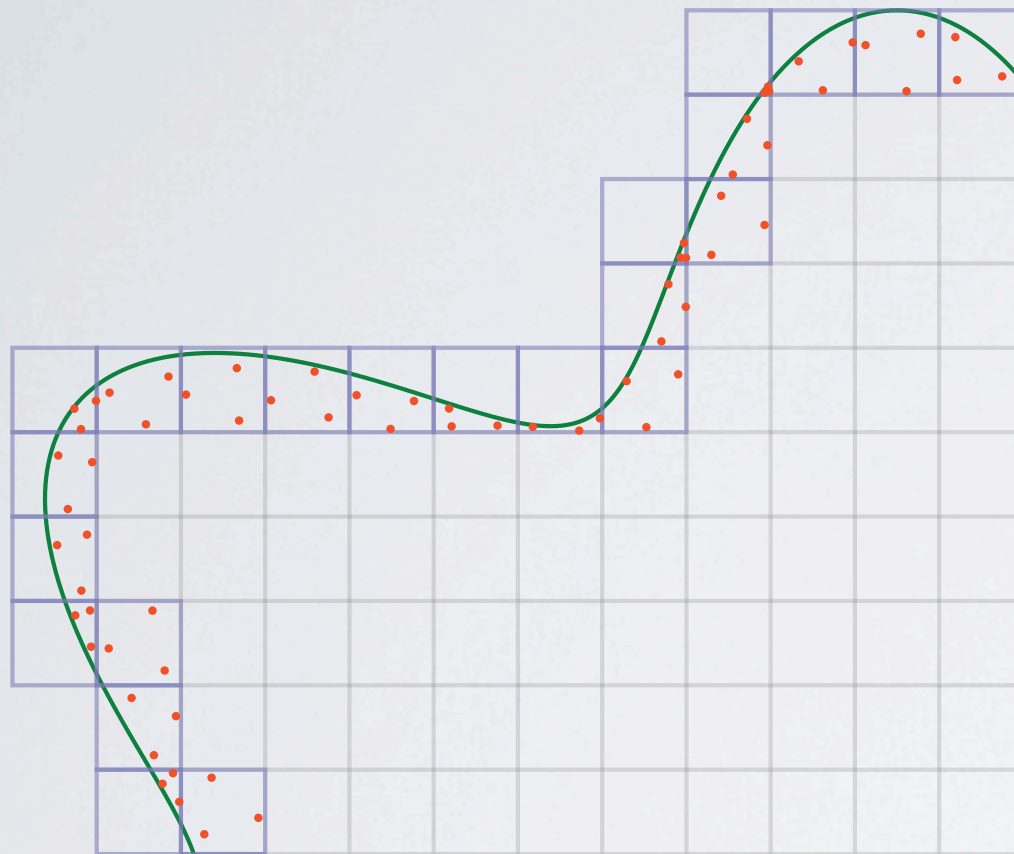
✓ Produces 2nd order accuracy

Boundary Cell Treatment: Recap



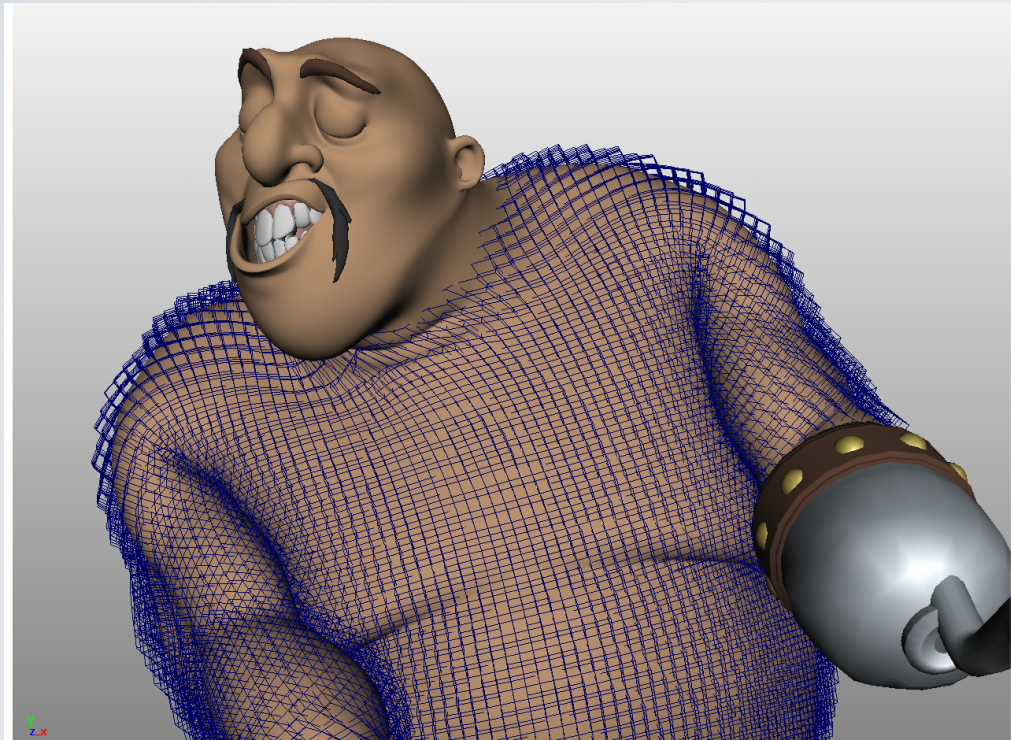
- ✓ Produces 2nd order accuracy
- ✓ Fixed work per cell (4 pts max)

Boundary Cell Treatment: Recap



- ✓ Produces 2nd order accuracy
- ✓ Fixed work per cell (4 pts max)
- ✗ Need to compute 4 sets of forces

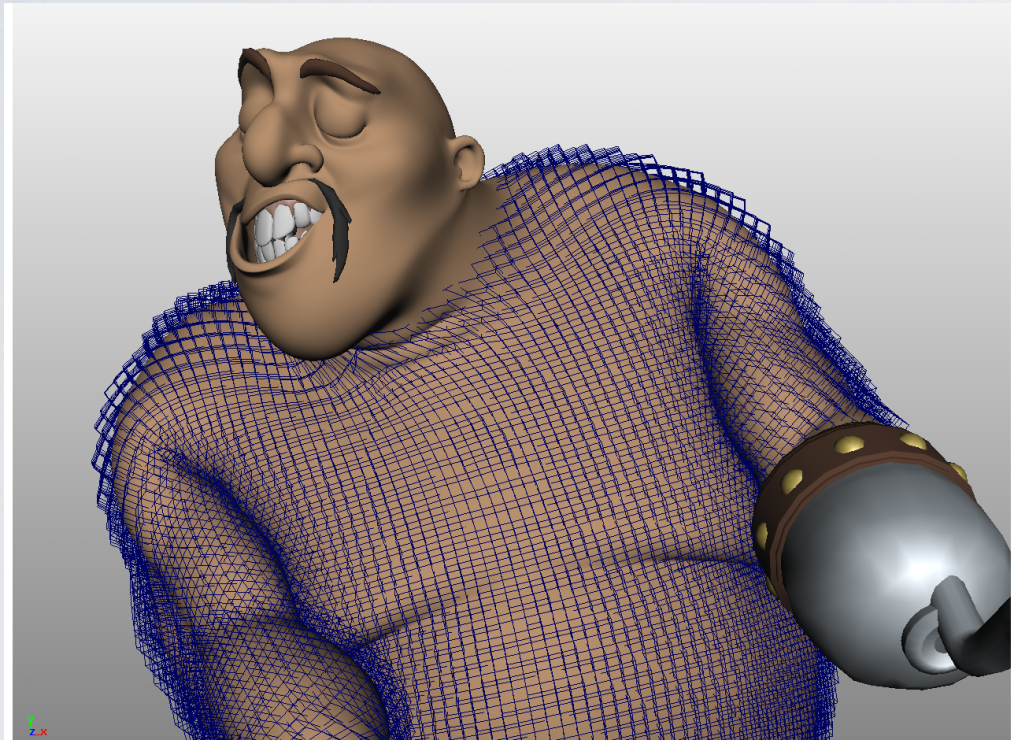
Alternative



[McAdams, et al. 2011]

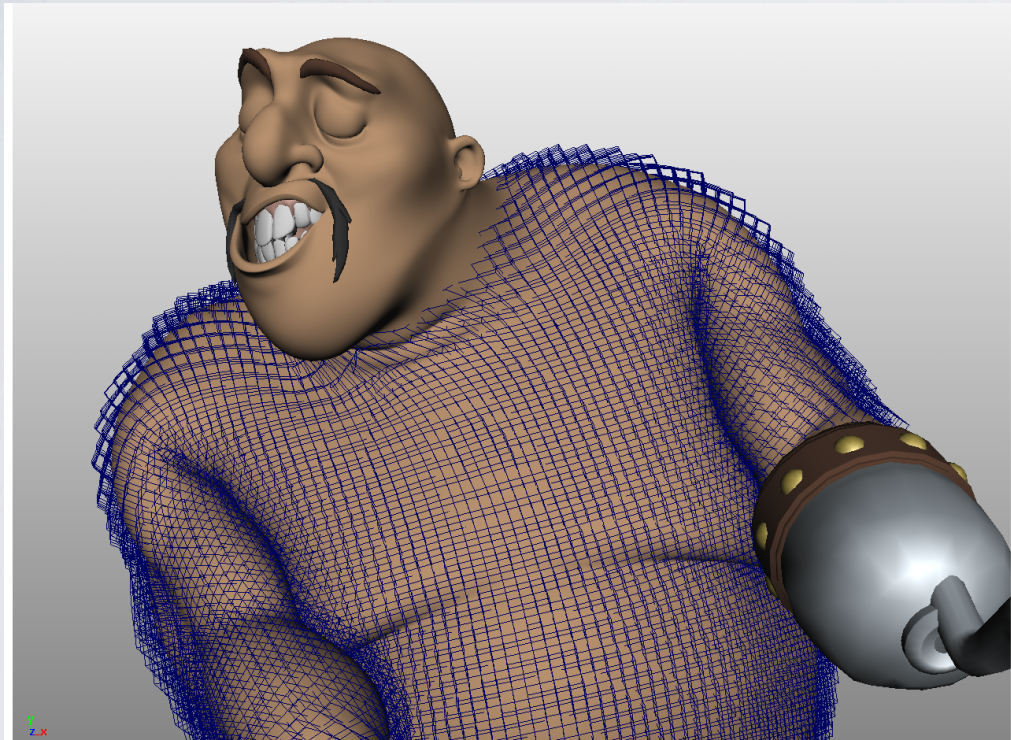
Alternative

✓ Uses whole cells



[McAdams, et al. 2011]

Alternative

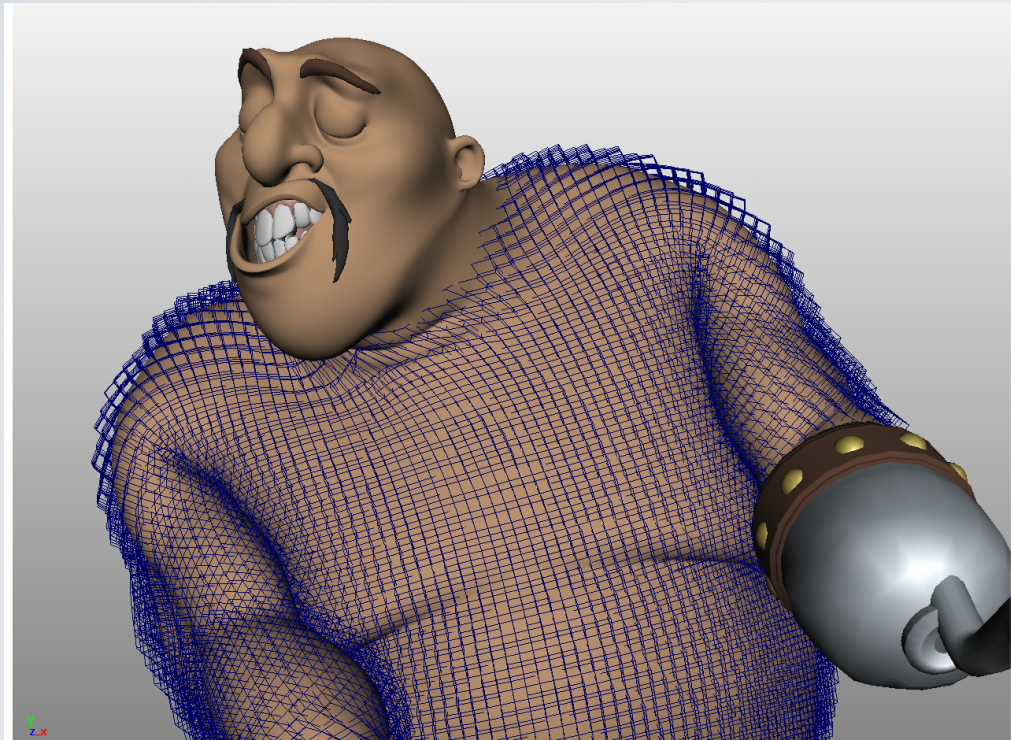


[McAdams, et al. 2011]

✓ Uses whole cells

✗ Less accurate

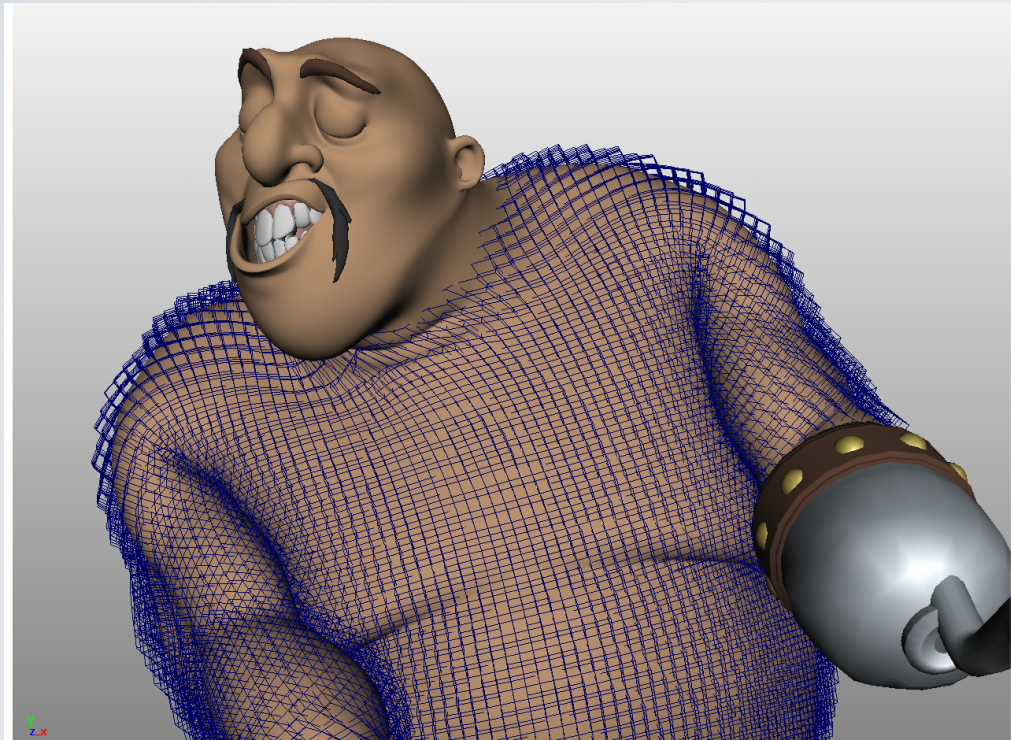
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- ✓ Uses whole cells
- ✗ Less accurate
- ✓ Stabilization allows 1-pt evaluation

Alternative



[McAdams, et al. 2011]

✓ Uses whole cells

✗ Less accurate

✓ Stabilization allows 1-pt evaluation

We extended this to arbitrary materials

SOLVING THE SYSTEM

Start with Energy Density



Apply Incompressibility Adjustment



Compute Discrete Energy \hat{E}



Derive Nodal Forces $f(x)$



Find Equilibrium $f(x) = 0 \implies \min \hat{E}$

SOLVING THE SYSTEM

Find Equilibrium $f(x) = 0 \implies \min \hat{E}$

OBJECTIVE: SOLVE FOR $F(X) = 0$

Solve $f(x) = 0$ $\xRightarrow{\text{Newton}}$ $x_0 \leftarrow$ Initial guess

for $k = 0, 1, \dots$

$$\text{Solve } \left\{ -\frac{\delta f}{\delta x} \bigg|_{x_k} \right\} \delta x = f(x_k)$$

$$\text{Update } x_{k+1} = x_k + \delta x$$

$\Rightarrow \lim x_k =$ Sub-voxel accurate solution of
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Compute with one
point method

$$\text{Solve } \underbrace{\left\{ -\frac{\delta f}{\delta x} \bigg|_{x_k} \right\}}_{\text{Jacobian}} \delta x = f(x_k)$$

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OBJECTIVE: SOLVE FOR $F(X) = 0$

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for $k = 0, 1, \dots$

Compute with four
point method

$$\text{Solve } \left\{ -\frac{\delta f}{\delta x} \bigg|_{x_k} \right\} \delta x = \underline{f(x_k)}$$

$$\text{Update } x_{k+1} = x_k + \delta x$$

$$\Rightarrow \lim x_k = \text{Sub-voxel accurate solution of } f(x) = 0$$

FEATURES

✓ Arbitrary Materials

✓ Incompressibility

✓ Sub-voxel Precision

Robust

Parallelism

FEATURES

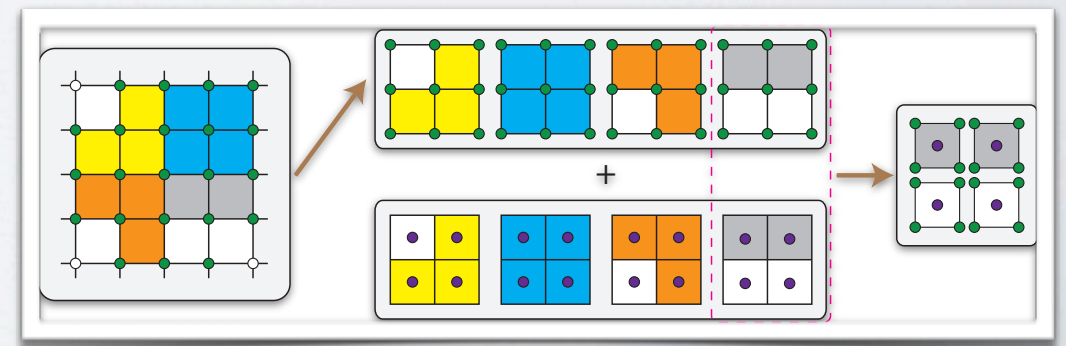
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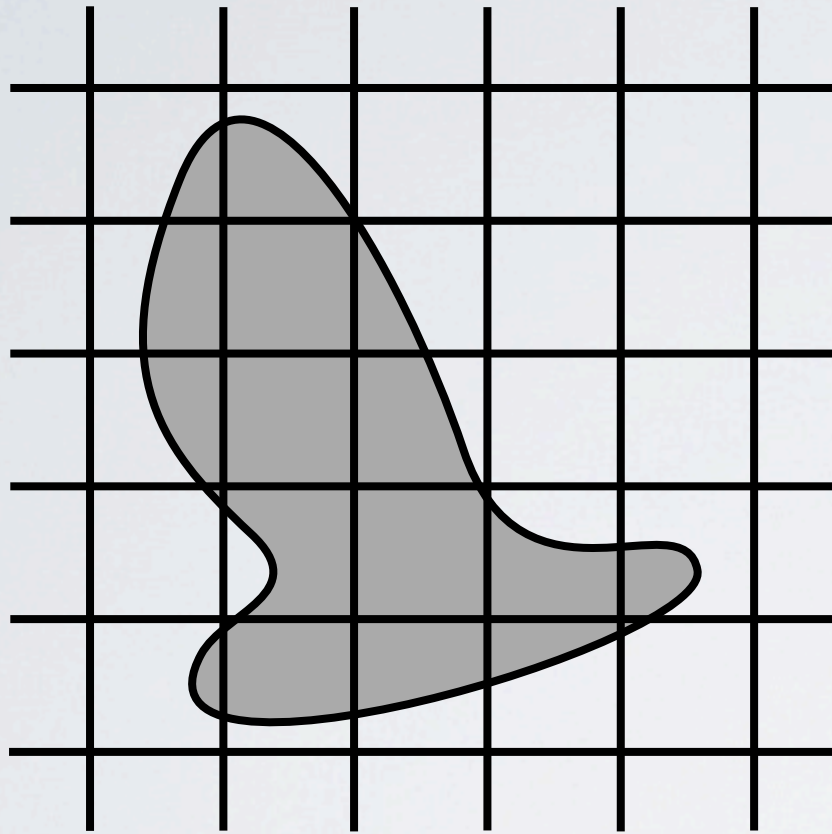
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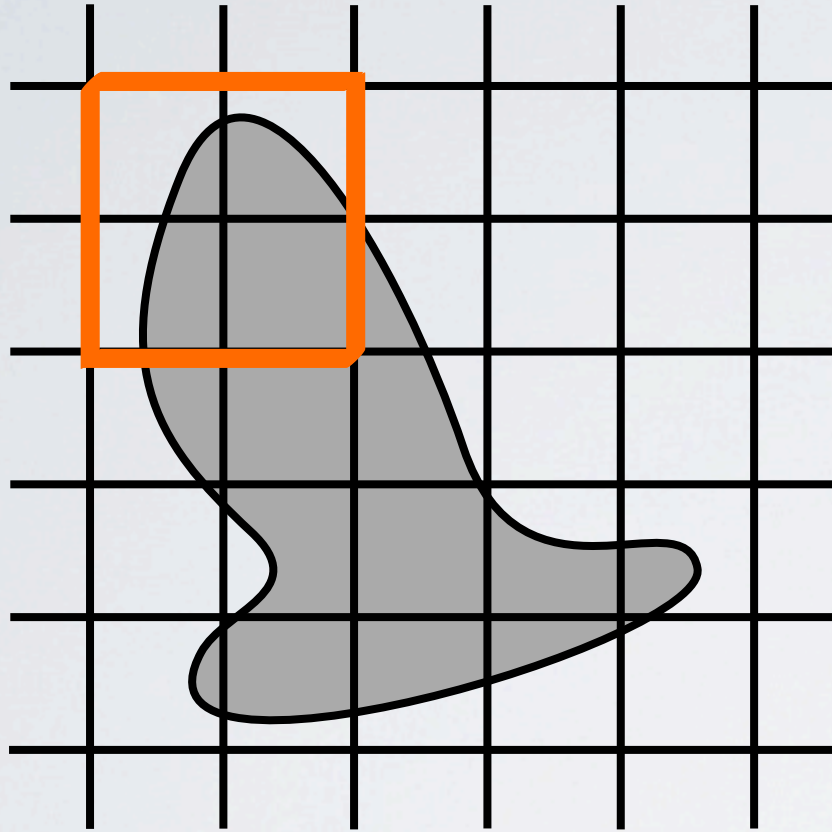
Parallelism



Parallelism



Parallelism

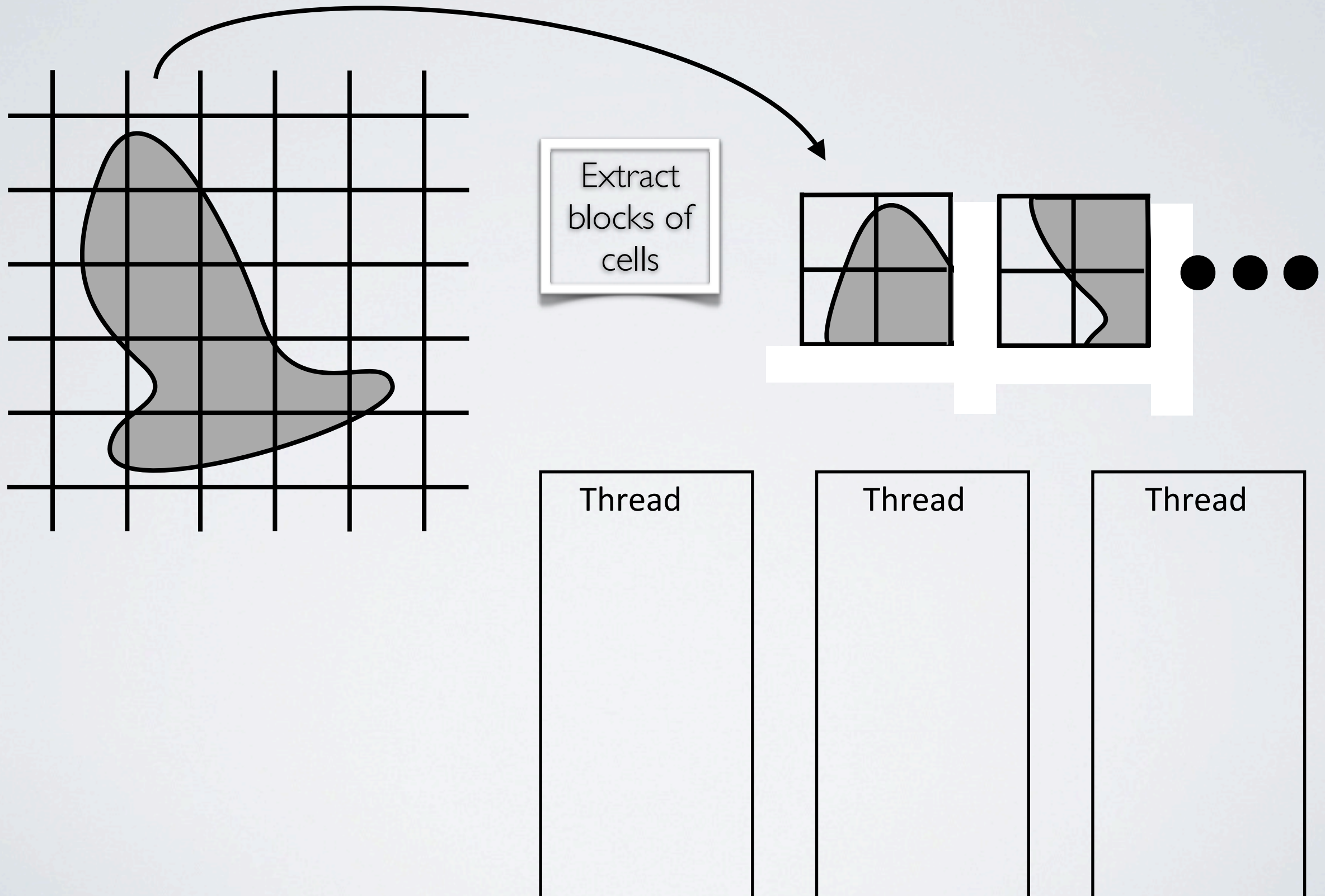


Thread

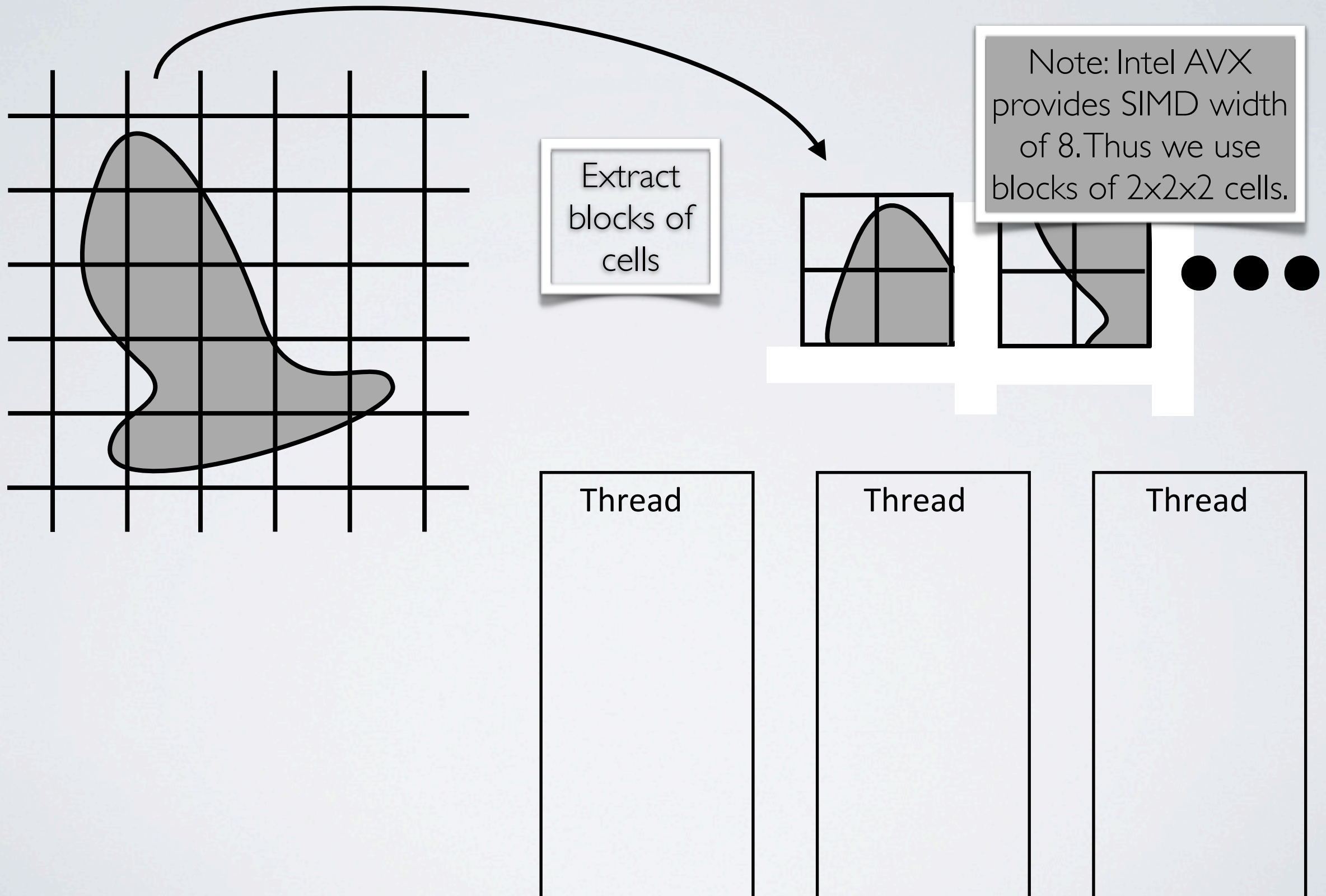
Thread

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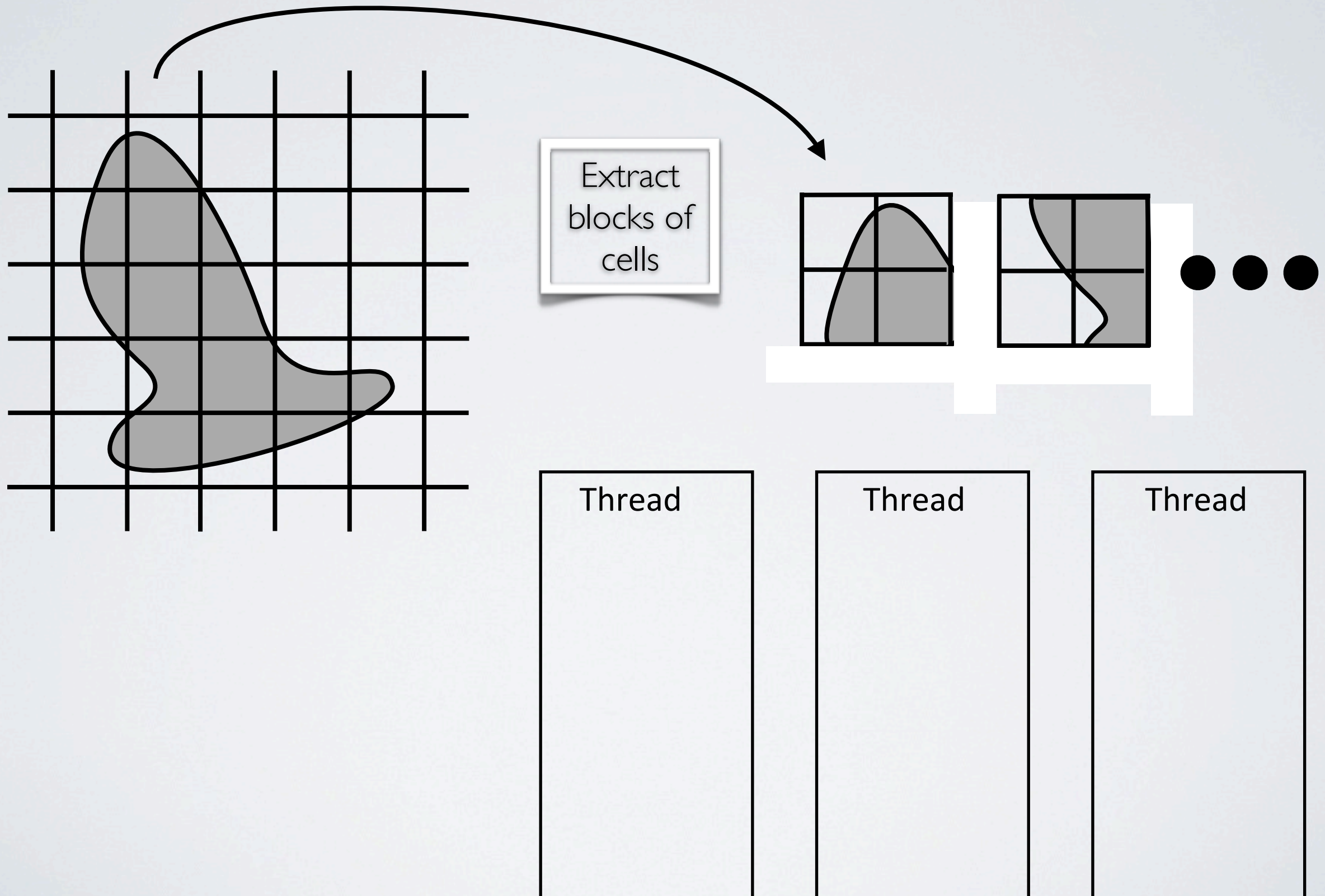
Parallelism



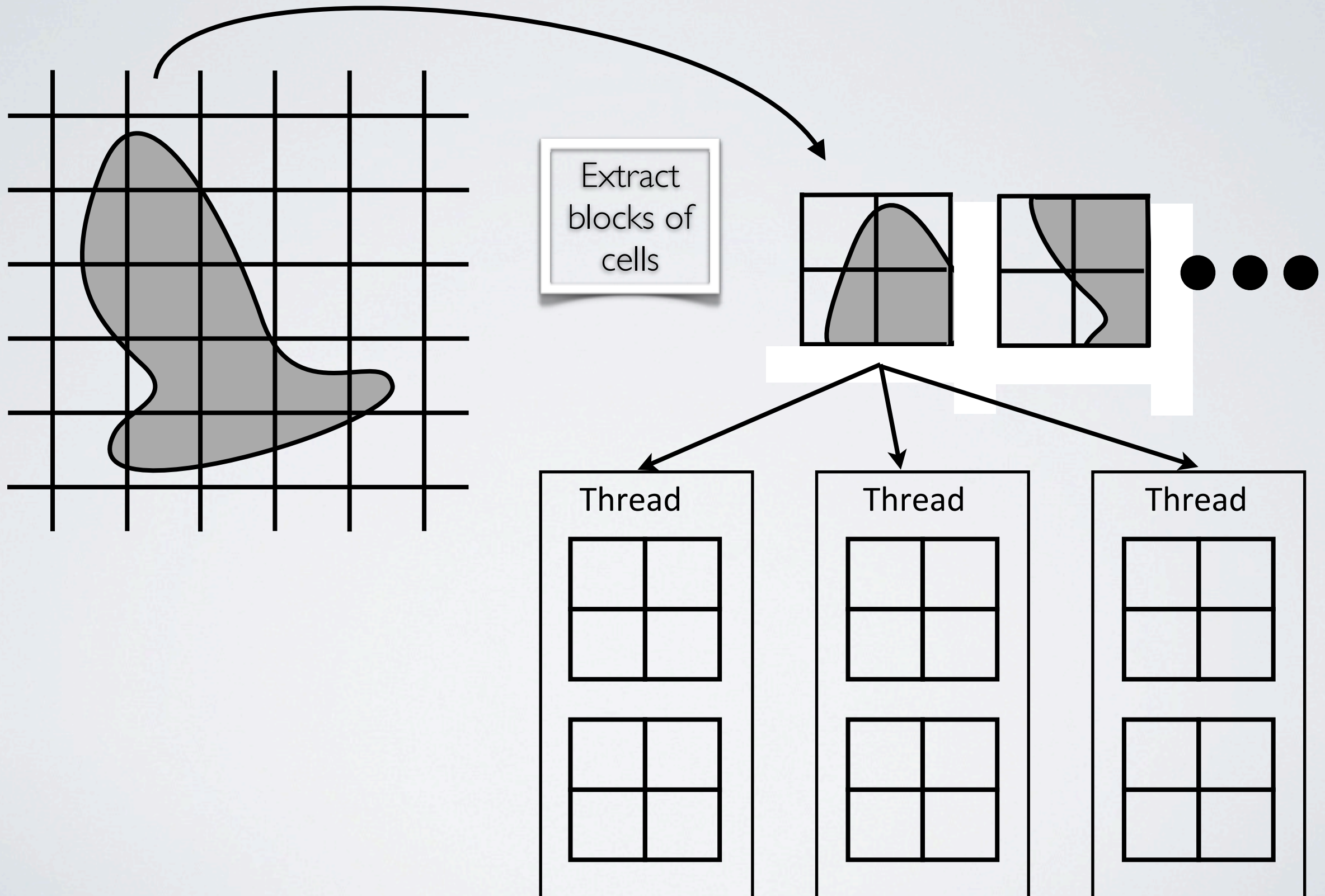
Parallelism



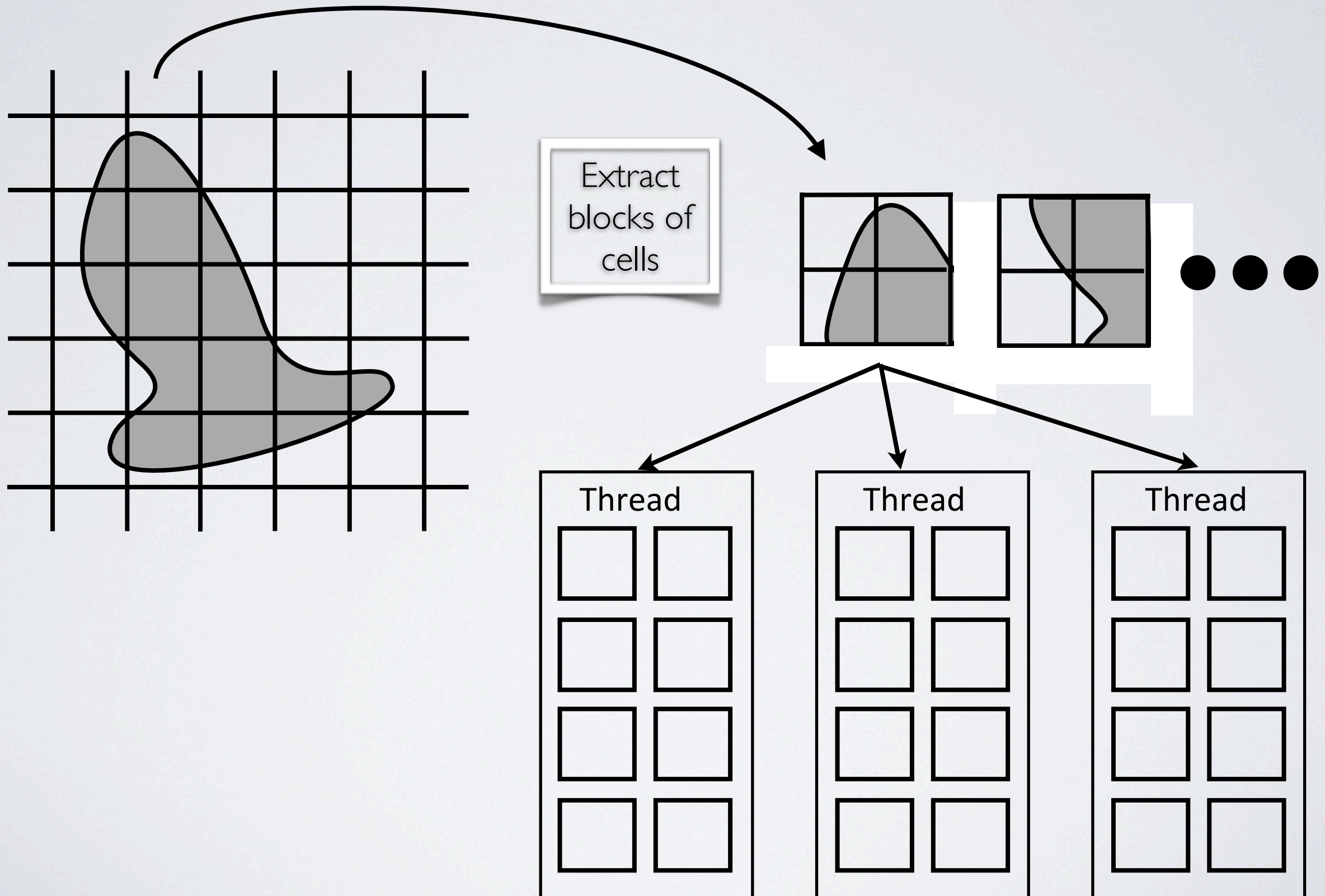
Parallelism



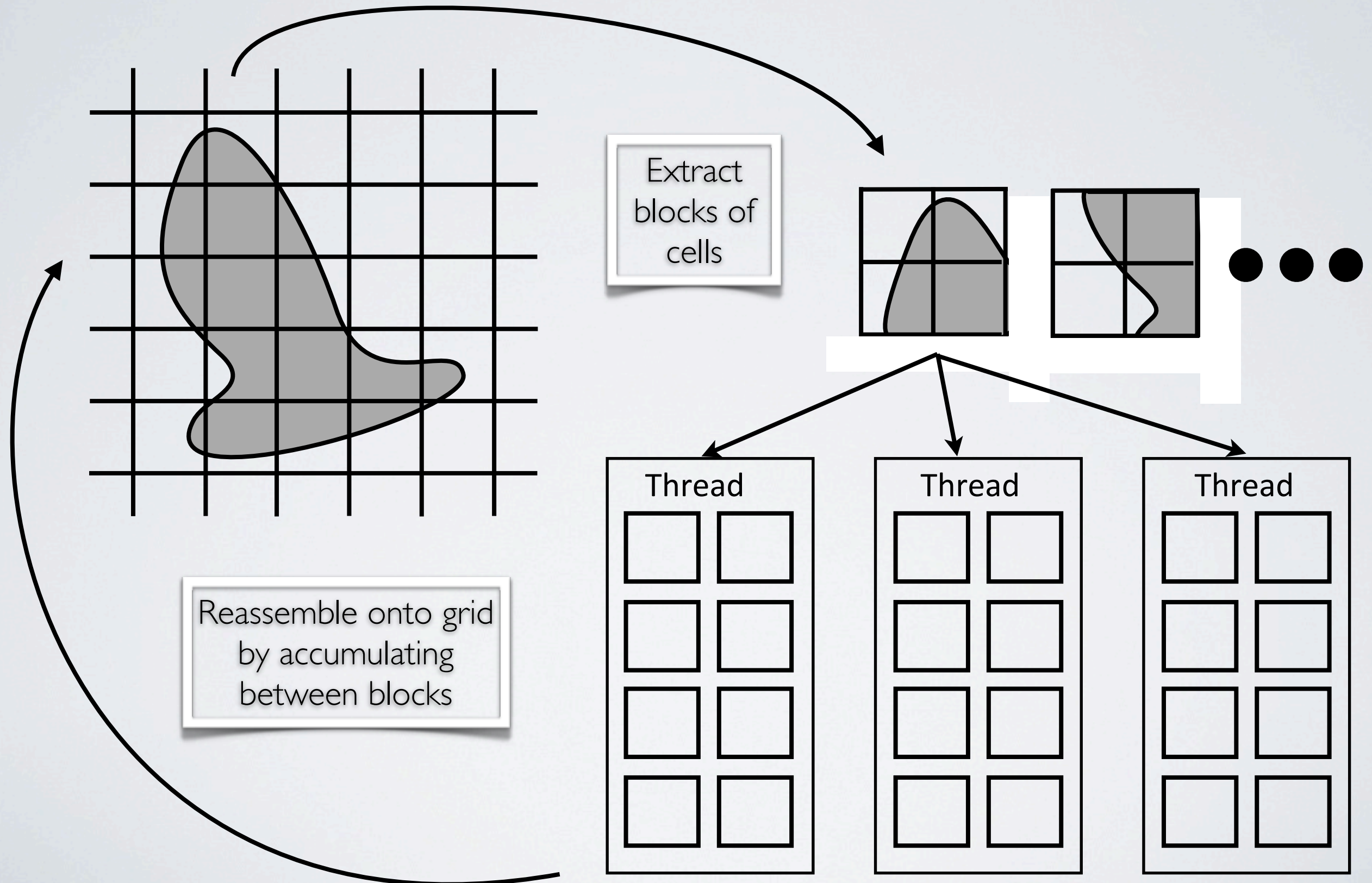
Parallelism



Parallelism



Parallelism



PERFORMANCE

		1 core (AVX) 1 thread	2 cores (AVX) 2 threads	4 cores (AVX) 4 threads	4 cores (AVX) 8 threads
Human model (101K cells)	Force Differentials	0.041	0.023	0.015	0.015
	One QMR Iteration	0.067	0.037	0.025	0.024
	Newton Iteration (including 100 QMR iterations)	7.035	4.066	2.727	2.645
	Typical frame (4-6 Newton iterations)	31.825	18.186	12.193	11.919
Human model (13.5K cells)	Force Differentials	0.005	0.003	0.002	0.002
	One QMR Iteration	0.007	0.005	0.003	0.003
	Newton Iteration (including 50 QMR iterations)	0.422	0.244	0.184	0.177
	Typical frame (3-5 Newton iterations)	1.466	0.842	0.640	0.626

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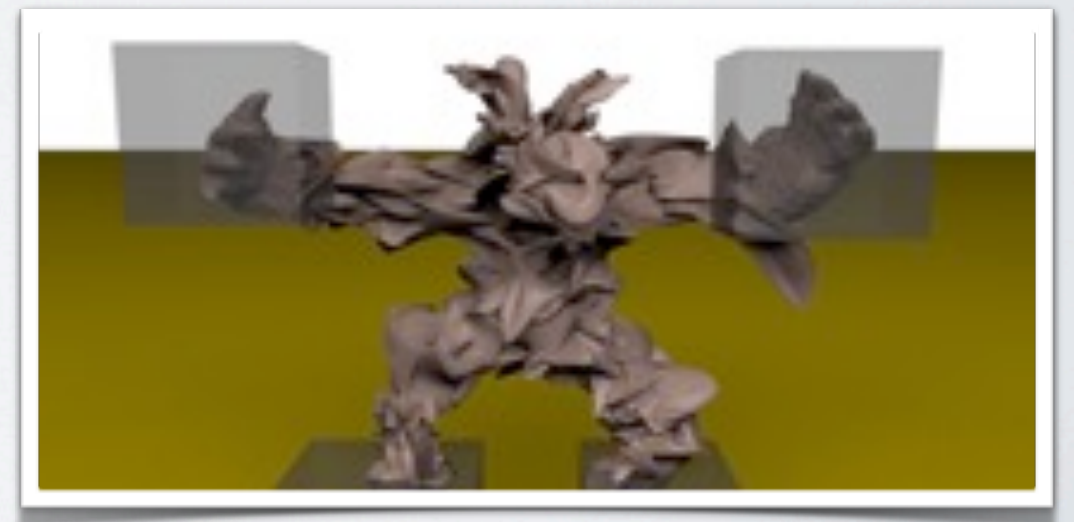
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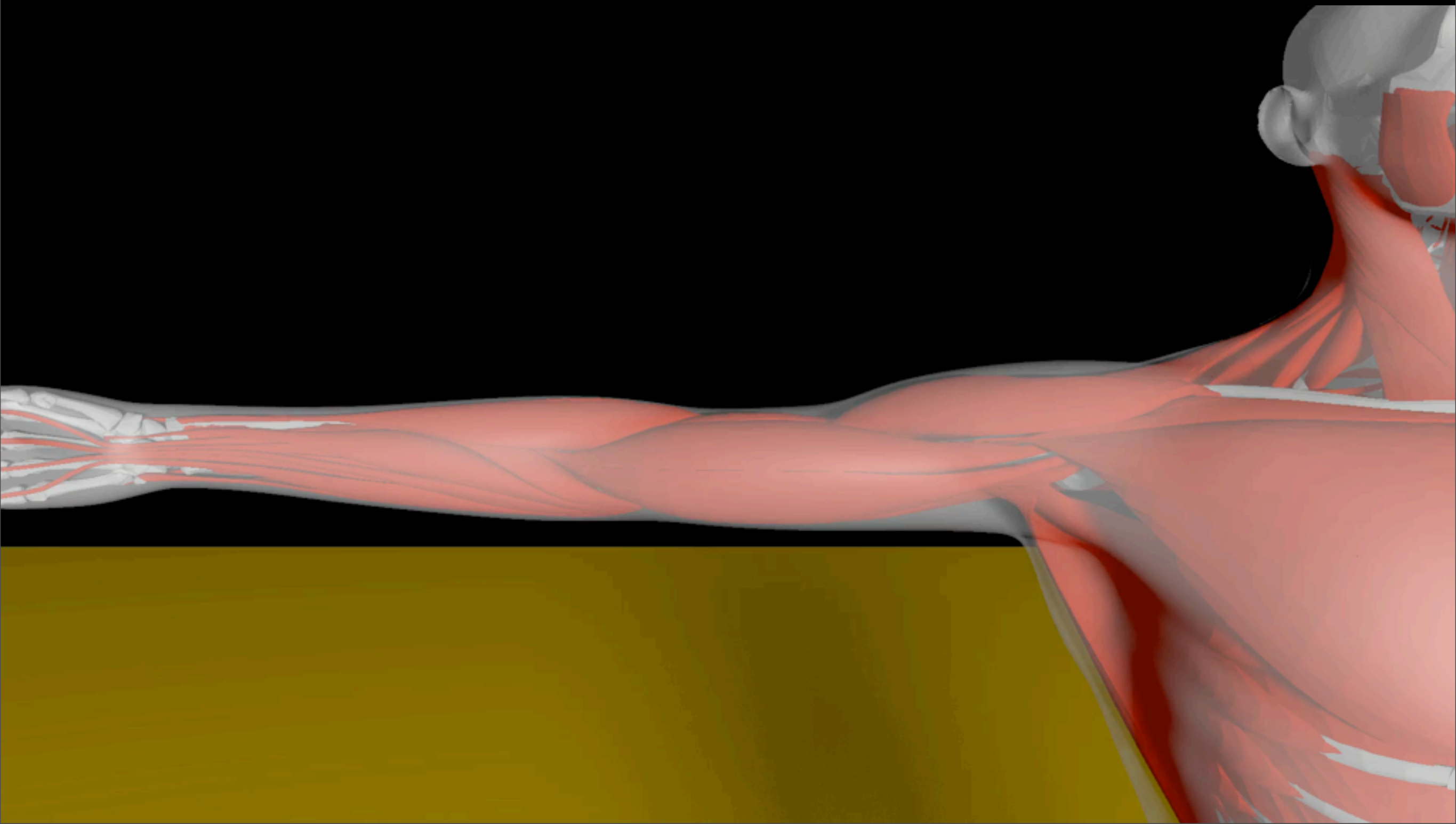
ROBUSTNESS

ROBUSTNESS

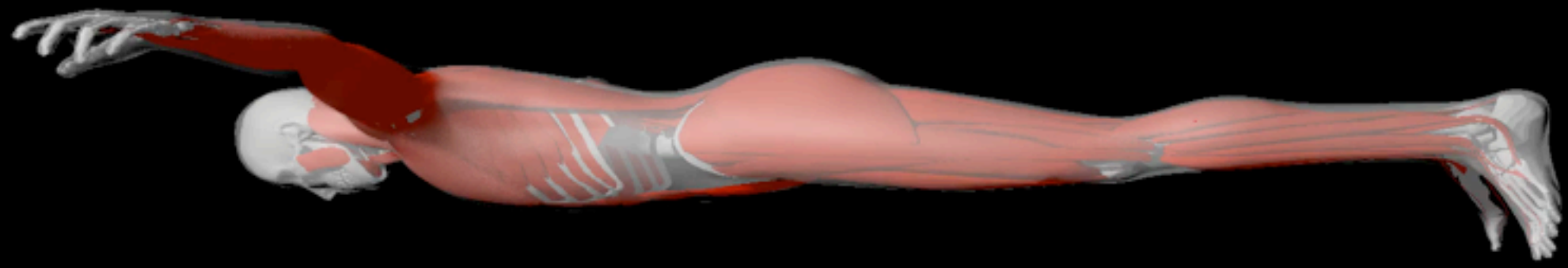












CONCLUSION OF COMPLETED WORK

Arbitrary Materials

Incompressibility

Sub-voxel Precision

Robust

Parallelism

CONCLUSION OF COMPLETED WORK

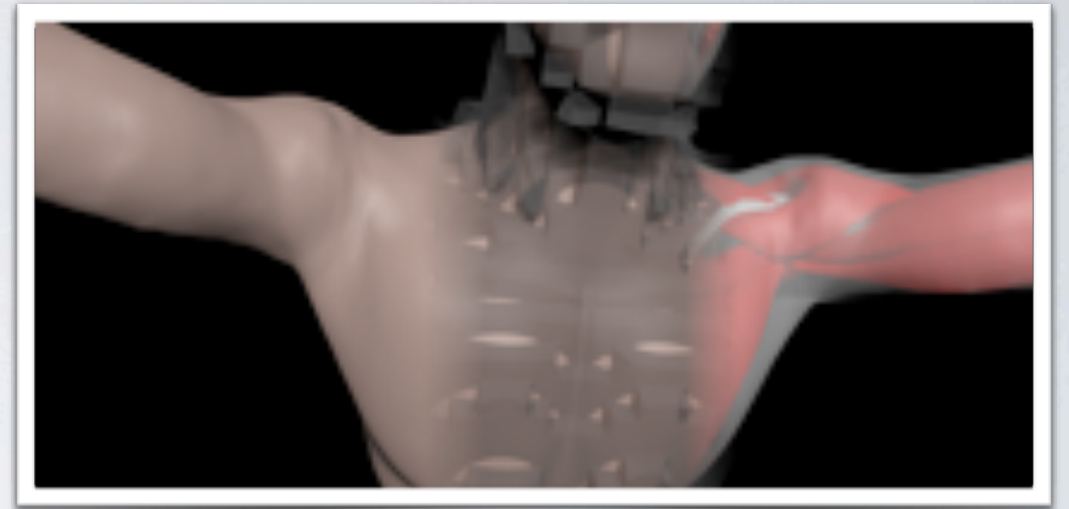
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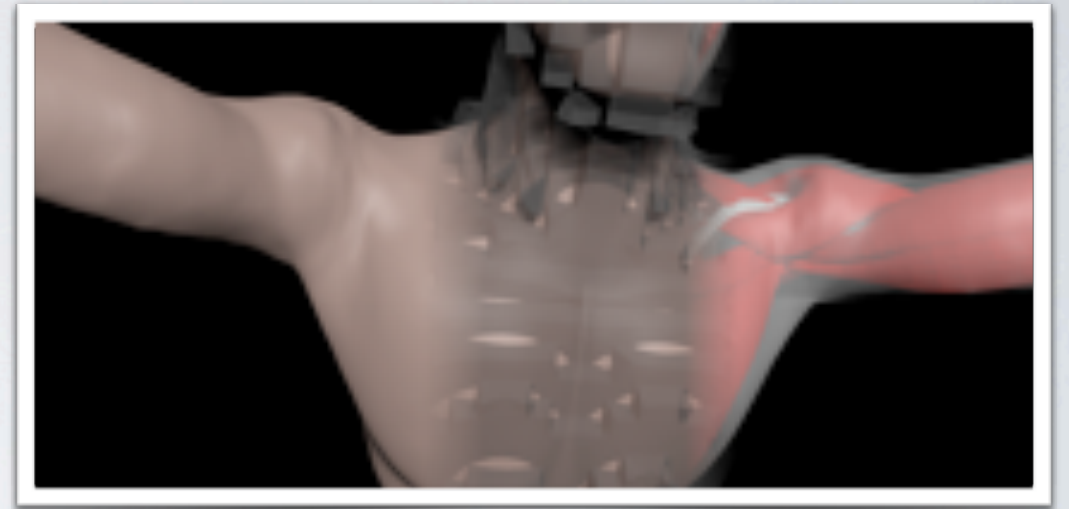
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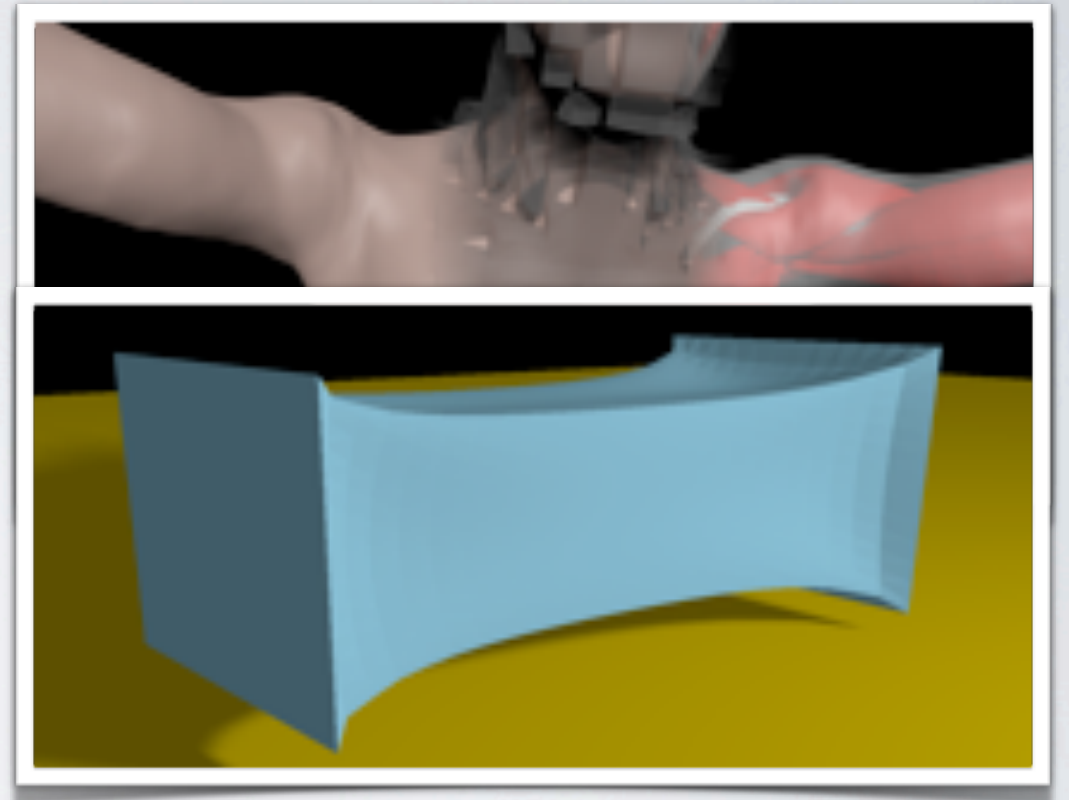
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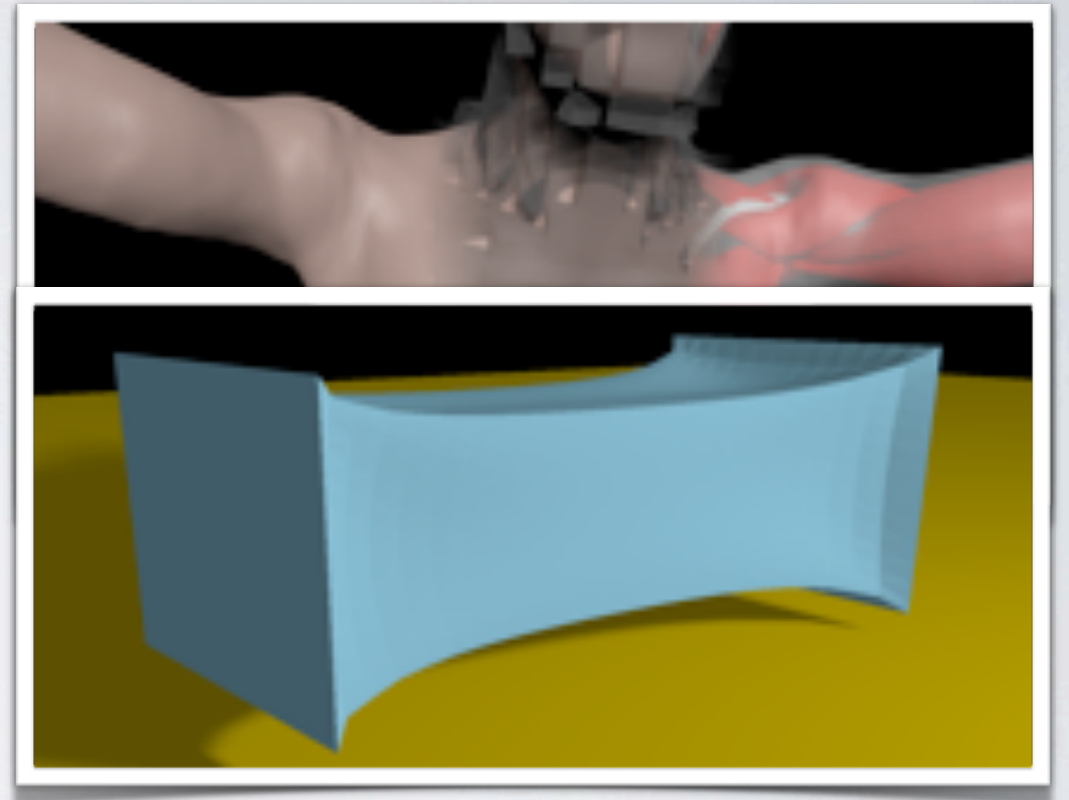
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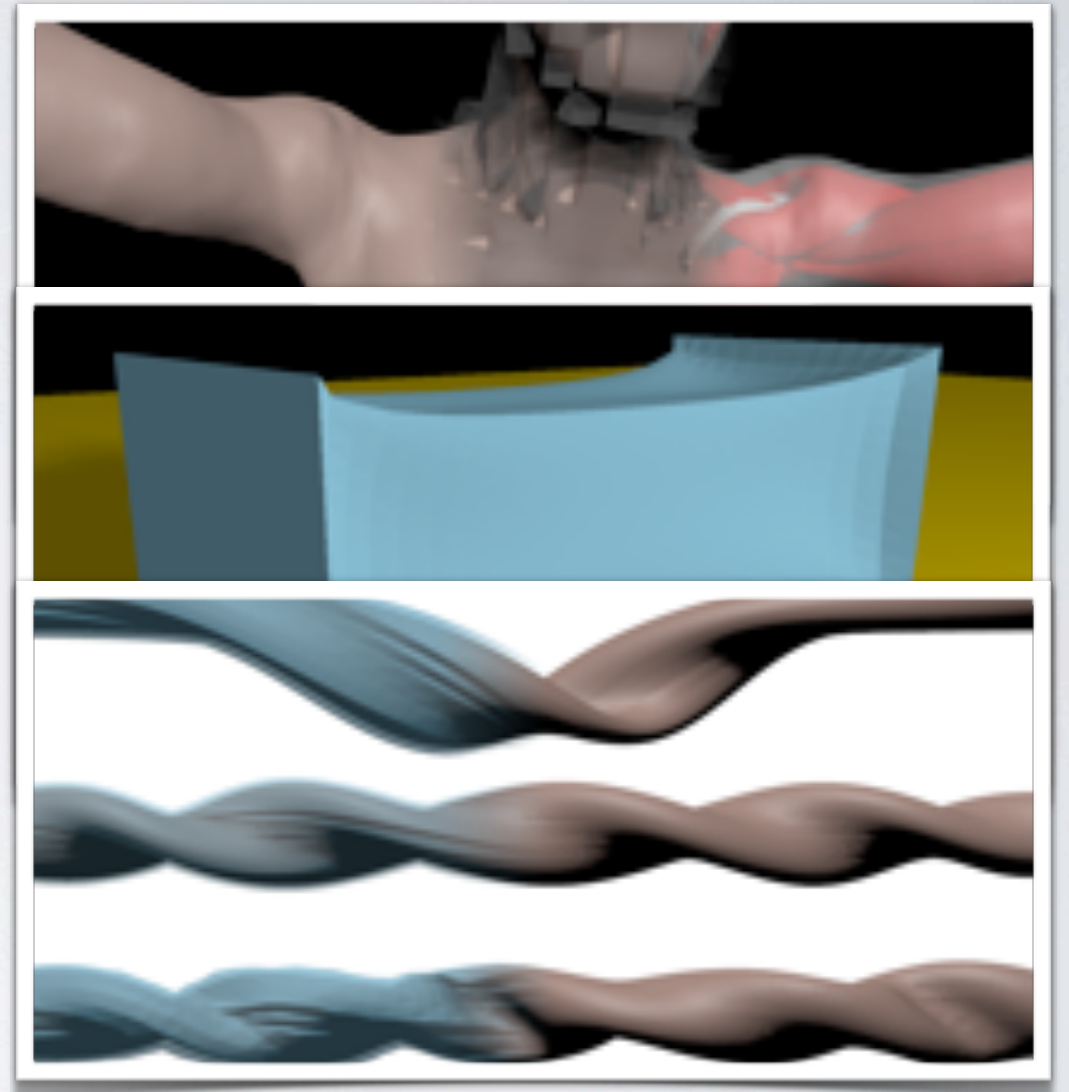
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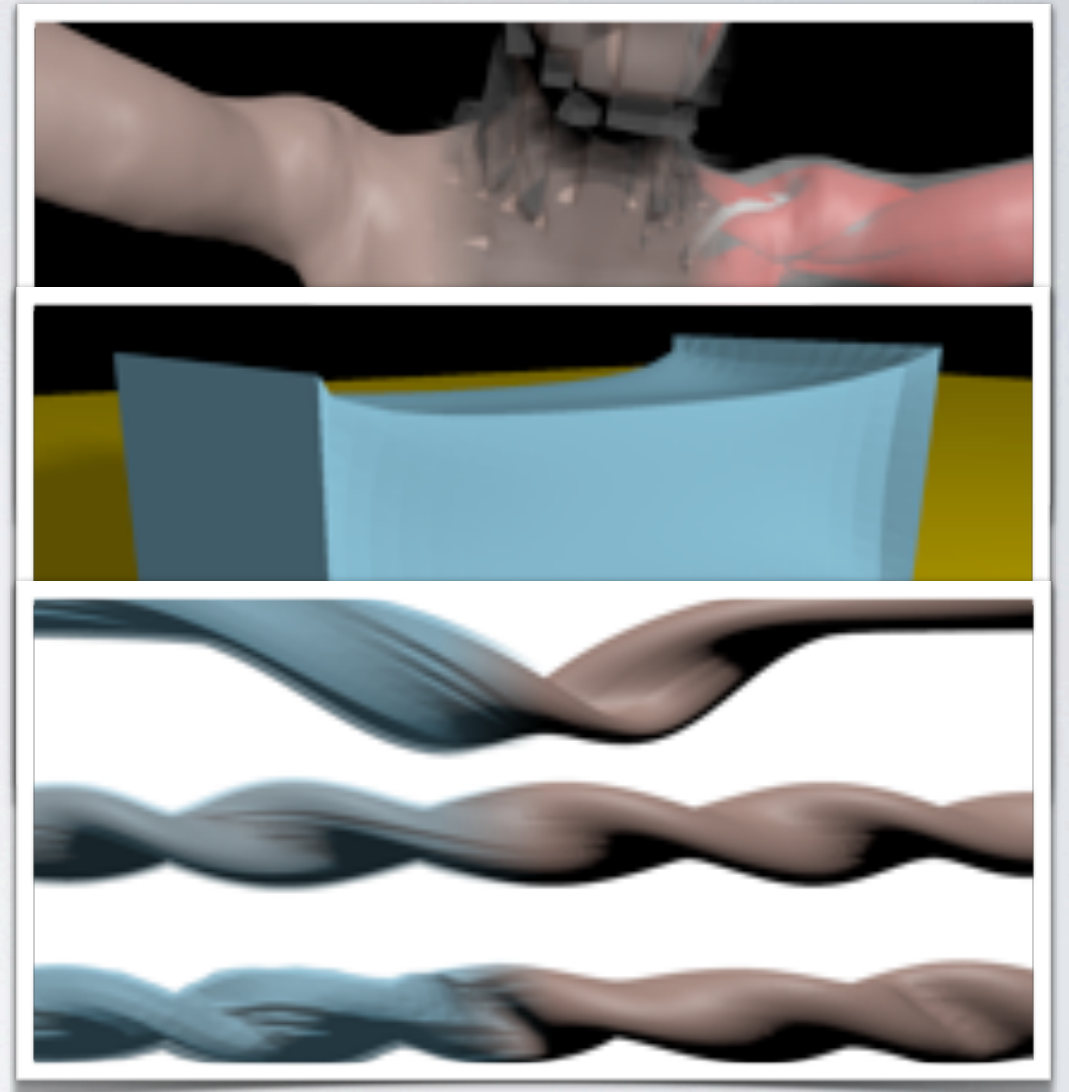
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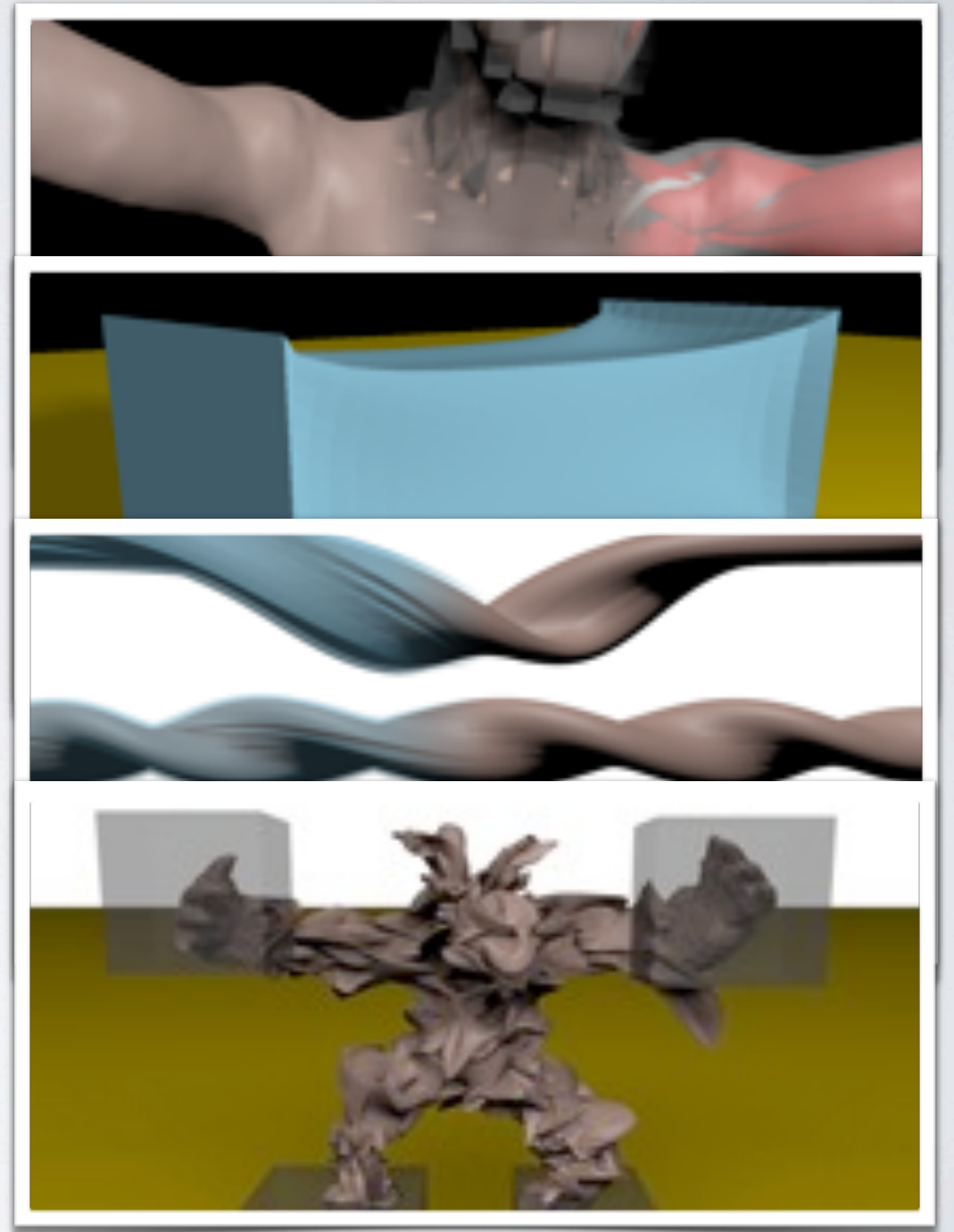
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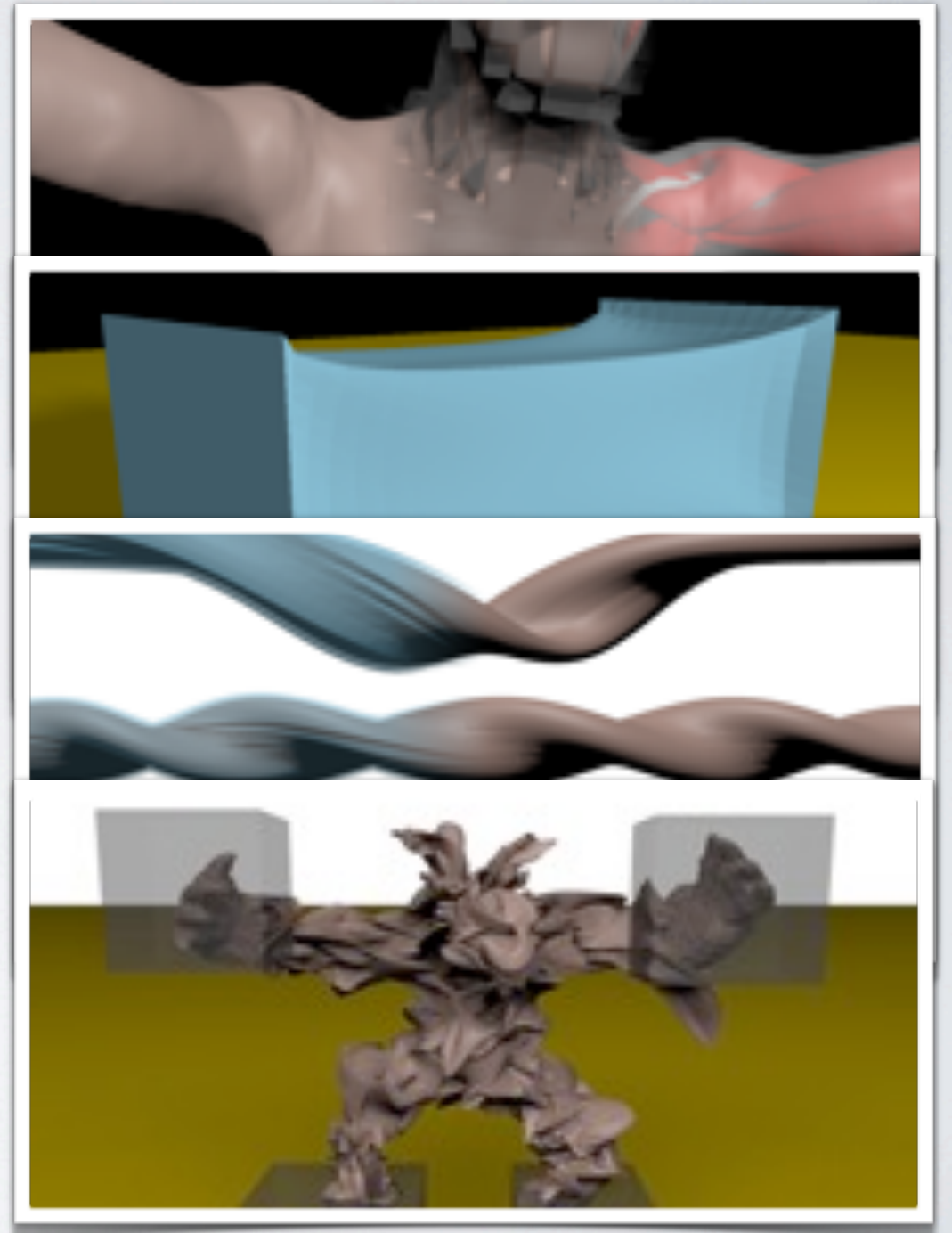
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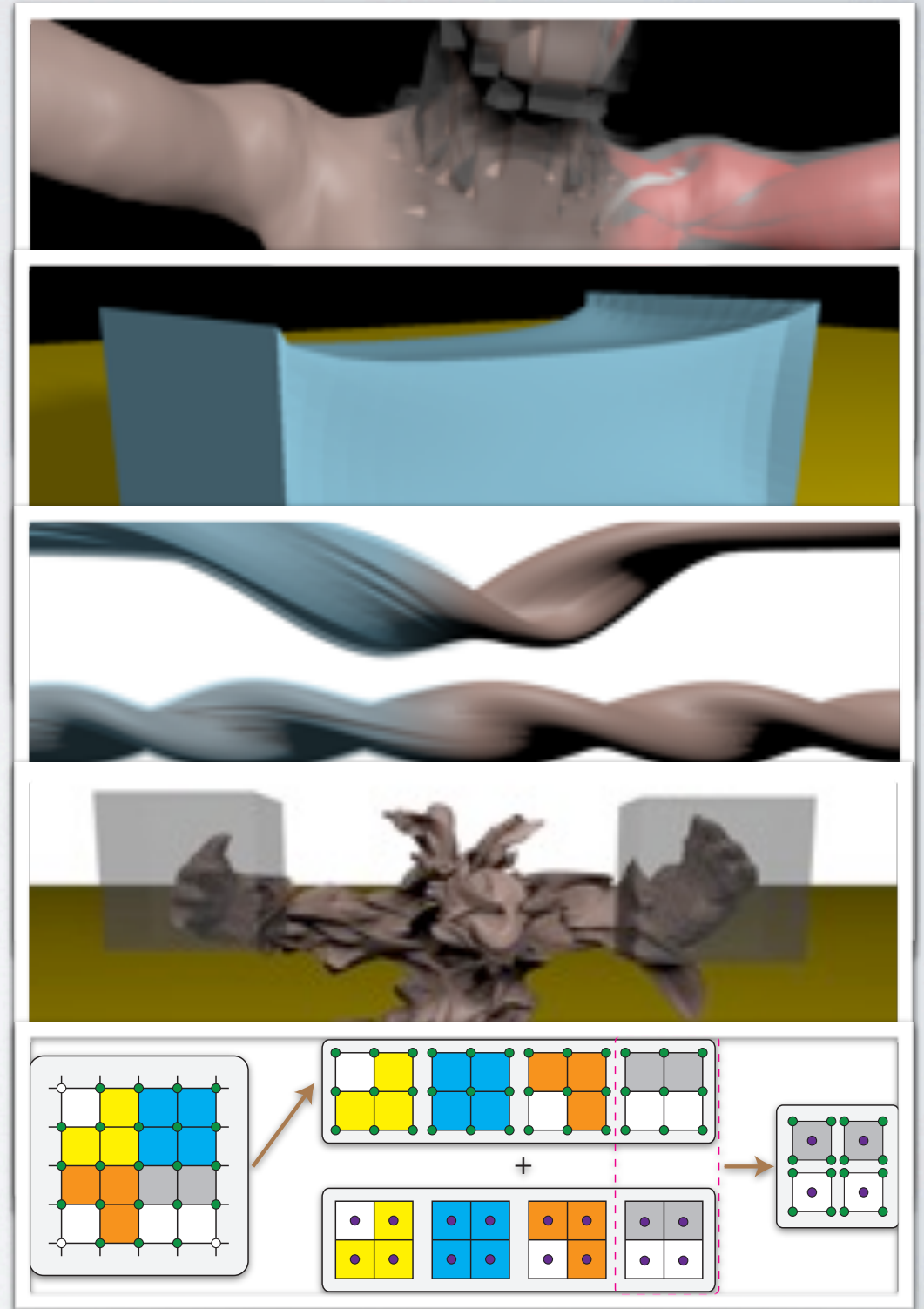
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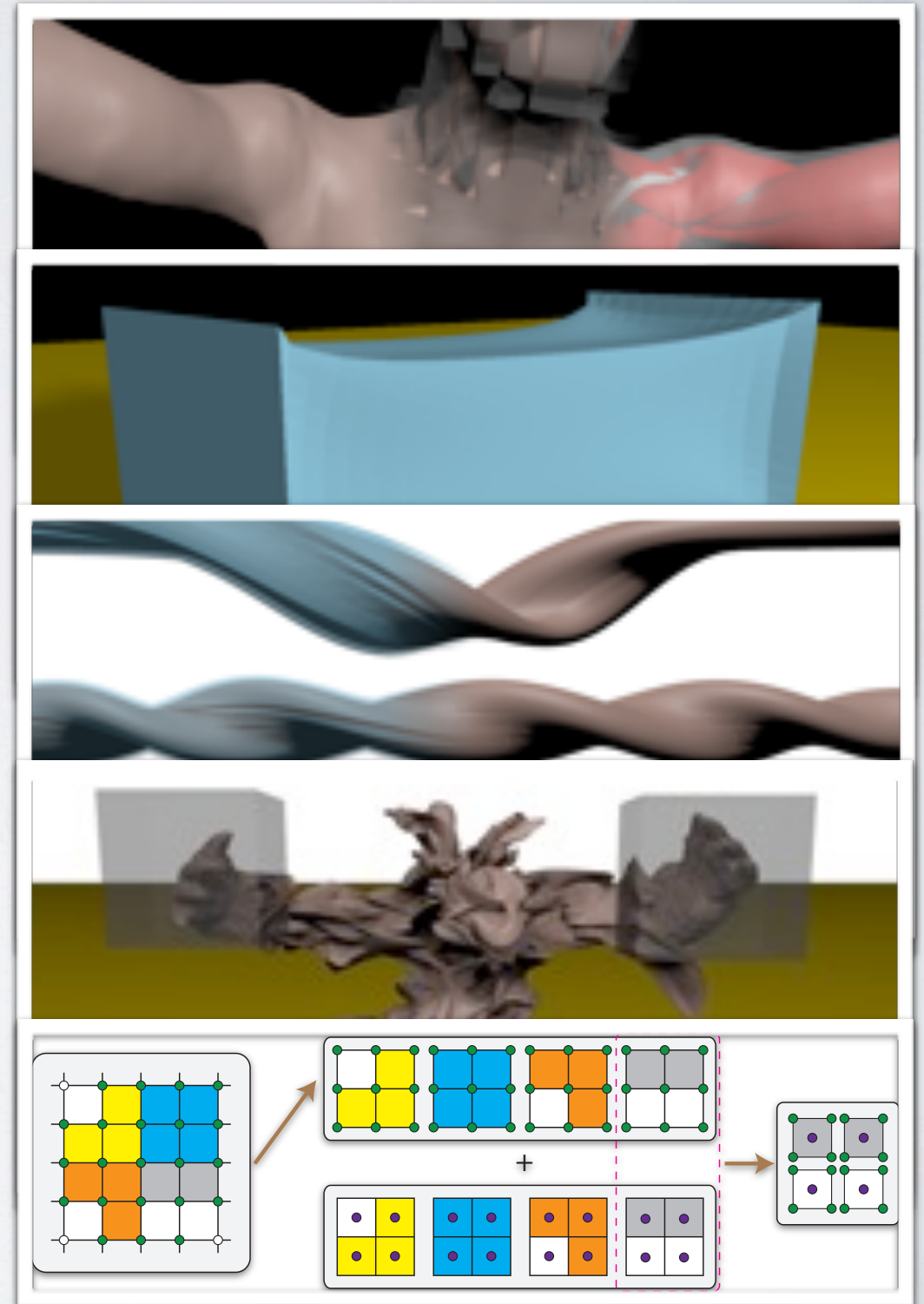
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LIMITATIONS AND FUTURE WORK

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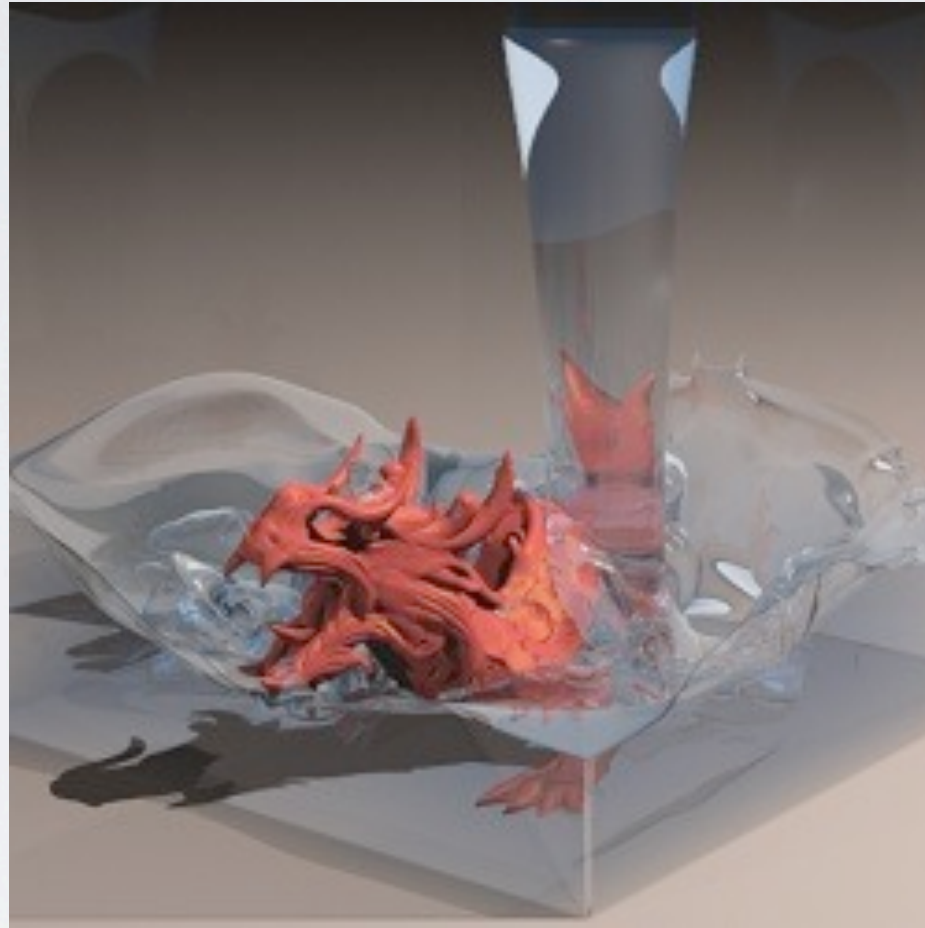
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FASTER SOLVERS

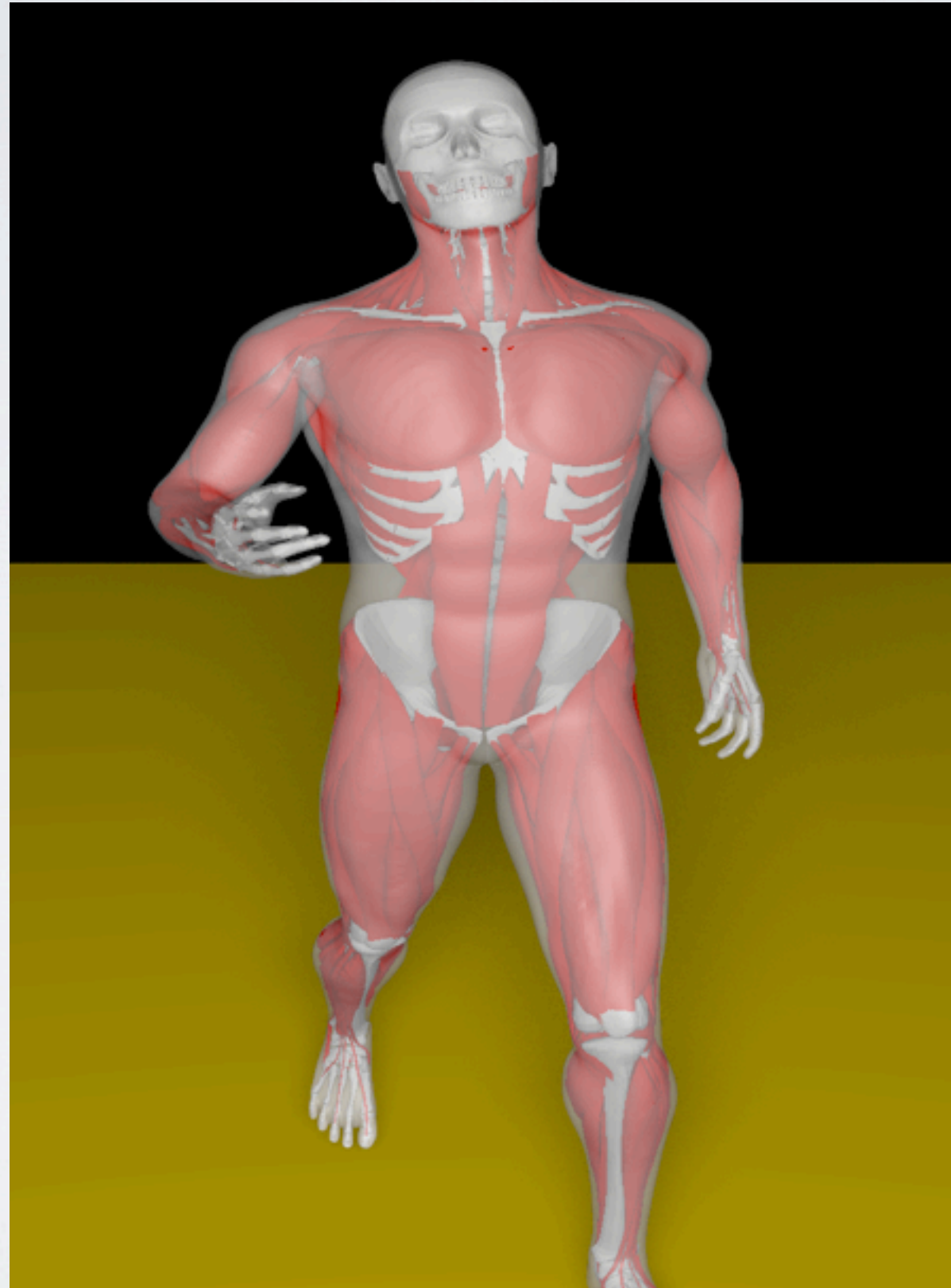
FASTER SOLVERS



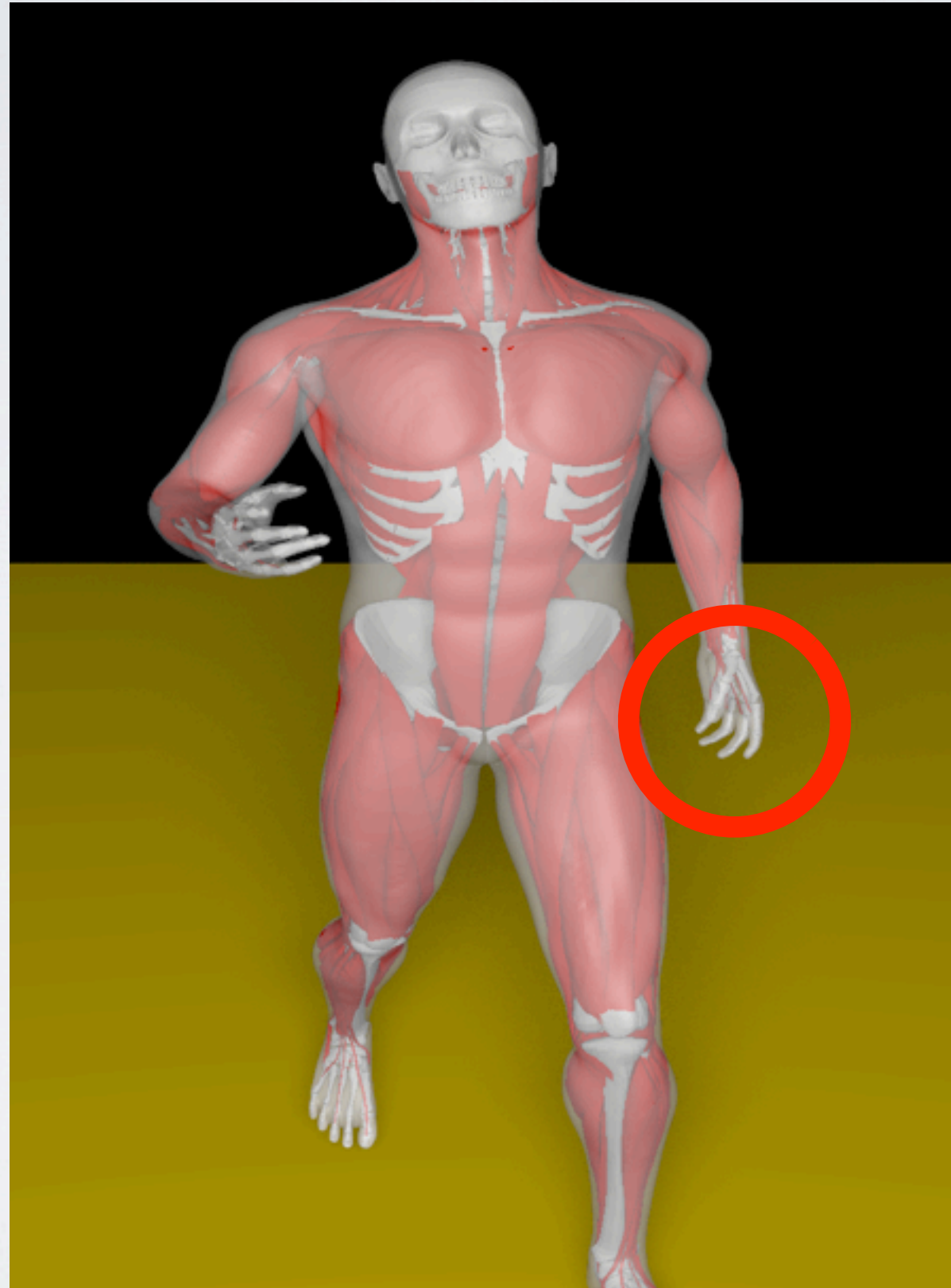
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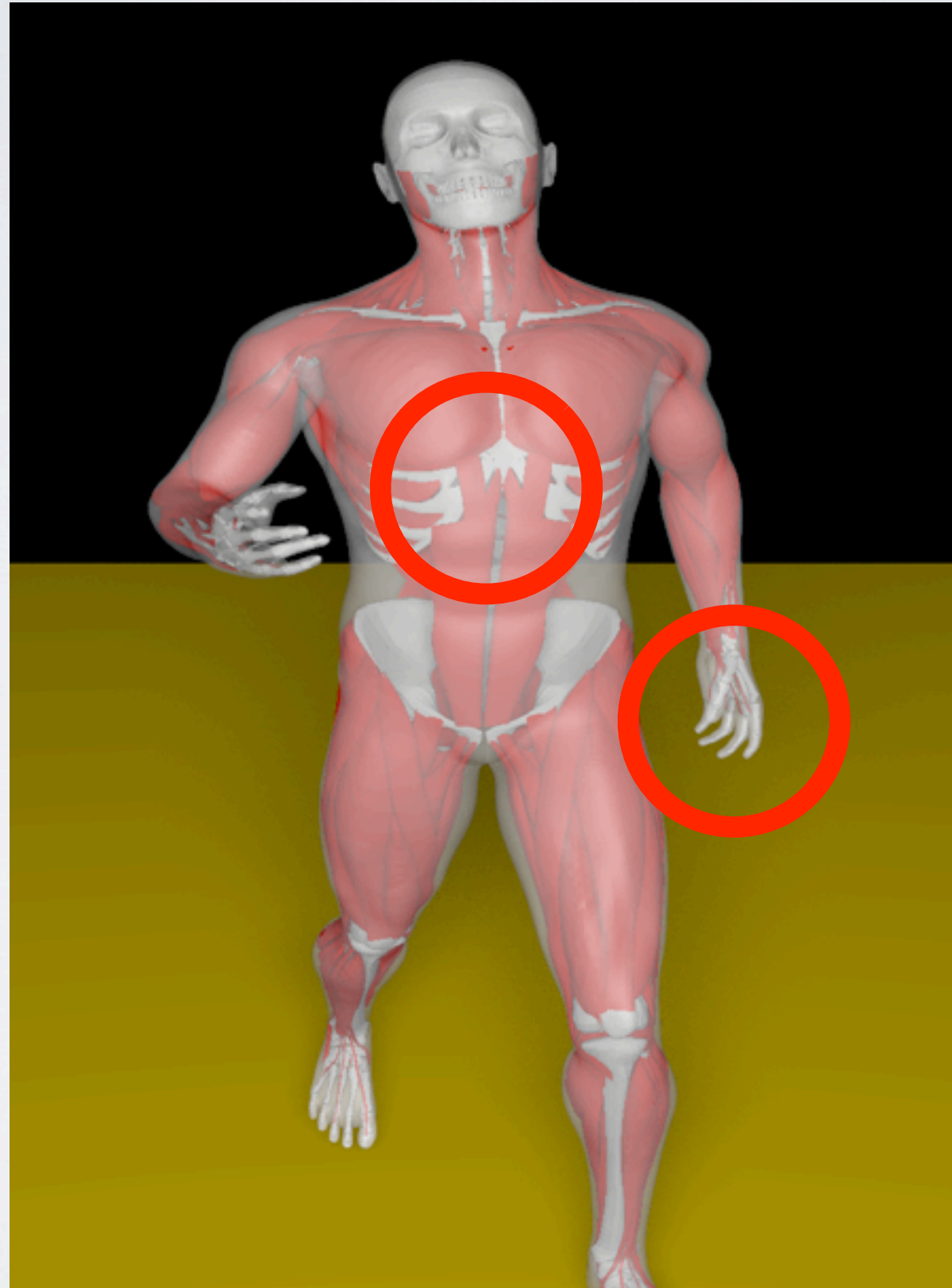
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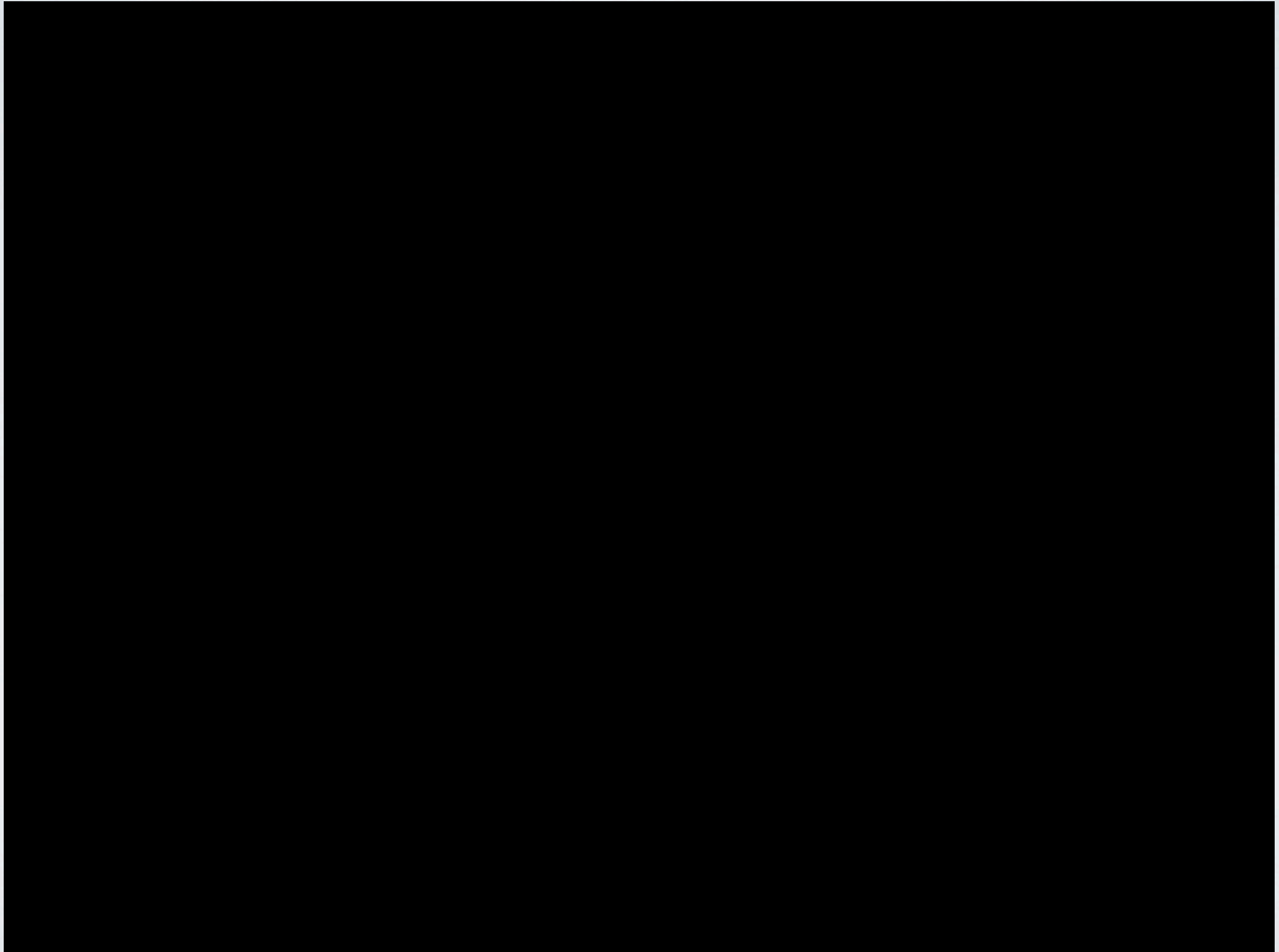
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TOPOLOGICAL CHANGE

[Sifakis et al 2009]

TOPOLOGICAL CHANGE



[Sifakis et al 2009]

ACKNOWLEDGEMENTS

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Eftychios Sifakis
Nathan Mitchell
Raj Setaluri

Thank you

Questions?